

The comparison of spatial resolution of ion chamber, diode, and EBT3 film based on the dose profile

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Background: It is essential for the physicist to quantify the dose of the radiation prior and during cancer treatment to ensure proper execution of the treatment plan. The most common way to measure the dose is utilizing Farmer chamber. The limitation of Farmer chamber is that it only provides dose of a specific point, while the beam dose profile is needed for the planning system. The Gafchromic EBT3 film can provide a quantitative dose profile in a 2D space. The EBT3 film has low energy dependence, similar effective atomic number to water, and self-developing; making it an ideal candidate for dose profile measurement.

Methods: Dose profiles of EBT3 was measured, analyzed and compared to semiflex chamber and EDGE detector under same conditions. The EBT3 films were placed at the center of RW3 water phantom (30×30× 30 cm³) under flattening filter free (FFF) Mode of Linac. The EBT3 films were calibrated by additional RW3 with a Farmer chamber under the stacked RW3 water phantom. Percentage depth dose (PDD) and Matlab were used to fit the dose curve of EBT3 and the results are presented.

Results: The penumbra of the measured dose profile through EBT3 film demonstrated little differences when comparing with that of the EDGE detector and noticeable differences when compared to that of the semiflex chamber. For a field size of $2\times 2 \text{ cm}^2$, (b=0.08, depth of 5 cm, beam off central axis 0.8 cm), the measured difference of dose profile between EBT3 and EDGE detector is -2.24%. Under the same conditions, the dose profile difference between EBT3 and semiflex chamber is 10.59%.

Conclusions: This study shows that EDGE detector has the highest spatial resolution to the dose profile. EBT3 film in combination with solid phantom can quickly sample dose profile in 2D. EBT3 film can be considered to be an excellent quality assurance (QA) tool with accurate dosimetry, a good spatial resolution and tolerable dose uncertainty.

Keywords: EBT3; EDGE detector; dose profile

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Introduction

In response to a single high-dose treatment, the linear accelerator can utilize a flattening filter free (FFF) mode to increase the dose rate and shorten the treatment time. In FFF mode, the dose profile is not a flat curve. The accuracy of the dose calculation in the treatment planning system is affected by the actual dose distribution. Thus, it is crucial to determine the dose profile accurately.

The tools usually used to measure the dose profile are an ion chamber (1-5) or a diode dosimeter with higher spatial resolution (6-8). The above two tools require a water



Figure 1 The location of the film.



Figure 2 The whole experimental design.

phantom system to obtain a dose profile instead of a point dose. We have to rely on other measurement tools such as radiochromic films (9-12) to display dimensional dose distribution information.

The market is currently dominated by EBT3 films (11-13). The spatial resolution can be affected by film quality, film scanning conditions and the size of the film's analysis area. A film with a smaller analysis area has a larger spatial resolution. Nonetheless, the spatial resolution cannot be elevated indefinitely since the dose uncertainty will increase during the same process.

This study's purpose is to find a precise, accurate, and high spatially resolved dose profile by comparing three different dose measurement tools, semiflex chamber, EDGE detector, and EBT3 film. This study also identified the appropriate analysis area unit by determining the different analysis areas units of EBT3 films along with its dosimetric uncertainty.

Methods

The linear accelerator Elekta Versa HD^{TM} used in this study produces 6 MV photon beam with no wedge.

According to the American Association of Physicists in Medicine (AAPM)'s Task Group (TG) reports (Klein *et al.* 2009, Kutcher *et al.* 1994, Schulz *et al.* 1983), the field size of the linear accelerator is 20×20 cm² and the percentage depth dose (PDD) of water phantoms was measured. The obtained data was converted into the PDD of polystyrene since the density difference between the polystyrene and the water had an inverse square relationship with the distance between them. The analyzed data was further used as the PDD table of RW3.

Film scanning

Ten copies of EBT3 films (lot no. 12281503) were obtained from Epson Expression 11000XL scanning. The unexposed pixel value (PV) film was defined pre-scan. The scanning mode had 48-bit full color, 127 dpi (5 pixels per mm) with a high-quality spatial resolution (14). Scanning always used portrait orientation.

The first batch of experimental exposure

According to the experimental design of a previous reference (15), RW3 was stacked into a $30 \times 30 \times 30 \text{ cm}^3$ cube. EBT3 film was placed vertically in the middle with the film facing toward the crosshairs in the in-plan direction (*Figure 1*). RW3 of the Farmer chamber was placed 1 cm below. Another 10 cm RW3 was stacked underneath it (*Figure 2*).

The field size was set to $20 \times 20 \text{ cm}^2$ with the source to surface distance (SSD) as 100 cm. Under flattening filter (FF) mode, the films were exposed under doses of 290 MU and 88 MU, respectively, 5 times. The temperature and pressure were recorded using a Farmer chamber, where the dose at 31 cm of RW3.

The exposed films were treated for 72 hours and subsequently measured by scanning. The scanning resolution conditions were the same as those above to obtain the PV at Therapeutic Radiology and Oncology, 2019



Figure 3 The selection method to analyze an area unit.

each point and this was defined as post-scan.

Establishment of a dose fitting formula

The analysis software Matlab (version 2016) was utilized. The image information of each film pre-scan and post-scan was transmitted into Matlab to obtain the PV under the red channel and then substituted into Eq. [1] to obtain the net optical density (NOD).

$$NOD(i, j) = log_{10}\left[\frac{PV_{pre}(i, j)}{PV_{post}(i, j)}\right]$$
[1]

where (i,j) refers to the position of the point on the film, PV_{pre} indicates the pre-scan PV, and PV_{post} (i,j) indicates the post-scan PV.

Along the central axis of the long side of the film, the unit of analysis area (*Figure 3*) was selected as $0.8 \times 0.8 \text{ cm}^2$ (b=0.4). All NOD values within this area were calculated and averaged. The selection range was 1.8-23.4 cm in terms of the depth of the film. Samples were collected at a 0.2 cm interval and each film could usually obtain 108 NOD values.

The NOD values obtained at the same depth for the five films of 290 MU and 88 MU are averaged again. The dose measured by the Farmer chamber on the day of the experiment was processed by the temperature and pressure correction formula and subsequently matched with the RW3 PDD table to determine the absolute dose corresponding to each depth NOD value on the film. The processed data was introduced into Eq. [2] in Matlab.

$$D_{fit} = a \times NOD + b \times NOD^c$$
^[2]

 D_{fit} is the dose obtained after fitting—defined as the fitted dose—and a, b, c are the fitting parameters.

No range was set for the first fitting parameters a and b. Parameter c was limited to 1–3. After obtaining the appropriate parameter c, the second fitting was performed. Parameter c was then fixed to reduce the uncertainty.

A complete equation was established after the calculation of all three parameters. Eq. [3] summarized the methods of calculating the uncertainty rates according to the guidelines of the Joint Committee for Guides in Metrology.

$$u_{c}^{2}(y) = \sum_{i=1}^{N} \left(\frac{\partial f}{\partial x_{i}}\right)^{2} u^{2}(x_{i})$$
[3]

 u_c (y) is the overall uncertainty and x_i is the value that impacted the uncertainty. There are a total of i, $u(x_i)$ is the standard deviation of the factors that impacted the uncertainty, and $\left(\frac{\partial f}{\partial x_i}\right)$ is the value after differentiating $u(x_i)$.

Two uncertainty sources may exist for this experiment, the scanning NOD values and the uncertainty caused by the fitting parameter in the fitting equation. Two uncertainty rates can be introduced into Eq. [4] to calculate the inaccurate percentage of doses, represented by $\delta_{dose\%}$.

$$\delta_{dose\%} = \frac{\sqrt{\delta_{exp}^2 + \delta_{fit}^2}}{D_{fit}} \times 100\%$$
[4]

$$\delta_{exp} = \sqrt{\left(a + c \cdot b \cdot NOD^{c-1}\right)^2 \cdot \delta_{NOD}^2}$$
[5]

$$\delta_{fit} = \sqrt{NOD^2 \cdot \delta_a^2 + NOD^{2c} \cdot \delta_b^2}$$
^[6]

$$\delta_{NOD} = \frac{\sqrt{\left(\frac{\delta_{PV_{pre}}}{PV_{pre}}\right)^2 + \left(\frac{\delta_{PV_{post}}}{PV_{post}}\right)^2}}{ln10}$$
[7]

 $\delta_{dose\%}$ is the percentage of the uncertainty of the dose obtained using the dose fitting equation; δ_{exp} is the uncertainty of the obtained NOD value, which also represents the standard deviation caused by the experiment; δ_{fit} refers to the uncertainty caused by parameters a and b in the dose fitting formula, which equals to the standard deviation of the dose fitting equation; δ_{NOD} is the uncertainty caused by PV. This was obtained by processing the PV_{pre} of the pre-scan and the PV_{post} of the post-scan to calculate the obtained standard deviation.

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The second batch of experimental exposure

Four copies of EBT3 films (lot no. 04201503) were used. RW3 was stacked into a $30\times30\times30$ cm³ cube and another 10 cm-thick RW3 was directly stacked underneath the first cube. The film was placed in the center of the upright RW3.

The SSD was 100 cm. Under the FFF mode, the field size was set to 2×2 and 3×3 cm². Each field of view was exposed to 200 MU twice and the irradiated films were in place for 72 hours and used in scanning afterward.

The image information of each film pre-scan and postscan was transmitted into Matlab to obtain the PV under the red channel and then substituted into Eq. [1] to obtain the NOD. The NOD values for a 2×2 and 3×3 cm² field size were subsequently averaged.

In the second batch of experimental analysis, the area unit is defined as below: b=0.04, b=0.08, b=0.2, and b=0.4. The NOD values in the area were averaged and substituted into the dose fitting Eq. [2] obtained in the first batch of experiments to calculate the value of the dot dose.

The dose profiles of the different depths 5, 10, and 20 cm were analyzed and compared with the same set of data in the EDGE detector and the semiflex chamber. Subsequently, the percentage differences between the various dose profiles were analyzed.

The differences between the dose points of EDGE detector and semiflex chamber were calculated by Eq. [8] below.

$$\frac{DP_semiflex \ chamber - DP_EDGE \ detector}{DP_EDGE \ detector} \times 100\% \ [8]$$

DP_semiflex chamber represents the dose profile measured by the semiflex chamber, while *DP_EDGE detector* represents the dose profile measured by the EDGE detector.

The differences between the dose points of EBT3 films and EDGE detector were calculated using Eq. [9] below. The same method is applied to EBT3 and semiflex chamber (Eq. [10]).

$$\frac{DP_EBT3 - DP_EDGE \ detector}{DP_EBT3} \times 100\%$$
[9]

$$\frac{DP_EBT3 - DP_semiflex \ chamber}{DP_EBT3} \times 100\%$$
[10]

DP_EBT3 represents the dose profile measured using EBT3 films, DP_semiflex chamber represents the dose profile

measured using the semiflex chamber, and *DP_EDGE detector* represents the dose profile measured using the EDGE detector.

Results

Comparison of the measured dose profiles using EDGE detector and semiflex chamber

Figures 4,5 show comparisons of the dose profiles measured using the EDGE detector and semiflex chamber in FFF mode. The X-axis represents the distance from the central axis of the beam. The symmetry of the beam was evaluated and shown in the figure. When the distance is positive, it represents dose profile location closer to gantry and vice versa. The Y-axis represents the percentage differences in the dose profiles. The doses were measured within 1.6 cm for a 2×2 cm² field size while they were analyzed within 2.4 cm for a 3×3 cm² field size. Profile measurements were made with depth of 5, 10, and 20 cm.

The analysis of $\delta_{dose\%}$ with different b values

Figure 6 shows the $\delta_{dose\%}$ —the percentage of dosimetric accuracy—for different radiation doses and calculated with b values of 0.04, 0.08, 0.2, and 0.4. The $\delta_{dose\%}$ calculated with b values of 0.04 or 0.08 were larger than those with b values defined as 0.2 or 0.4. With a low radiation dose of 30–60 cGy, the differences between $\delta_{dose\%}$ might reach 2% at most.

The comparison of measured dose profiles between EBT3 films and the semiflex chamber and also between EBT3 and the EDGE detector

Figures 7,8 show comparisons of measured dose profiles between EBT3 films and semiflex chamber and between EBT3 films and EDGE detector for depths of 5, 10, and 20 cm under FFF mode. The doses were measured within 1.6 cm for a 2×2 cm² field size and were analyzed within 2.4 cm for a 3×3 cm² field size. The b value, which defines the analysis unit, was 0.08 for the analysis of both field sizes.

The comparison of dose profiles with different b values

Figures 9,10 show the comparison of the dose profiles measured by EBT3 films to those measured by either



Figure 4 The comparison of dose profiles measured by the EDGE detector and semiflex chamber in a 2×2 cm² field size.



Figure 5 The comparison of dose profiles measured by the EDGE detector and semiflex chamber in a 3×3 cm² field size.

EDGE detector or semiflex chamber with four different b values either in a 2×2 cm² or a 3×3 cm² field. The b values for *Figure 9A and Figure 10A*, *Figure 9B and Figure 10B*, *Figure 9C and Figure 10C*, *Figure 9D and Figure 10D* were 0.04, 0.08, 0.2, and 0.4, respectively. The furthest points from the central beam axis in the 2×2 and 3×3 cm² fields were ± 0.8 and ± 1.2 cm, respectively.

Discussion

The EDGE detector has an active volume of 0.019 mm^3 . In contrast, the semiflex chamber has an active volume of 0.125 cm^3 , which is over 6,000-fold that of the EDGE detector. Usually, the smaller the active volume, the higher the spatial resolution. Additionally, the severe average



Figure 6 Analysis of $\delta_{dose\%}$ with different b values.



Figure 7 A comparison of dose profiles measured by EBT3 films to those measured by either EDGE detector or semiflex chamber in the 2×2 cm² field size.

volume effect of the semiflex chamber leads to an even lower spatial resolution, particularly in the large gradient region of the dose distribution. Consistently, *Figures 4,5* have shown that larger differences were detected in the dose profile measurements at the depth of 5 cm compared to that measured at the depths of 10 and 20 cm.

It is critical to determine the b value unit used in this study to optimize between EBT3 film spatial resolution and measurement accuracy. As the field (b value) becomes smaller, the higher the contribution of noise. Therefore, measurements by EBT3 film may not achieve as high a spatial resolution as an EDGE detector. The spatial resolution, or changes in the gradient of the dose profile throughout the field, is of interest in this study. Therefore, the uncertainty ($\delta_{dose\%}$), of varying b value is shown in *Figure 6*. B values of 0.2 and 0.4 were excluded, even though the $\delta_{dose\%}$ was low, the spatial resolution was sacrificed. Within the radiation dose of 100–300 cGy, it was observed that b=0.08 showed a more



Figure 8 A comparison of dose profiles measured by EBT3 to those measured by either the EDGE detector or semiflex chamber in the 3×3 cm² field size.



Figure 9 Graphical representation of varying depth dose profile comparison of EBT3 film versus either EDGE detector (x) or semiflex chamber (o) with varying b values (the unit of analysis area): (A) b=0.04 cm, (B) b=0.08 cm, (C) b=0.2 cm, and (D) b=0.4 cm. Field size is 2×2 cm².

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Figure 10 Graphical representation of varying depth dose profile comparison of EBT3 film versus either EDGE detector (x) or semiflex chamber (o) with varying b values (the unit of analysis area): (A) b=0.04 cm, (B) b=0.08 cm, (C) b=0.2 cm, and (D) b=0.4 cm. Field size is 3×3 cm².

consistent $\delta_{doxe\%}$, signifying a greater balance between signal and noise. B value =0.04 showed excessive noise when the radiation dose was 122.6 cGy.

When the b value was fixed at 0.08, the field of analysis radiation area for EBT3 films, the EDGE detector, and the semiflex chamber were 0.0256, 0.0064, and 0.3575 cm², respectively. Among the three different measurement methods, EDGE detector achieved the highest spatial resolution.

EBT3 films shows greater flexibility in by adjusting the field size for analysis and can complement a variety of dose measurement tools. Its measurement was similar to the EDGE detector measurement when its analysis area was close to the field of analysis of the EDGE detector. Similarly, its measurement was similar to the semiflex chamber measurement when its analysis area was close to the field of analysis of the semiflex chamber. Consistently, *Figures 9,10* have shown that the differences in the dose profile measurements between EBT3 films and EDGE detector became larger as the b value increased, while the differences in the dose profile measurements between EBT3 films and the semiflex chamber reduced. This observation is because as b value increases, the spatial analysis area approaches the analysis area of semiflex chamber.

Figures 7,8 show that the does profile measurements with EBT3 films and EDGE detector were similar for the depths 5, 10, and 20 cm under the same radiation dose. This showed that EBT3 film has the ability to be correlative to EDGE detector; especially at areas where the dose profile gradient is large when compared to measurements obtained from semiflex chamber. The only exception was with the measurements on the point that was -0.8 cm from the central beam axis in the 2×2 cm² field size with the 20 cm depth. The difference in the measured dose profile with EBT3 films and EDGE detector was 4.54%, while the difference in the measured dose profile with EBT3 films and the semiflex chamber was 1.6%, which was smaller than that measured with EBT3 films and EDGE detector. This was due to inaccuracies resulting from the dose fitting equation, as the uncertainty was increased with smaller radiation doses.

Conclusions

The EDGE detector had the highest spatial resolution. Our results show that the dose profile measured at the same point with the same field sizes and at the same depth ranked from high to low were: EDGE detector, EBT3 films, and semiflex chamber. As the more accurate dose profiles measured in FFF mode led to more accurate treatment planning, using the EDGE detector was recommended instead of the currently widely used semiflex chamber to measure the dose profiles and serve as the gold standard.

By adjusting the field size, EBT3 film can offer great flexibility to complement EDGE detector, semiflex chamber or other does measurement tools.

Dose profile measured with EBT3 films showed that as one reduces the analysis area, the dose profile is more refined but also comes with greater dosimetric uncertainty, especially at lower radiation dose. Therefore, lowering the b values might not always lead to definite dose profile measurements. Our results have indicated that the optimal setting for the b value was 0.08 as it provides the desired balance between spatial resolution and uncertainty.

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Footnote

Conflicts of Interest: All authors have completed the ICMJE uniform disclosure form (available at http://dx.doi. org/10.21037/tro.2019.09.02). The authors have no conflicts of interest to declare.

Ethical Statement: The authors are accountable for all aspects of the work in ensuring that questions related to the accuracy or integrity of any part of the work are appropriately investigated and resolved.

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