

# Application of 3D printing technology to thoracic wall tumor resection and thoracic wall reconstruction

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**Background:** Thoracic wall tumors can leave large defects in the thoracic wall after tumor resection. Currently, the shape of the materials commonly used for thoracic wall repair, including dacron mesh and titanium alloy mesh, cannot readily conform to the shapes of defect sites. In this study, we aimed to retrospectively review and evaluate the outcomes of applying three-dimensional (3D) printing technology in assisting in thoracic wall tumor resection and thoracic wall construction.

**Methods:** Six patients with thoracic wall tumors underwent thin-slice CT scanning. We 3D reconstructed pleural tumors and adjacent structures with Amira software and 3D printed them. Preoperative simulation, surgical rehearsal, and surgical planning were performed, and 3D conformal titanium plates were created based on 3D reconstruction models and sutured to the defect sites of the thoracic wall. We also retrospectively reviewed 10 patients who underwent this surgery with conventional methods. All of the demographic data, clinical data, and laboratory findings (non-normally distributed variables) were compared between these two groups.

**Results:** 3D reconstructions of the tumors and their adjacent structures were successfully performed, and 3D printing physical models and conformal titanium plates were also successfully obtained. The plate afforded accurate matching, less bleeding, fewer postoperative complications, and less pain.

**Conclusions:** This 3D printing technology can aid in preoperative rehearsal, surgical planning, and the manufacturing of 3D implants. The 3D titanium plate has such advantages over traditional implants as having good fit and hardness, improving the surgical accuracy and curative effect, and reducing complications, such as bleeding and pain.

Keywords: 3D printing; 3D visualization; thoracic tumor resection; thoracic wall reconstruction

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#### Introduction

Thoracic wall tumors originate from such tissues as thoracic wall bones, muscles, blood vessels, and nerves (1). These common thoracic tumors erode the thoracic wall and muscle. Thoracic surgery is often performed to resect thoracic wall tumors and their adjacent thoracic wall structures, but this often produces large defects in the thoracic wall, thoracic wall abnormalities, thoracic wall

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collapse, abnormal breathing, thoracic wall necrosis, and other complications (2). Polyester mesh and titanium alloy mesh are commonly used to repair these thoracic wall defects. However, polyester mesh has limited hardness, and conventional titanium plates are not suitable for the shape of damaged thoracic walls, creating difficulties for repair and giving rise to postoperative complications, such as pain, bleeding, and restricted respiratory movement.

In recent years, 3D printing has become widely used in the medical field, especially in surgical simulation, preoperative rehearsal, and the development of auxiliary surgical tools (3-8). Due to controversy regarding the hardness, stability, and quality of 3D-printed products, there are still few reports regarding the use of 3D-printed implants in the human. In addition, reports regarding the use of 3D printing technology in thoracic surgery remain limited, and it still remains unclear whether this technology can improve the accuracy and effect of surgery and reduce the rate of surgical complications.

We selected 6 patients who required thoracic wall tumor resection and thoracic wall reconstruction. We created 3D reconstructions of the thoracic walls and adjacent structures using computer tomography (CT) data, followed by 3D printing. We then simulated and rehearsed the surgery. Finally, we created conformal titanium plates for thoracic wall reconstruction. The clinical records of these 6 patients were retrospectively analyzed and also to those of patients who underwent surgery with conventional materials.

# Methods

#### **Patient selection**

The patients were selected from January 2016 to January 2018. Inclusion criteria were as follows: (I) thoracic tumor; (II) requirement for resection of part of the thoracic wall and thoracic wall muscles and resultant postoperative thoracic wall defects; (III) otherwise good health. Exclusion criteria were as follows: (I) tuberculosis or inflammatory lesions; (II) Diameter of the excision range under than 5 cm.

Six patients were selected as the 3D-printing group, including 3 males and 3 females, with an average age of  $(43.2\pm23.8)$  years (range, 10–68 years) (*Table 1*). Ten patients were selected as the conventional methods group, including 6 males and 4 females, with an average age of  $(42.9\pm14.3)$  years (range, 14–64 years) (*Table 2*).

## Strategy for 3D-printing group

## Three-dimensional reconstruction

We imported the patient's Dicom format image data using Amira software (http://www.amiravis.com, version 5.2.2) to segment the patient's tumor, lung, sternum, rib, thoracic vertebrae, costal cartilage, lung, liver, skin, and other structures. The lungs, sternum, ribs, thoracic vertebrae, and skin were automatically segmented. The costal cartilage, liver, and other structures were semi-automatically segmented and 3D reconstructed. Then, the model was smoothed and simplified, followed by 3D visualization and measurement. Finally, STL format files were generated for 3D printing.

# **3D** printing

We used stereolithography (SLA) (Formlabs Form2) for 3D digital model printing with liquid photosensitive resin with a maximum print size of 145×145×175 mm<sup>3</sup> and a print layer thickness of 0.02–0.1 mm. The larger models were printed using the MakerBot ReplicatorTM 2X, with a maximum print size of 400×300×200 mm<sup>3</sup> and a print layer thickness of 0.1–0.4 mm. After 3D printing was completed, the 3D printed models were simplified, and their surfaces were smoothed. The tumor, bone, and cartilage tissue structures in the model were colored using spraypaint and acrylic paint.

# Surgical planning

The 3D model constructed using Amira software was used to design the surgical approach and method of operation. The surgical resection line of the tumor was drawn, an outline at least 2.5 cm around the malignant tumor (9). Then, the 3D implant plate was designed to perfectly match the excision margin. Simultaneously, according to the 3D printing model, the 3D morphology and spatial adjacency relationship of the tumor were re-observed, and the plans for tumor resection and thoracic wall reconstruction were applied.

#### 3D conformal titanium plate production

Using to the 3D printing model, the homemade CNC and EDM equipment was used to produce point-to-point extrusion. The operating engineer set the processing parameters for one-time shaping based on the patient's condition. During the process, a 3D engraving machine was

Case	Sex	Age ł years) th	Part of 3D loracic we	o all	Tumor pathology	Tumor Ti volume (cm <sup>3</sup> ) w	he size of tumor thoracic vall projection area (cm <sup>2</sup> )	Whether to inv the sternum	ade Wheth	her to invade pracic vertebra i	Whether to invade the r	rib o
-	Male	65 Left a	interior the wall	oracic	Desmoid tumors	2208.5	21.7×18.7	Yes		No	The third to ninth rib	9
2	Male	10 Right th	t posterolá ioracic wá	ateral all	Langerhans cell histiocytosis	51.8	9.7×4.8	No		No	The fifth to seventh rit	۵ ۵
ო	Female	56 Left i th	anterior co Ioracic wa	enter all	Papillary adenocarcinoma	8.8	3.3×3.2	Yes		No	The first to second rik	0 0
4	Male	68 Right	lateral thc wall	oracic	Neurilemmoma	552.5	13.8×9.9	No		No	The sixth t ninth rib	Q
Q	Female	35 Ri	ight anteri ioracic we	ior all	Breast wall recurrence after right breast cancer surgery	25.4	7.1×3.8	Yes		No	he third to f rib	fifth
9	Female	25 Left th	posterola ioracic wa	uteral all	Ewing's sarcoma ribs	79.3	11.2×4.9	No		No	The eighth tenth rib	ę
Table	2 Operati	on condition	1 of conver	ntion r	nethod group				4			
Case	Tumor	pathology	Sex	Age	Patching material thc	The size of tumor sracic wall defect (	r cm²) Location	Operation Amo time (min) bleedi	unt of ng (mL)	Postoperative complication	e s	ain
-	Chol sarcor	ndroma matosum	Male	1 4	Conventional titanium plate	7×8	Front right Upper thoracic wall	170 5	50 Tit su le	anium plate pun Jbclavian artery, eading to hemori	ictured 8 which rhage	Ø
5	Desmc	aid tumors	Male	29	Conventional titanium plate	11×12	Left anterior thoracic wall	120 1.	200 Tit.	anium plate pun skin	Ictured	2
ო	Lung ca invaded t	incer which horacic wall	Female I	64	Conventional titanium plate	9×8	left thoracic wall	180 5	.00 Tit.	anium plate pun skin	Ictured	2
4	Giant cé ste	ell tumor of srnum	Male	38	Conventional titanium plate	7×10	sternum	150 6	00	None		2
£	Ewing'	s sarcoma	Male	57	Conventional titanium plate	10×10	sternum	210 8	00	None	9	9
9	Lung ca invaded t	incer which horacic wall	l Male	45	Polypropylene patch and bone cement complex	7×7	Right anterior chest wall	190 4	.00 Infe	ection of transple	antation	5
7	Desmc	aid tumors	Female	47	Polypropylene patch and bone cement complex	12×12	Right anterior lower chest wall	180 1,-	000	None		80
œ	Desmc	aid tumors	Female	52	Polypropylene patch and bone cement complex	8×8	Left anterior lower chest wall	150 9	00	None	9	9
თ	Lung ca invaded t	incer which horacic wall	l Male	46	titanium mesh	6×6	Right thoracic wall	130 1,	100	None		5
10	Rhabdon	nyosarcoma	ו Female	37	titanium mesh	11×12	Right thoracic wall	170 5	00	None	U	9

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Table 1 Patient information of 3D print group

Tabl	e o Operation contantion of the second	dnoig								
Casi	e Tumor pathology	Sex	Age	Patching material	The size of tumor thoracic wall defect $(\mathrm{cm}^2)$	Location	Operation time (min)	Amount of bleeding (mL)	Postoperative complications	Pain
-	Desmoid tumors	Male	65	3D conformal titanium plate	21.7×18.7	Left anterior thoracic wall	240	1,500	None	ю
N	Langerhans cell histiocytosis	Male	10	3D conformal titanium plate	9.7×4.8	Right posterolateral thoracic wall	190	100	None	ო
с	Papillary adenocarcinoma	Female	56	3D conformal titanium plate	3.3×3.2	Left anterior center thoracic wall	110	100	None	ო
4	Neurilemmoma	Male	68	3D conformal titanium plate	13.8×9.9	Right lateral thoracic wall	100	200	None	ო
Q	Breast wall recurrence after right breast cancer surgery	Female	35	3D conformal titanium plate	7.1×3.8	Right anterior thoracic wall	240	100	None	ω
9	Ewing's sarcoma ribs	Female	25	3D conformal titanium plate	11.2×4.9	Left posterolateral thoracic wall	140	200	None	4

used to create a 1:1 3D conformal titanium plate, followed by inspection, disinfection, and packaging.

# Surgery

Before surgery, we calculated each patient's pulmonary function. We performed thoracic wall tumor resections in the patients. The excision range included the entire thoracic wall tumor, tumor-infiltrated ribs, costal cartilage, and intercostal muscle. The resection margin was at least 2.5 cm around the tumor. In the surgical margin, we collected tissue from the cutting edge and made frozen pathological sections to check for metastasis and so avoid incomplete excision. We located the 3D conformal titanium into the thoracic wall defect and fixed it to the thoracic wall with screws (*Table 3*).

# Fifteen days follow-up

We performed thin-layer high-resolution CT scan as a recheck 15 days after surgery, with a scan image resolution of 512×512 and a layer spacing of 0.7 mm. Then, 3D reconstruction of the 3D conformal titanium plate and the thoracic wall bone was performed, and the titanium plate insertion was re-checked. We also calculated the pulmonary function of the patients in the 3D group.

# Strategy for the conventional method group

We performed thoracic wall tumor resections in the 10 patients. The excision range included the entire thoracic wall tumor, tumor-infiltrated ribs, costal cartilage, and intercostal muscle. The resection margin was at least 2.5 cm around the tumor. We inserted the conventional titanium plate, titanium mesh, or polypropylene patch and bone cement complex into the thoracic wall defect and fixed it to the thoracic wall with screws (*Table 2*).

# Ninety days of follow-up

In a further follow-up after 3 months, the patients were reexamined by the surgeon, which included pain and CT exams.

# Statistical analysis

SPSS 22.0 statistical software was used for statistical analysis. Data were expressed as the frequency and percentage for categorical variables and the mean  $\pm$  standard deviation for continuous variables or the median and inter



**Figure 1** Tumors and adjacent structures of the 6 surgical patients. (A) 3D reconstruction images of aggressive fibroma and adjacent structures for case 1; (B) 3D reconstruction images of Langerhans cell histiocytosis tumor and adjacent structures for case 2; (C) 3D reconstruction images of papillary adenocarcinoma and adjacent structures for case 3; (D) 3D: reconstruction images of neurovascular and adjacent structures for case 4; (E) 3D reconstruction images of right breast cancer and adjacent structures for case 5; (F) 3D reconstruction images of right breast cancer and adjacent structures for case 5; (F) 3D reconstruction images of right breast cancer and adjacent structures for case 5; (F) 3D reconstruction images of rib Ewing's sarcoma and adjacent structures for case 6. T: tumor; C: cartilage; L: lung; Li: liver.

quartile range (IQR). All demographic data, clinical data and laboratory findings (non-normally distributed variables) were compared between the two groups using the Wilcoxon signed rank test and Mann-Whitney U test for other variables. To compare the proportions of patients,  $\chi^2$  test or Fisher exact test was performed. All statistical tests were two-sided and significance was defined as P<0.05.

## Results

We successfully constructed 3D digital models of thoracic tumors and their adjacent structures and reconstructed thoracic walls. The adjacent structures included pulmonary blood vessels, lungs, bronchi, ribs, sternum, and costal cartilage (*Figure 1*). The tumor volumes ranged from 8.8–



**Figure 2** 3D reconstruction images, titanium plate design, intraoperative photographs and postoperative CT images of giant desmoid tumors and adjacent structures. (C) 3D reconstruction images of giant desmoid tumors (left front view) and position of the transverse sections in panels (A-B); (D) a 3D conformal titanium plate was successfully implanted in the patients' body; (E) 3D conformal titanium plate design; (F) CT images at 2 weeks after operation. T: tumor.

2,208.5 cm<sup>3</sup> (*Table 1*). Case 1 had the largest tumor volume. This tumor protruded into the left anterior and inferior thoracic wall and the sternum (*Figures 1A*,2). Case 6 was Ewing's sarcoma, which was located in the posteromedial lateral thoracic wall (*Figure 1F*). Case 4 was neurilemmoma, 552.5 cm<sup>3</sup> that protruded substantially into the outer side of the sixth to ninth chest ribs (*Figure 1D*). Case 5 was breast cancer recurrence, which was located in the third to fifth ribs of the right anterior thoracic wall, with invasion of the sternum (*Figure 1E*).

Based on the 3D reconstruction model, we successfully 3D printed the model using a photosensitive resin printer

and studied the 3D morphology and the spatial relationships of the tumor. The scope of the surgical resection and the size, area, space location, and shape of the resected thoracic wall were clarified to provide enough information prior to surgery. The 3D conformal titanium models were successfully designed and created (*Figures 3-5*).

We successfully completed the thoracic tumor resection and thoracic wall reconstruction. Since the tumor in case 1 was large, diaphragmatic and pericardial repair were performed (*Table 3*). The recurrent breast cancer patient (case 5) had thoracoabdominal wall flap metastasis; so we performed flap transplantation. The skin was obtained



**Figure 3** 3D reconstruction images, 3D prints and surgical charts of Ewing's sarcoma tumor and adjacent structures. (A) CT cross-sectional image of Ewing sarcoma (A level); (B) CT cross-sectional image of Ewing's sarcoma (B level); (C) 3D reconstructed images and surgical resection area of Ewing's sarcoma and adjacent structures; (D) 3D printing model of Ewing's sarcoma and the corresponding ribs and thoracic vertebra; (E) 3D conformal titanium plate; (F) A 3D conformal titanium plate was successfully implanted in the patient's body. T: tumor.

from the right femur. Although the sizes of the resected tumors were different (*Table 1*) and the volume of these tumors was relatively large, the 3D-shaped titanium plates were completely consistent with the thoracic wall defect. In 3D-printing group, the surgical bleeding was less, and the patients had good curative effect and recovery (*Table 4*).

According to the 3D reconstructed images by CT scan (*Figure 4*) at 15 days after operation, it was found that titanium plates produced with the assistance of 3D printing were completely consistent with the thoracic wall defect sites in all 6 cases (*Figure 2D*). No fixed titanium

plate displacement was observed, and patients had good postoperative activity, good respiratory movement, and no abnormal respiratory movements.

According to the CT exam performed 90 days after surgery, in the 3D-printing group, there were no postoperative complications in the 3D-printing group, such as hemorrhage, pneumothorax, fixed titanium plate displacement, metastasis, or abnormal breathing. However, in the conventional methods group, 4 patients showed such complications as infection and puncture of the artery or skin by the titanium plate (*Tables 3,4*). The post-operation pain



**Figure 4** 3D reconstruction images, 3D prints and surgical photographs of breast cancer and adjacent structures. (A) 3D reconstruction image of breast cancer (front view); (B) 3D model of breast cancer (front view); (C) A 3D conformal titanium plate was successfully implanted in the patient's body; (D) flap transplantation was performed after 3D titanium plate insertion. T: tumor; S: sternal; C: cartilage.

score was lower than in the conventional methods group (*Tables 2,3*).

The pulmonary function of the patients in 3D group showed no significant difference before and after the operation (P<0.05) (*Table S1*).

## Discussion

3D printing technology is widely used in medicine, including such fields as orthopedics, plastic surgery, maxillofacial surgery, dentistry, and urology (3-8). 3D printing is mainly used for auxiliary diagnosis, surgical design, and surgical rehearsal. Resection of the sternum, rib and cartilage requires thoracic wall reconstruction using a material that permits stabilization of the chest, ensures proper respiratory function, and protects the thoracic organs (10). To date, no treatment scheme has been established for the thoracic wall. There is a general consensus that every malignant tumor should be removed entirely, ideally with 2–5 cm margins of healthy tissue (11). The choice of chest reconstruction depends on the size of the defect and operator preferences. Defects of <5 cm in diameter do not usually require rigid implant reconstruction (12,13). Therefore, for resection of larger sternal and rib fragments, it is often recommended that they be replaced with homogenous or allogeneic material.

The range of implants used in the thoracic wall is very broad. The most commonly used materials are methyl methacrylate (10), titanium (9) coated with sealed prolene mesh from inside and outside of the thoracic wall, Marlex, polytetrafluoroethylene, and Vicryl. In addition, for the Ley's prostheses in the form of a footprint-shaped titanium plate fixed to the ribs with metal threads, 8 sternum and rib fragments made of 3D-printed titanium (14,15) are also used; however, this 3D technology is expensive, and 3D printing has yet to undergo ethical review. Silicone implants based on patients' chest prints prior to surgery can be used as a less expensive surgical option, but they have the most complications, including seroma formation (31%) and lower aesthetic satisfaction (only 69%). This patient had a severe physical examination (PE) deformity and in retrospect would have been a better candidate for thoracic surgical correction at a young age because the implant was not very hard (16). Autografts of osseous tissue and muscle fragments and allografts of the sternal fragment can be obtained from deceased donors (11). However, these implants are less rigid



**Figure 5** 3D reconstruction images, titanium plate design, intraoperative photographs and postoperative CT images of giant invasive fibroma and adjacent structures. (A) 3D reconstruction images of giant invasive fibroma (left front view); (B) A 3D conformal titanium plate was successfully implanted in the patients' body; (C) 3D conformal titanium plate design; (D) CT images at 2 weeks after operation. T: tumor; Bo: bone in tumor; Ar: artery; Tr: trachea.

Characteristics	3D print group	Convention method group	P value
Number	6	10	
Mean age	45.5 [21.25–65.75]	45.50 [35.00–53.25]	0.914
Male gender	3 (50%)	6 (60%)	1
Operation time (min)	165 [108–240]	170 [145–182]	0.957
Amount of bleeding (mL)	150 [100–525]	700 [500–1,025]	0.029
Postoperative complications	0	4	0.234
Pain	3 [3–5]	6 [5–7]	0.024

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and do not resist stress from respiration, thoracic support, or load-bearing. An implant should be resistant to the forces that act on the skeleton in the chest but pliable enough to adjust it according to the size of the sternum defect, translucent under X-rays, and made of a material that resists bacterial growth (10). Polyethylene appears to be a good material for sternal implants because it is rigid and nonabsorbable and it does not react with bones, soft tissues, or body fluids. It has proper rigidity and resistance but it is radio-opaque on X-rays. It can be fixed to metal plates (titanium, surgical steel) and bones using screws. However, it is not recommended for joints as an endoprosthesis because it is prone to surface abrasion, which can be harmful.

Reconstruction procedures after sternum resection are difficult and are complicated by a significant percentage of cases with complications-estimated between 33% and 46%. The most often observed complications are those associated with respiratory disorders (16). Other known complications associated with sternum implants are chronic pain, chest deformations, local pleural thickening, and necrosis of pedicle muscle lobes (9), mediastinitis, and loosening of the implant mounting, resulting in instability of the chest. Sternal implant fractures have also been reported (17). A conventional titanium plate is flat and rectangular, and it does not line up with the broken ends of bone defects, does not fit the thorax, shifts easily, and wears through the skin, causing postoperative pain and hematoma. The 3D printing of titanium alloy implants remains controversial in surgery. Due to their hardness and strength, titanium alloy 3D implants have yet to be approved by hospital ethics committees and they bring on certain medical risks. Nevertheless, it is feasible to use 3D printing to assist the formation of titanium plates, as the titanium plate prior to 3D printing has passed FDA certification.

3D digital navigation and printing technology are used in tumor resection and reconstruction of the chest in the field of thoracic surgery, which helps surgeons better understand the preoperative thoracic wall tumor site, 3D morphology, invasion range, and spatial adjacency relationships, and helps thoracic surgeons make preoperative surgical plans and conduct surgical rehearsals. The 3D-printingassisted titanium plate completely conforms to the threedimensional shape of the thoracic wall, thereby improving the curative effect of the surgery, shortening the operation time, and substantially reducing the abrasion of the implant on the residual sternum, ribs, thoracic wall muscle, and pleura. No surgical complications, such as bleeding or abnormal breathing, were observed in 6 cases, but in the conventional methods group, 4 patients had such complications as infection and puncture of the skin or artery by the titanium plate. Moreover, the cardiothoracic implants designed by 3D printing were used to fill the thoracic wall, which played an important role in protecting the contents of the thorax, such as the heart and lungs, and did not involve bearing weight or strenuous exercise. Therefore, the biomechanical requirements of the 3D conformal titanium plate were lower than those of orthopedic load-bearing parts, rendering the procedure easier.

3D conformal titanium plates are not prone to show dislocation or displacement postoperatively. They do not rub against the thoracic wall during normal breathing, thus avoiding local thoracic wall injuries and hematomas. Patients showed little bleeding, except for the 1,500 mL blood loss in one patient with a large chest tumor. Surgical bleeding was only 100-200 mL in the remaining patients, reducing both blood transfusion costs and the risks of transfusion. The 3D conformal titanium itself is made of titanium alloy. It has a rigid structure, does not deform postoperatively, and resists gravity and tension caused by breathing and tensile forces. The recovery time is greatly shortened, decreasing from two weeks to one week. Moreover, the 3D conformal titanium plate is not actually a 3D-printed titanium plate and thus is consistent with FDA certification and is easy to implant.

In this study, 3D printing aided successful thoracic tumor resection and thoracic wall reconstruction in 6 cases, bringing thoracic surgical resection and thoracic wall reconstruction to a new level.

# Limitations

Due to the limited number of procedures, and differences among the tumor resection sites and the size and nature of the tumors, it is difficult to develop surgical criteria for resection and reconstruction of the thoracic wall. We expect to increase the number of surgical procedures in the future to improve 3D printing in assisting thoracic tumor resection and thoracic wall reconstruction and to develop criteria for the procedure.

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# Footnote

*Conflicts of Interest:* The authors have no conflicts of interest to declare.

*Ethical Statement:* The study was approved by the Ethical Committee of Southwest Hospital (IRB number: KY201846). Informed consent of the operation was obtained from all patients before surgery.

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# Supplementary

# Table S1 Pulmonary function before and after operation

Case	FEV1 before operation (L)	FEV1 after operation (L)	MVV before operation (L/min)	MVV after operation (L/min)
1	2.2	2.0	80	78
2	1.8	1.7	100	97
3	2.0	2.0	90	90
4	2.0	1.9	85	83
5	1.8	1.8	78	77
6	1.9	1.8	102	98