



# Contrast enhanced magnetic resonance imaging–based radiomics nomogram for preoperatively predicting expression status of Ki-67 in meningioma: a two-center study

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**Background:** The aim of this study was to develop and validate a radiomics nomogram for preoperative prediction of Ki-67 proliferative index (Ki-67 PI) expression in patients with meningioma.

**Methods:** A total of 280 patients from 2 independent hospital centers were enrolled. Patients from center I were randomly divided into a training cohort of 168 patients and a test cohort of 72 patients, and 40 patients from center II served as an external validation cohort. Interoperator reproducibility test, Z-score standardization, analysis of variance (ANOVA), and least absolute shrinkage and selection operator (LASSO) binary logistic regression were used to select radiomics features, which were extracted from contrast-enhanced T1-weighted imaging (CE-T1WI) imaging. The radiomics signature for predicting Ki-67 PI expression was developed and validated using 4 classifiers including logistic regression (LR), decision tree (DT), support vector machine (SVM), and adaptive boost (AdaBoost). Finally, combined radiological characteristics with radiomics signature were used to establish the nomogram to predict the risk of high Ki-67 PI expression in patients with meningioma.

**Results:** Fourteen radiomics features were used to construct the radiomics signature. The radiomics nomogram that incorporated the radiomics signature and radiological characteristics showed excellent discrimination in the training, test, and validation cohorts with areas under the curve of 0.817 (95% CI: 0.753–0.881), 0.822 (95% CI: 0.727–0.916), and 0.845 (95% CI: 0.708–0.982), respectively. In addition, the calibration curve for the nomogram demonstrated good agreement between prediction and actual observation.

**Conclusions:** The proposed contrast enhanced magnetic resonance imaging (MRI)–based radiomics nomogram could be an effective tool to predict the risk of Ki-67 high expression in patients with meningioma.

**Keywords:** Meningioma; magnetic resonance imaging; radiomics; Ki-67

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## Introduction

Meningioma is one of the most frequent primary central nervous system (CNS) tumors (1,2). According to the 2016 World Health Organization (WHO) classification of CNS tumors, meningioma can be classified into 3 histological grades and 15 subtypes (3), among which grade I accounts for 81% to 95% of meningioma (2,4). However, the 5-year recurrence rate of grade I meningioma is more than 10% after complete resection (5,6), and some have the potential to transform into high-grade subtypes (7). In the past half century, prediction of meningioma recurrence and invasiveness has relied solely upon histological features, which, however, has proven inadequate in evaluating survival outcomes (8). Thus, it is essential to explore new auxiliary diagnostic techniques or histological markers to evaluate the complex clinical and biological behavior of meningioma (9,10). Proliferation markers include the *p53* gene, Ki-67 proliferation index (Ki-67 PI), argyrophilic nucleolar organizer regions, 5-bromo-2-deoxyuridine, and proliferating cell nuclear-antigen. Among these markers, Ki-67 PI is the most valuable, as it is expressed in all active phases of the cell cycle (G1, S, G2, M) except the G0 phase (11). Recently, its negative effects on clinical outcomes have been extensively proven for most solid tumors (12–16). Many studies have demonstrated that Ki-67 is an important surrogate marker of meningioma grade, prognosis, and malignant transformation (17–19). Telugu *et al.* reported that Ki-67 PI correlated well with increasing the histological grade and biological behavior of meningioma (17). Furthermore, it has been found that higher Ki-67 PI expression is negatively associated with survival in meningioma, with Ki-67 PI >4% being more appropriate for prognosis prediction; it has been thus highly recommended that patients with elevated expression of Ki-67 PI undergo stricter follow-up (18).

At present, the expression of Ki-67 PI in clinical practice is mainly detected through immunohistochemical (IHC) analysis of postoperative specimens. However, sampling error, delays, and the high cost of IHC analysis reduce the value of Ki-67 PI in preoperative evaluation and treatment planning of patients with meningioma (20). In contrast, radiomics, which involves analyzing the distribution and relationship of pixel or voxel gray levels in the lesion area, has been used to quantitatively assess tumor heterogeneity in more detail than has visual evaluation (21,22). It can evaluate the holistic characteristics of meningioma comprehensively, noninvasively, and in a timely manner (23). Previous studies

showed that analysis using magnetic resonance imaging (MRI)-based radiomics features perform well in predicting Ki-67 PI of CNS tumors (24,25).

Considering the above cumulatively, our study aimed to develop and validate a classifier and integrate radiological characteristics with radiomics features to construct a nomogram for preoperatively predicting Ki-67 PI expression in meningioma. The aim was to provide valuable information for predicting the intrinsic clinical and biological behavior of meningioma. The following article is presented in accordance with the TRIPOD reporting checklist (available at <https://qims.amegroups.com/article/view/10.21037/qims-22-689/rc>).

## Methods

### Patients

The study was conducted in accordance with the Declaration of Helsinki (as revised in 2013) and approved by the ethics board of the First Affiliated Hospital of Kunming Medical University (ethics No. 2021-L-6). Individual consent for this retrospective analysis was waived. The data of consecutive patients with pathologically confirmed meningioma who were hospitalized in 2 centers between June 2016 and June 2020 were reviewed. Patients were included only if they met all of the following criteria: (I) received neurosurgery treatment and diagnosed with meningioma based on pathology results, (II) underwent head MRI scanning within 1 month before neurosurgery, (III) underwent postoperative IHC analysis of Ki-67 PI, and (IV) accurate results (Ki-67 PI ≤4% was recorded as low expression, and Ki-67 PI >4% was recorded as high expression) (18,26,27). Patients were excluded if they met any of the following criteria: (I) insufficient quality of MRI images or (II) incomplete clinical or pathological information. Patients from center I were enrolled in the training and test cohort, while center II patients were enrolled in the external validation cohort.

### MRI image acquisition and evaluation

The following MRI scanners were used: center I, Philips 1.5-Tesla (Achieva, Philips, Amsterdam, The Netherlands); and center II, Siemens (Area) 1.5-Tesla (Siemens, Munich, Germany). The MRI protocol of center I was as follows: T1-weighted imaging [T1WI; repetition time/time to echo (TR/TE) =550 ms/15 ms], T2-weighted imaging (T2WI;

TR/TE =4,000 ms/100 ms), fluid-attenuated inversion recovery (FLAIR; TR/TE/TI =7,000 ms/120 ms/2,200 ms), and diffusion-weighted imaging (DWI; TR/TE =2,533 ms/94 ms, b =1,000 s/mm<sup>2</sup>); apparent diffusion coefficient (ADC) maps were automatically reconstructed and contrast enhanced T1-WI was used (CE-T1WI; TR/TE =250 ms/2.5 ms). All sequences were acquired with the following range of parameters: slice thickness =6 mm, slice spacing =1 mm, field of view (FOV) =240 mm × 240 mm, and number of excitations (NEX) =1. For contrast medium, gadopentetate Di meglumine (Gd-DTPA) was injected into the cubital vein using a high-pressure syringe at a dose of 0.2 mmol/kg and a rate of 2.0 mL/s.

Radiological characteristics were assessed randomly by 2 radiologists (YL and YHG) with more than 8 years' experience in CNS radiology. Both were blinded to the histopathological information of patients. Any disagreement was resolved through consultation.

### ***IHC analysis***

The surgical specimens were fixed in 10% buffered neutral formalin entirely sampled and embedded in paraffin, and 5-µm sections were stained with hematoxylin and eosin (HE). Ki-67 PI was recorded as the percentage of positively labeled tumor nuclei with Ki-67 monoclonal antibody per 1,000 tumor cells. Tumor grading was classified according to the 2016 WHO classification (3).

### ***Tumor segmentation and radiomics feature extraction***

The axial CE-T1WI images of all patients were imported into IBEX radiomics software (version 1.0, [http://bit.ly/IBEX\\_MDAnderson](http://bit.ly/IBEX_MDAnderson)) with the DICOM format. The tumor contours were manually delineated using outermost boundaries slice by slice. Two regions of interest (ROIs) were independently delineated by two radiologists (ZQO and YZ) and reviewed by a senior radiologist (XJS) with more than 30 years' experience in CNS radiology. Before extraction of radiomics features, resample voxel size and a Laplacian filter were used to preprocess these delineated ROIs. In total, 838 radiomics features were extracted by IBEX from 3 categories, including (I) shape and size features, (II) first-order statistics features, and (III) texture-based features, which were calculated from gray-level co-occurrence matrix (GLCM) and gray-level run-length matrix (GLRLM).

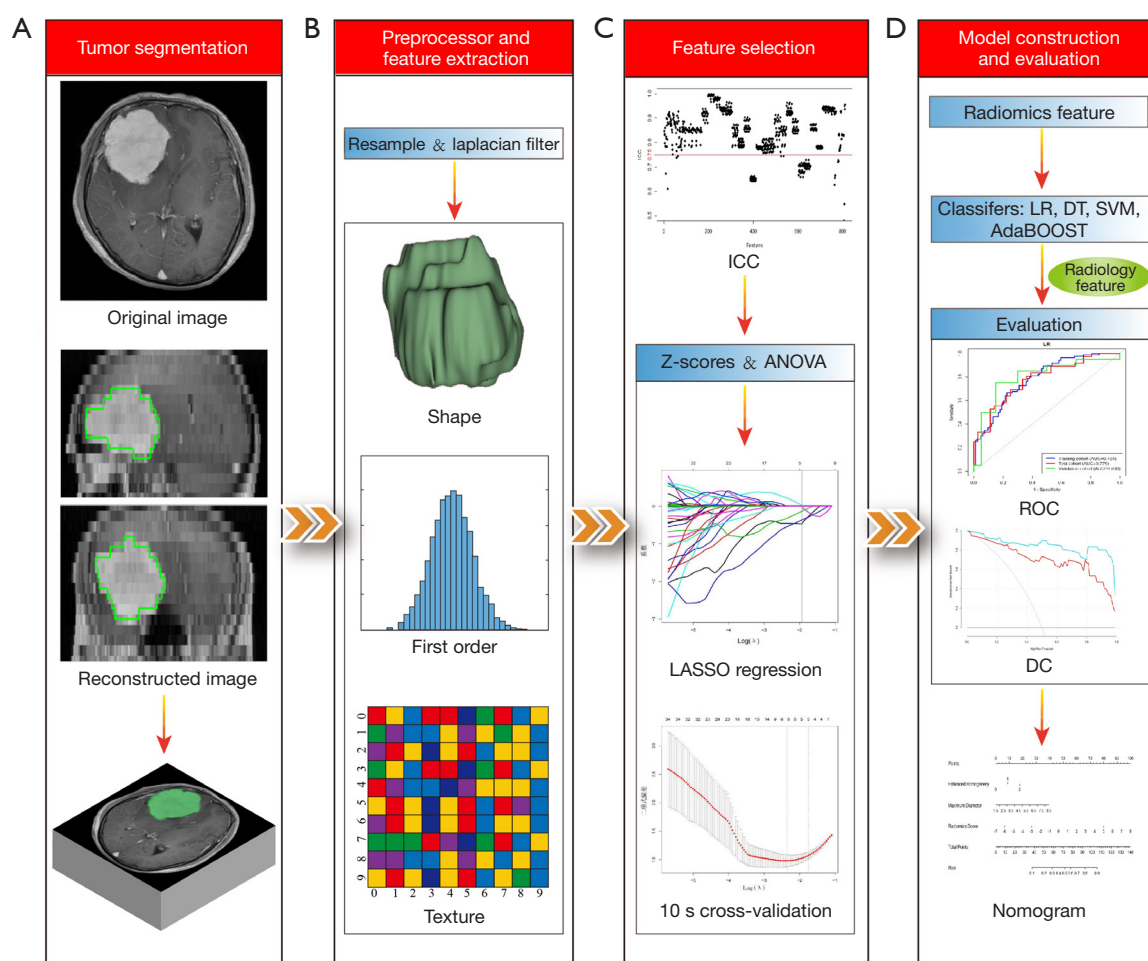
### ***Radiomics feature selection and model construction***

To avoid dimensional disarray and choose related features that made a major contribution to the predictive models, a 4-stage feature selection was performed. First, the inter-operator reproducibility of 2 ROIs was evaluated using the intraclass correlation coefficient (ICC) (28). Radiomics features with an ICC value >0.75 were categorized as good agreement with high reproducibility. Second, the radiomics features with an ICC value >0.75 were normalized using Z-scores to eliminate differences introduced due to value scales. Then, the normalized data were randomly divided into training and test cohorts using a random function with a 7:3 ratio. Third, the radiomics features of the training cohort were preliminarily screened using 1-way analysis of variance (ANOVA). Finally, a least absolute shrinkage and selection operator (LASSO) binary logistic regression and 10-fold cross-validation were conducted to select the effective radiomics features with nonzero coefficients in the training cohort.

After the above steps were conducted, the features selected by the training cohort were entered into the following classifiers to construct a radiomics signature: logistic regression (LR), decision tree (DT), support vector machine (SVM), and adaptive boost (AdaBoost). Additionally, the 4 classifiers were internally validated in the test cohort. In addition, radiological characteristics with significant differences were combined with the radiomics signature to construct a combined model. Based on the combined model, a radiomics nomogram was constructed to preoperatively quantify the risk of Ki-67 high expression in patients with meningioma. The formula of the radiomics score was fitted using the linear combination of the selected features, which were weighted by their LASSO coefficients. For the specific methods, refer to Wu *et al.* (29). Finally, the radiomics score was included in the nomogram to calculate the risk of high expression Ki-67 in patients with meningioma.

### ***External validation and model evaluation***

The data obtained from center II were normalized with Z-scores to perform external validation of the above models. Receiver operating characteristic (ROC), area under curve (AUC), sensitivity, specificity, and accuracy were used to evaluate the performances of the prediction models. Moreover, a decision curve (DC) was used to



**Figure 1** Study flowchart. (A) The ROI of Meningioma was delineated in contrast-enhanced T1-weighted imaging. (B) After image preprocessing, 3 categories of radiomics features were extracted from the ROI. (C) Four selection steps were applied to all extracted radiomics features. (D) A final prediction model was constructed by incorporating both a radiomics and a radiological signature; a receiver operating curve and decision curve were generated for further statistical analyses, and a combined nomogram was adopted to present the outcomes of prediction to achieve clinical usefulness. ROI, region of interest; ICC, intraclass correlation coefficient; LR, logistic regression; DT, decision tree; SVM, support vector machine; AdaBoost, adaptive boost; ANOVA, analysis of variance; ROC, receiver operating characteristic; LASSO, least absolute shrinkage and selection operator; DC, decision curve.

compare the overall net benefits between the radiology signature, radiomics signature, and the combined model. A calibration curve (CC) was used to evaluate the reliability of the nomogram.

The workflow is shown in *Figure 1*.

### Statistical analysis

The sample size of our study was determined using binormal

ROC curve analysis, which was performed using diagnostic accuracy studies in PASS software (version 15.0; NCSS LLC, Kaysville, UT, USA; <https://www.ncss.com>). Statistical analysis was performed using SPSS software (version 23.0; IBM Corp, Armonk, NY, USA) and the R software package (version 4.0.2; The R Foundation for Statistical Computing, Vienna, Austria; <https://www.r-project.org>). Differences in clinical characteristics were assessed by *t*-test, chi-squared test, or Fisher exact test, as appropriate, and a 2-sided P value

**Table 1** Clinical and pathological characteristics

| Characteristics          | Training cohort |           |            |         | Test cohort |            |            |         |
|--------------------------|-----------------|-----------|------------|---------|-------------|------------|------------|---------|
|                          | Ki-67≤4%        | Ki-67>4%  | $t/\chi^2$ | P value | Ki-67≤4%    | Ki-67>4%   | $t/\chi^2$ | P value |
| Gender                   |                 |           | 0.544      | 0.461   |             |            | 0.071      | 0.789   |
| Male                     | 21 (25.0)       | 17 (20.2) |            |         | 9 (25.0)    | 10 (27.8)  |            |         |
| Female                   | 63 (75.0)       | 67 (79.8) |            |         | 27 (75.0)   | 26 (72.2)  |            |         |
| Age (years)              | 52.8±11.4       | 52.6±11.6 | −0.067     | 0.947   | 52.2±11.9   | 50.5±15.0  | 0.549      | 0.585   |
| Ki-67 PI (%)             | 1.82±0.81       | 7.41±5.74 | −6.886     | <0.01   | 2.04±0.83   | 10.43±8.55 | −4.683     | <0.001  |
| Pathological grade (WHO) |                 |           | 11.087     | 0.002   |             |            | 8.824      | 0.011   |
| I                        | 76 (90.5)       | 59 (70.2) |            |         | 33 (91.7)   | 23 (63.9)  |            |         |
| II                       | 8 (9.5)         | 23 (27.4) |            |         | 3 (8.3)     | 8 (22.2)   |            |         |
| III                      | 0 (0)           | 2 (2.4)   |            |         | 0 (0)       | 5 (13.9)   |            |         |

Numerical data are presented as mean ± standard deviation, categorical data as numbers (%). PI, proliferation index; WHO, World Health Organization.

<0.05 was considered statistically significant.

## Results

### *Clinical, pathological, and radiological characteristics of patients*

A total of 240 eligible patients, including 120 patients with high Ki-67 expression and 120 patients with low Ki-67 expression were enrolled in our study. Among these patients, 168 cases were randomized to the training cohort, and the remaining 72 cases were enrolled in the test cohort. As is shown in *Table 1*, except for expression of Ki-67 PI ( $P<0.001$ ) and postoperative pathological grade ( $P=0.002$  and  $P=0.011$ , respectively), no significant differences were found between groups regarding age and gender in either cohort. *Table 2* shows the radiological characteristic data; only enhanced homogeneity showed significant differences in both the training and test cohorts ( $P=0.008$  and  $P=0.009$ , respectively). The above results demonstrated that pathological grade was positively correlated with a high expression of Ki-67, which is consistent with results of previous studies (18,26,30–32), and patients with meningioma with higher Ki-67 PI expression were more likely to exhibit less homogeneous/heterogeneous enhancement on MRI.

### *Analysis of radiomics feature*

In total, 838 radiomics features were extracted from the CE-

T1WI image. Among these, 783 radiomics features were regarded as stable features after being assessed with ICC. In all, 622 radiomics features showed significant differences between the high and low expression groups according to ANOVA. These features were then imported into the LASSO regression with 10-fold cross-validation to select the most important features (*Figure 2*). Finally, 14 radiomics features with nonzero coefficients were selected (*Table 3*).

### *Predictive performance of the models*

The LR classifier demonstrated the best predictive performance in the training, test, and validation cohorts, with an AUC of 0.784, 0.779, and 0.800, respectively. The ROC and predictive performances of the 4 classifiers are shown in *Figure S1* and *Table 4*. The odds ratio (OR) and P values of the 14 radiomics features are shown in *Table S1*. The combined model achieved the highest predictive performance in the training, test, and validation cohorts, with an AUC of 0.817, 0.822, and 0.845, respectively (*Figure 3* and *Table 5*). Moreover, the DCs showed that the combined model consistently exhibited higher overall net benefits than did conventional radiological characteristics in the training (*Figure 3*), test, and validation cohorts (*Figure S2*).

With the coefficients weighted by the LR algorithm, a radiomics score was calculated for each patient as follows: radiomics score =  $16.884 + 0.962 \times X_1 - 3.176 \times X_2 - 2.661 \times X_3 - 1.418 \times X_4 - 7.242 \times X_5 - 0.418 \times X_6 + 0 \times X_7 - 0.922$



**Table 2** Radiological characteristics

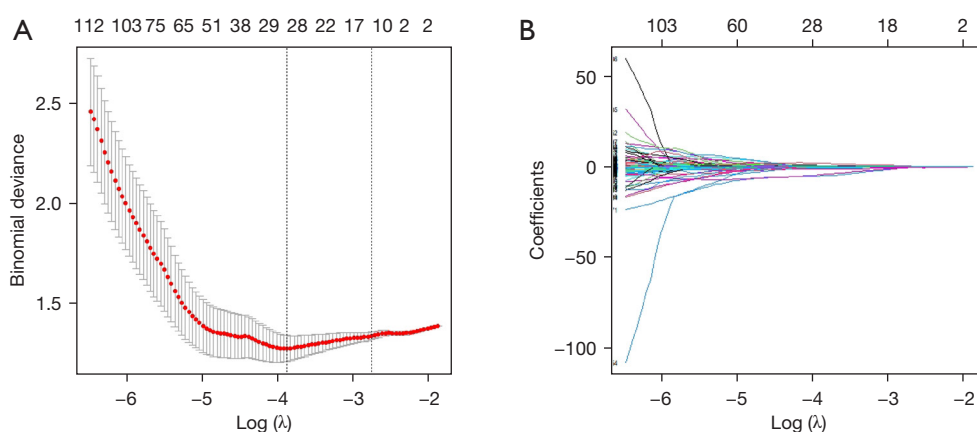
| Characteristics          | Training cohort |           |            |         | Test cohort |           |            |         |
|--------------------------|-----------------|-----------|------------|---------|-------------|-----------|------------|---------|
|                          | Ki-67≤4%        | Ki-67>4%  | $t/\chi^2$ | P value | Ki-67≤4%    | Ki-67>4%  | $t/\chi^2$ | P value |
| Number of lesions        |                 |           | 1.701      | 0.192   |             |           | 0.860      | 0.354   |
| Single                   | 81 (96.4)       | 77 (91.7) |            |         | 32 (88.9)   | 35 (97.2) |            |         |
| Multiple                 | 3 (3.6)         | 7 (8.3)   |            |         | 4 (11.1)    | 1 (2.8)   |            |         |
| Location                 |                 |           | 6.655      | 0.225   |             |           | 5.461      | 0.242   |
| Cerebral convexity       | 55 (65.5)       | 62 (73.8) |            |         | 22 (61.1)   | 17 (47.3) |            |         |
| Deep brain               | 2 (2.4)         | 3 (3.6)   |            |         | 0 (0)       | 0 (0)     |            |         |
| Cerebellar hemisphere    | 11 (13.1)       | 6 (7.1)   |            |         | 1 (2.8)     | 3 (8.3)   |            |         |
| Peri skull base          | 6 (7.1)         | 9 (10.7)  |            |         | 8 (22.2)    | 8 (22.2)  |            |         |
| Cerebellopontine angular | 9 (10.7)        | 3 (3.6)   |            |         | 5 (13.9)    | 4 (11.1)  |            |         |
| Lateral ventricle        | 1 (1.2)         | 1 (1.2)   |            |         | 0 (0)       | 4 (11.1)  |            |         |
| Shape                    |                 |           | 0.867      | 0.351   |             |           | 0.000      | 1.000   |
| Round-like               | 50 (59.5)       | 44 (52.4) |            |         | 20 (55.6)   | 20 (55.6) |            |         |
| Irregular                | 34 (40.5)       | 40 (47.6) |            |         | 16 (44.4)   | 16 (44.4) |            |         |
| Peritumoral edema        |                 |           | 0.902      | 0.337   |             |           | 0.900      | 0.343   |
| Yes                      | 50 (59.5)       | 56 (66.7) |            |         | 18 (50.0)   | 22 (61.1) |            |         |
| No                       | 34 (40.5)       | 28 (33.3) |            |         | 18 (50.0)   | 14 (38.9) |            |         |
| Enhanced degree          |                 |           | 0.256      | 0.613   |             |           | 0.514      | 0.473   |
| Mild/moderate            | 1 (1.2)         | 3 (3.6)   |            |         | 0 (0)       | 2 (5.6)   |            |         |
| Marked                   | 83 (98.8)       | 81 (96.4) |            |         | 36 (100.0)  | 34 (94.4) |            |         |
| Enhanced homogeneity     |                 |           | 9.665      | 0.008   |             |           | 9.533      | 0.009   |
| Homogeneous              | 55 (65.5)       | 37 (44.0) |            |         | 25 (69.4)   | 14 (38.8) |            |         |
| Less homogeneous         | 19 (22.6)       | 23 (27.4) |            |         | 9 (25.0)    | 11 (30.6) |            |         |
| Heterogeneous            | 10 (11.9)       | 24 (28.6) |            |         | 2 (5.6)     | 11 (30.6) |            |         |
| Diffusion limited        |                 |           | 4.550      | 0.033   |             |           | 0.000      | 1.000   |
| Yes                      | 8 (9.5)         | 18 (21.4) |            |         | 2 (5.6)     | 3 (8.3)   |            |         |
| No                       | 76 (90.5)       | 66 (78.6) |            |         | 34 (94.4)   | 33 (91.7) |            |         |
| Dural tail sign mater    |                 |           | 1.532      | 0.216   |             |           | 0.223      | 0.637   |
| Yes                      | 49 (58.3)       | 41 (48.8) |            |         | 20 (55.6)   | 18 (50.0) |            |         |
| No                       | 35 (41.6)       | 43 (51.2) |            |         | 16 (44.4)   | 18 (50.0) |            |         |
| Maximum diameter         | 3.66±1.76       | 4.61±1.81 | -3.446     | 0.001   | 3.82±1.57   | 4.26±1.52 | -1.226     | 0.224   |

Numerical data are presented as mean ± standard deviation, categorical data as numbers (%).

$\times X8 + 0.717 \times X9 + 2.355 \times X10 + 0 \times X11 + 0.289 \times X12 + 0 \times X13 - 5.429 \times X14$ . A *t*-test confirmed that there were significant differences between Ki-67 PI high expression and low expression of the radiomics score in each cohort (Figure 4).

### Development and validation of nomogram

The above analysis revealed that the radiomics score and enhanced homogeneity were significant predictive factors



**Figure 2** LASSO regression model. (A) Tuning parameter  $\log(\lambda)$  selection in the LASSO regression used 10-fold cross-validation via the minimum criterion. Dotted vertical lines were drawn at the optimal values by using the minimum criterion and the 1 standard error of the minimum criterion, and a value  $\lambda$  of 0.063 was chosen. (B) LASSO coefficient profiles, displaying 622 radiomics features of contrast-enhanced T1-weighted imaging. A coefficient profile plot was produced against the  $\log(\lambda)$  sequence. Finally, 14 radiomics features with nonzero coefficients were selected. LASSO, least absolute shrinkage and selection operator.

**Table 3** Characteristics of radiomics features

| Numbers | Sequence | Feature type              | Feature name                        | LASSO coefficient |
|---------|----------|---------------------------|-------------------------------------|-------------------|
| X1      | CE-T1WI  | Shape                     | Max 3D diameter                     | 0.382             |
| X2      | CE-T1WI  | Shape                     | Spherical disproportion             | -0.423            |
| X3      | CE-T1WI  | Shape                     | Sphericity                          | 0.058             |
| X4      | CE-T1WI  | Gradient orient histogram | 5th percentile                      | -0.133            |
| X5      | CE-T1WI  | Intensity direct          | Local entropy max                   | -0.497            |
| X6      | CE-T1WI  | Intensity direct          | 10th percentile                     | -0.037            |
| X7      | CE-T1WI  | Intensity histogram       | 10th percentile                     | -2.025e-16        |
| X8      | CE-T1WI  | Intensity histogram       | 10th percentile area                | -0.324            |
| X9      | CE-T1WI  | GLCM                      | 333-4 correlation                   | 0.009             |
| X10     | CE-T1WI  | GLCM                      | 0-1 correlation                     | 0.548             |
| X11     | CE-T1WI  | GLCM                      | 180-1 correlation                   | 1.993e-14         |
| X12     | CE-T1WI  | GLCM                      | 270-7 correlation                   | -0.419            |
| X13     | CE-T1WI  | GLCM                      | 45-7 difference entropy             | -1.686e-14        |
| X14     | CE-T1WI  | GLRLM                     | 0 short run low gray-level emphasis | -0.661            |

CE-T1WI, contrast-enhanced T1-weighted imaging; GLCM, gray-level co-occurrence matrix; GLRLM, gray-level run-length matrix; LASSO, least absolute shrinkage and selection operator.

of Ki-67 expression in meningioma. The odds ratio (OR) and P values of the 2 variables are shown in Table S2. To facilitate the use in clinical practice, a nomogram was constructed for the combined model (Figure 5).

In addition, the CCs of the radiomics nomogram demonstrated a good agreement between the predictive and actual performance of the Ki-67 expression status in each cohort (Figure 5).

**Table 4** Predictive performance of 4 classifiers

| Classifiers | Cohort     | AUC (95% CI)        | Sensitivity | Specificity | Accuracy |
|-------------|------------|---------------------|-------------|-------------|----------|
| LR          | Training   | 0.784 (0.716–0.852) | 69.0%       | 69.0 %      | 69.0%    |
|             | Test       | 0.779 (0.673–0.886) | 63.9%       | 75.0%       | 69.4%    |
|             | Validation | 0.800 (0.651–0.949) | 75.0%       | 80.0%       | 77.5%    |
| DT          | Training   | 0.839 (0.781–0.898) | 78.6%       | 79.8%       | 79.2%    |
|             | Test       | 0.605 (0.477–0.733) | 58.3%       | 58.3%       | 58.3%    |
|             | Validation | 0.764 (0.614–0.913) | 60.0%       | 85.0%       | 72.5%    |
| SVM         | Training   | 0.998 (0.994–1.000) | 96.4%       | 95.2%       | 95.5%    |
|             | Test       | 0.769 (0.648–0.891) | 61.1%       | 75.0%       | 68.1%    |
|             | Validation | 0.765 (0.601–0.929) | 50.0%       | 95.0%       | 72.5%    |
| AdaBoost    | Training   | 0.732 (0.667–0.797) | 61.9%       | 84.5%       | 73.2%    |
|             | Test       | 0.444 (0.333–0.556) | 75.0%       | 35.0%       | 55.0%    |
|             | Validation | 0.450 (0.305–0.595) | 75.0%       | 35.0%       | 55.0%    |

AdaBoost, adaptive boost; AUC, area under curve; CI, confidence interval; DT, decision tree; LR, logistic regression; SVM, support vector machine.

## Discussion

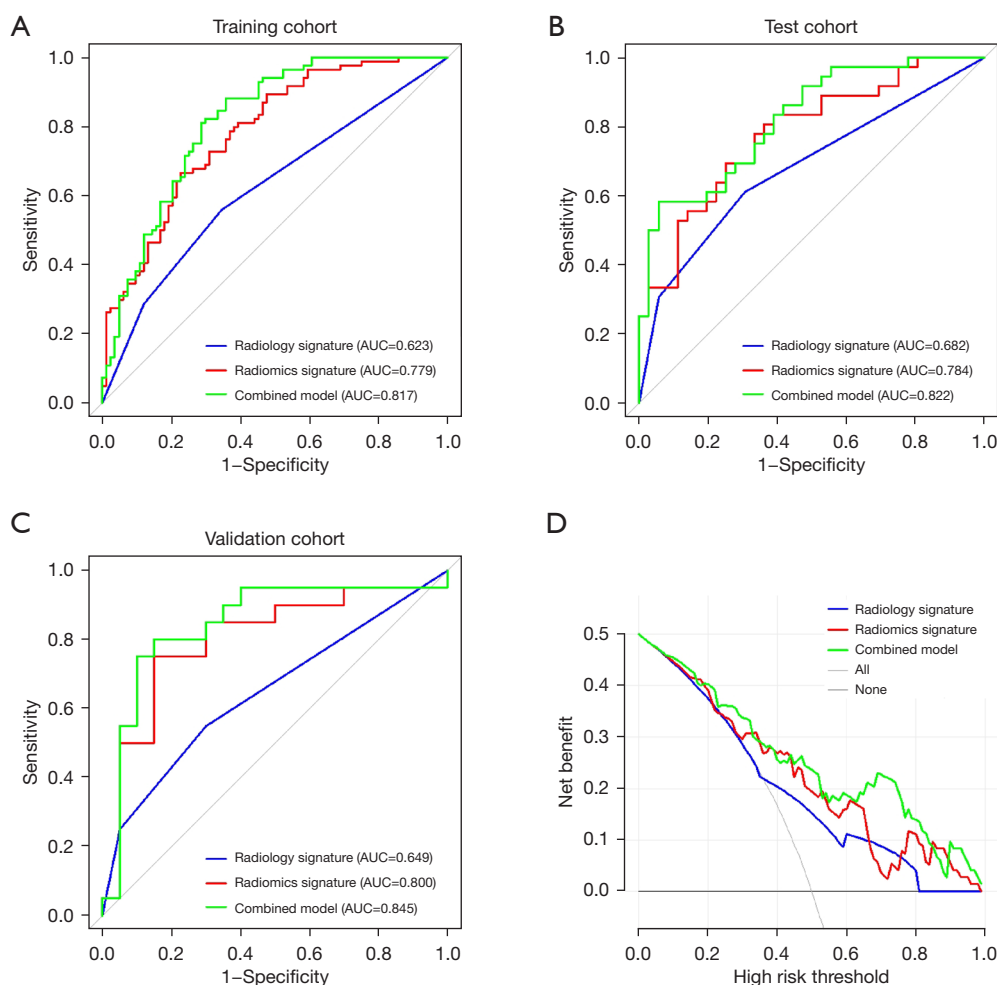
In this study, we found the CE-T1WI-based radiomics features were predictive of Ki-67 expression in patients with meningioma. Subsequently, we developed and validated a radiomics nomogram, which combined a radiomics signature with radiological features to achieve higher sensitivity and accuracy than have previous models for individualized prediction of Ki-67 status (33).

The status of Ki-67 expression is recognized as a complementary factor, which reflects the biological behavior of meningioma. Preoperative assessment of Ki-67 expression can provide additional information for clinical decision-making (17–19,30). Previous studies have confirmed that using 4% as the cutoff value of Ki-67 in patients with meningioma can predict prognosis (18,26,27). However, since evaluation of Ki-67 is easily influenced by tumor heterogeneity, the whole specimen, and not only the core biopsy specimen, must be evaluated and correlated with mitotic count (31). A related study showed that the apparent diffusion coefficient (ADC) value of DWI was negatively correlated with Ki-67 level in meningioma (34). In another study, the metric kurtosis (MK) and radial kurtosis (RK) values of diffusion kurtosis imaging (DKI) were positively correlated with the Ki-67 level in meningioma (32). It appears that these quantitative parameters can be used as

imaging biomarkers for predicting the expression of Ki-67 PI in meningioma. However, functional MRI sequences are not commonly used in clinical practice and merely provide a few quantitative parameters. In contrast, radiomics analysis cannot only extract thousands of quantitative radiomics features from routinely acquired images but can also evaluate the biological behavior of tumors in a timely and noninvasive manner (35,36).

Fourteen effective radiomics features were selected to construct classification models in this study. The correlations between the selected quantitative radiomics features and Ki-67 expression status can be interpreted on the basis of the biological behavior of tumors (37). Among the selected features, 3 were related to shape and size features because higher Ki-67 PI means the faster growth of tumors (33,38). In addition, 5 features were first-order statistical features, including entropy and percentile. Entropy, as one of the most representative parameters of tumor heterogeneity, can reflect the unpredictability of the information content in images (39). In general, entropy is positively correlated with signal dispersion, and the more scattered the tumor signals are, the stronger the uncertainty of the signals and the higher the entropy value in the ROI of the tumor (40). Entropy can make up for the deficiency of the resolution of the human eyes, which is not sufficiently high for identifying tumor heterogeneity in CE-





**Figure 3** ROCs of the radiology signature (blue line), the radiomics signature (red line), and the combined model (green line) in the training (A), test (B), and validation (C) cohorts, respectively. (D) Decision curve for 3 models in the training cohort. The y-axis indicates the net benefit; the x-axis indicates the threshold probability. For differentiating the high expression of Ki-67 from low expression in meningioma, the combined model (green line) had a higher overall net benefit than did the radiology model (blue line) and simple diagnoses such as all Ki-67 $\leq$ 4% patients (gray line) or all Ki-67 $>$ 4% patients (black line) across the full range of conceivable threshold probabilities. AUC, area under curve; ROC, receiver operating characteristic curve.

T1WI images (41). The remaining features are texture-based features, including GLCM and GLRLM. As the second- or higher-order features pairwise relations between 2 or multi-neighboring pixels, GLCM and GLRLM can provide better results (42). It is conceivable that 2 kinds of meningioma with different Ki-67 expression statuses have a similar distribution of intensities with different spatial interrelationships. In such a situation, second- or higher-order features may be the preferred predictive factors.

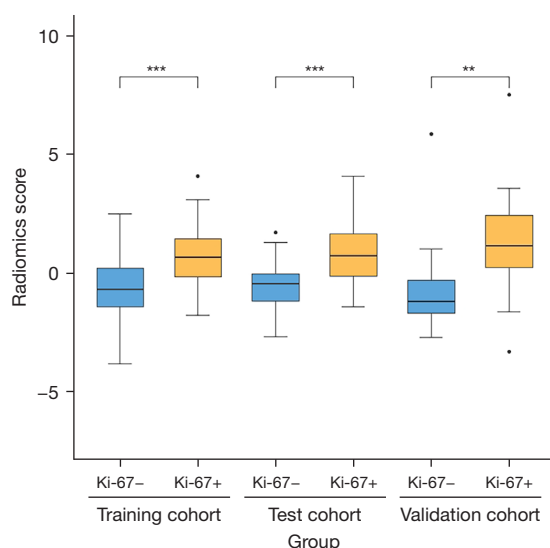
Based on the selected radiomics features, we constructed and validated the radiomics models to predict the expression

status of Ki-67 in meningioma. Among the 4 radiomics models, the LR-based model was superior at predicting status of Ki-67 expression with AUCs of 0.779 and 0.800 in the test cohort (internal validation) and validation cohort (external validation), respectively. In a recent study, a multiparametric MRI-based radiomics model was established to predict the Ki-67 expression of meningioma. This multiparametric model achieved an excellent performance in both the training and internal validation cohorts, with AUCs of 0.84 and 0.83, respectively (33). However, the robustness of the selected radiomics features

**Table 5** Predictive performance of 3 models

| Models    | Cohort     | AUC (95% CI)        | Sensitivity | Specificity | Accuracy |
|-----------|------------|---------------------|-------------|-------------|----------|
| Radiology | Training   | 0.623 (0.547–0.699) | 56.0%       | 65.4%       | 60.7%    |
|           | Test       | 0.682 (0.571–0.794) | 61.1%       | 69.4%       | 65.3%    |
|           | Validation | 0.649 (0.495–0.802) | 55.0%       | 70.0%       | 62.5%    |
| Radiomics | Training   | 0.784 (0.716–0.852) | 69.0%       | 69.0%       | 69.0%    |
|           | Test       | 0.779 (0.673–0.886) | 63.9%       | 75.0%       | 69.4%    |
|           | Validation | 0.800 (0.651–0.949) | 75.0%       | 80.0%       | 77.5%    |
| Combined  | Training   | 0.817 (0.753–0.881) | 79.8%       | 71.4%       | 75.6%    |
|           | Test       | 0.822 (0.727–0.916) | 80.6%       | 75.0%       | 77.8%    |
|           | Validation | 0.845 (0.708–0.982) | 75.0%       | 85.0%       | 80.0%    |

AUC, area under curve; CI, confidence interval.

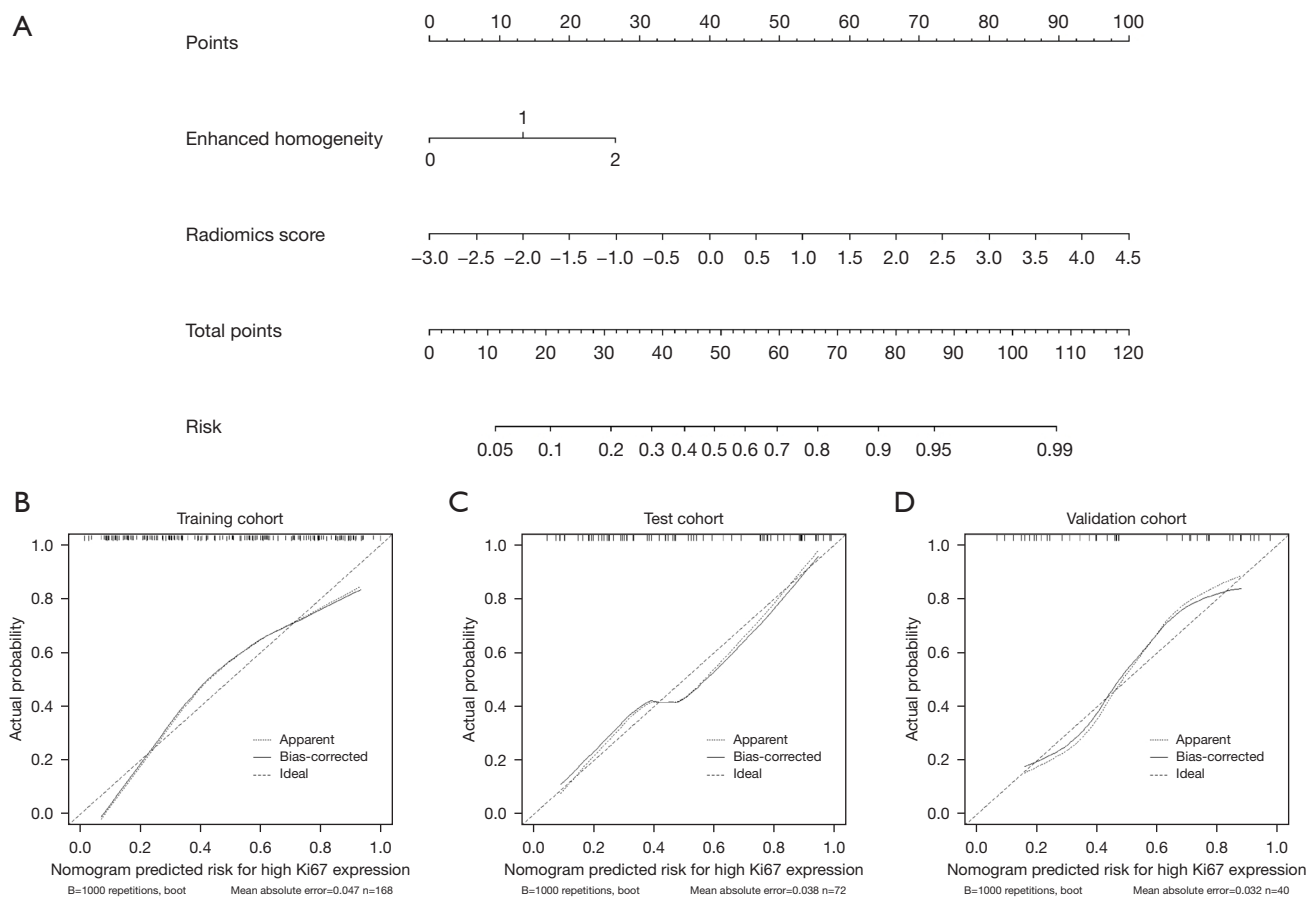


**Figure 4** A *t*-test showed significant differences in the radiomics scores between the Ki-67+ and Ki-67- groups in the training, test, and validation cohorts (training cohort:  $0.630 \pm 1.097$ , *vs.*  $-0.634 \pm 1.175$ ,  $P < 0.001$ ; test cohort:  $0.722 \pm 1.267$  *vs.*  $-0.484 \pm 0.972$ ,  $P < 0.001$ ; validation cohort:  $1.232 \pm 2.270$  *vs.*  $-0.763 \pm 1.867$ ,  $P = 0.004$ ); considering all the data, the radiomics scores were significantly higher in the Ki-67+ group than in the Ki-67- group; \*\*,  $P < 0.01$ ; \*\*\*,  $P < 0.001$ .

and the generalization of the predictive model have not been proven due to a lack of external verification. In contrast, our result of external validation demonstrated that the predictive model established has a good stability and is valuable for preliminarily generalization. Furthermore,

a previous study suggested that multiparametric MRI images can provide more radiomics features and achieve a better performance in the predictive model (33). Therefore, we extracted numerous radiomics features from multiparametric MRI images, including T1WI, T2WI, FLAIR, ADC, and CE-T1WI, to construct relative models for predicting Ki-67 expression in the pre-experimental setting. Unfortunately, the results showed that performances of the multiparametric MRI-based models were not as good as that of a CE-T1WI-based model even though we tried ANOVA, max-relevance, min-redundancy (mRMR), and LASSO regression to reduce the dimension of radiomics features. The main reason for this may be that too many radiomics features extracted from the multiparametric images led to poor fitting of the classifiers. Additionally, a multiparametric model requires patients to undergo additional MRI examinations, which could increase patients' economic burden and hinder clinical practice (33,43). By contrast, our study demonstrated that the fewer radiomics features were included from CE-T1WI images, the better the efficacy was for predicting KI-67 expression in meningioma.

To further improve the accuracy and practical value of our model, we combined the radiomics signature with conventional radiological characteristics to construct a nomogram. Interestingly, the conventional radiological characteristic formed a good fit with the radiomics signature, and the AUCs of the combined model rose to 0.822 and 0.845 in the test and validation cohorts, respectively. It has been suggested that enhanced homogeneity could reflect the degree of damage to the blood–brain barrier and identify

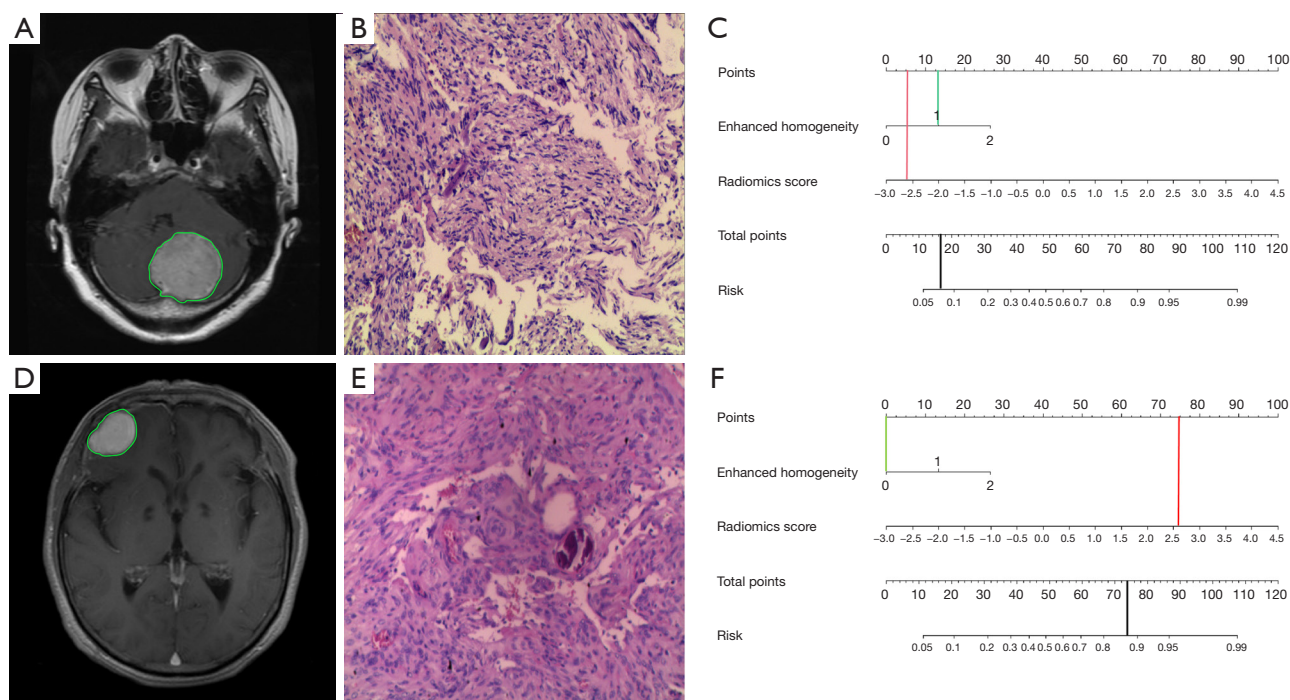


**Figure 5** Development and validation of the nomogram. (A) The radiomics nomogram based on the training cohort. Calibration curves for the radiomics nomogram in the training (B), test (C), and validation (D) cohorts. The solid line represents the ideal reference line that predicts Ki-67 expression status and corresponds to the actual outcome, the short-dashed line represents the apparent prediction of the nomogram, and the 45° diagonal dotted line represents an ideal evaluation. All 3 calibration curves showed similar trends, and the actual probability corresponded closely to the predictive probability of the radiomics nomogram.

the heterogeneity of meningioma (42) in similar fashion to selected radiomics features. Compared with a previous study (44), the nomogram we established had a higher sensitivity (0.75 *vs.* 0.31, respectively) and a higher accuracy (0.80 *vs.* 0.56, respectively). In addition, this previous study was limited to predicting the status of Ki-67 of I grade meningioma (33), while the internal and external validations of the present nomogram showed that it has good predictive accuracy for Ki-67 status for various meningioma grades. Finally, the visual and quantitative prediction of Ki-67 expression was assessed using logistic regression to weight 2 predictors, and the usage of the nomogram is shown in Figure 6.

There are several limitations to our study. First, the

design was retrospective and therefore had potential bias, and so additional studies that can prospectively validate our radiomics signature are needed. Second, we only validated whether the 1.5-Tesla-based model could be suitably applied in different machines (other 1.5-Tesla MR scanners) but did not validate different field strengths (3.0-Tesla). Third, we only constructed the radiomics signature based on CE-T1WI images due to the existence of overfitting, and further studies should address poor fitting to obtain better predictive effectiveness based on multiparametric images. Finally, the present study included only a relatively small number of participants enrolled from only 2 centers. To confirm the generalizability and the stability of the predictive model, future studies should be multicentered in



**Figure 6** Examples of using the nomogram to predict the individual risk of high Ki-67 expression in meningioma by manually placing straight lines across the diagram. (A-C) A 70-year-old female with cerebellum meningioma. CE-T1WI showed a tumor with less homogeneous enhancement (green line on the “Points” scale =12 points); the radiomics score was -2.7 (red line on the “Points” scale =5 points). The above 2 “Points” were added to obtain total points (12+5=17 points). The graph revealed that the risk of Ki-67 high expression turned out to be about 8% (low risk) via the drawing of a black line on the “Total points” scale. (B) Postoperative immunohistochemistry proved the Ki-67 PI of this patient was less than 1% (HE,  $\times 100$ ). (D-F) A 50-year-old female with right frontal meningioma. The tumor exhibits homogeneous enhancement in CE-T1WI (green line on the “Points” scale =0 point); the radiomics score was 2.6 (red line on the “Points” scale =75 points). A total of 75 points was obtained. The risk of high Ki-67 expression was about 88% (extremely high risk). (E) Postoperative immunohistochemistry proved the Ki-67 PI of this patient was about 5% (HE,  $\times 100$ ); CE-T1WI, contrast-enhanced T1-weighted imaging; HE, hematoxylin and eosin staining.

design and recruit larger samples (35,45).

In conclusion, the CE-T1WI-based radiomics nomogram is a valuable reference tool for the preoperative assessment of cell proliferation during the onset of meningioma. It can accurately and robustly predict high Ki-67 expression in meningioma and provide supplementary information for accurate medical treatment and clinical decisions. However, extensive multicenter validations of the proposed approach are required prior to clinical application.

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## Footnote

**Reporting Checklist:** The authors completed the TRIPOD reporting checklist. Available at <https://qims.amegroups.com/article/view/10.21037/qims-22-689/rc>

**Conflicts of Interest:** All authors have completed the ICMJE uniform disclosure form (available at <https://qims.amegroups.com/article/view/10.21037/qims-22-689/coif>). The authors have no other conflicts of interest to declare.

**Ethical Statement:** The authors are accountable for all aspects of the work in ensuring that questions related to the accuracy or integrity of any part of the work are appropriately investigated and resolved. The study was conducted in accordance with the Declaration of Helsinki

(as revised in 2013). This study was approved by the Ethics Committee of the First Affiliated Hospital of Kunming Medical University (No. 2021-L-6). Written informed consent was waived by the institutional review board.

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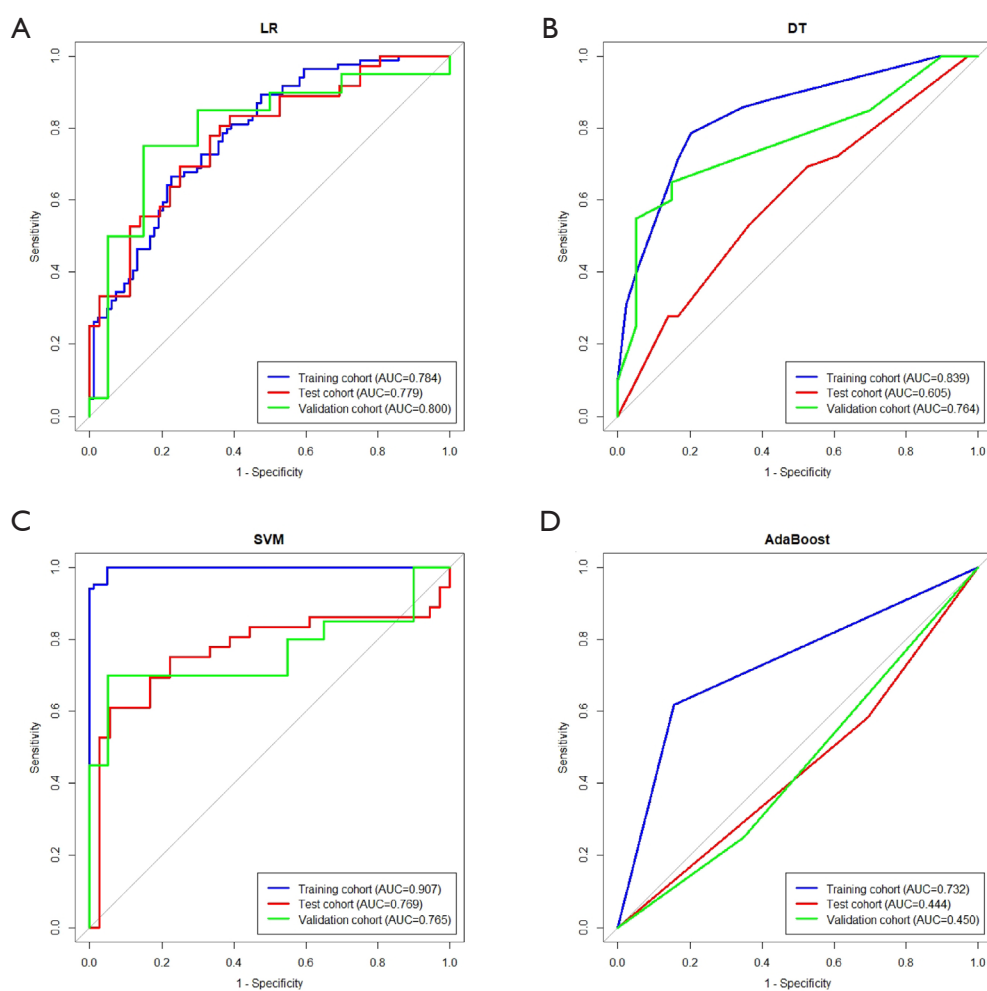
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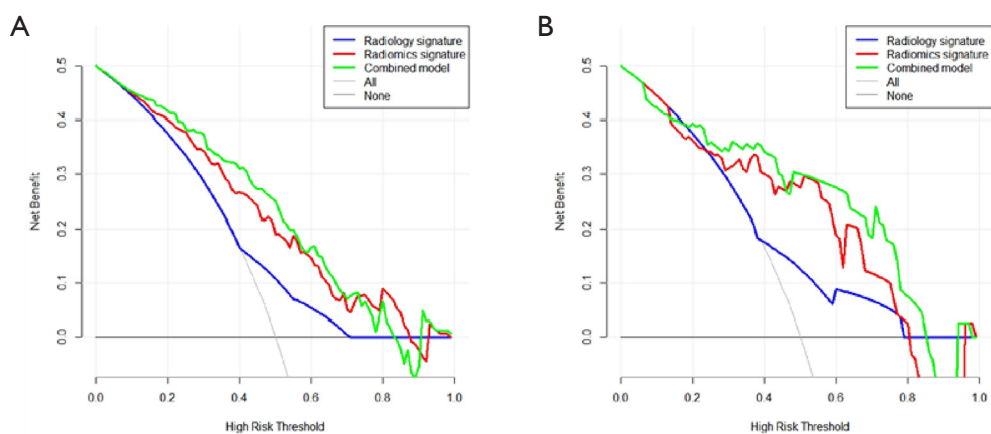
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**Figure S1** The ROC curves of LR (A), DT (B), SVM (C), and AdaBoost (D) in the training cohort (blue line), test cohort (red line), and validation cohort (green line), respectively. AdaBoost, adaptive boost; AUC, area under curve; DT, decision tree; LR, logistic regression; ROC, receiver operating characteristic curve; SVM, support vector machine.



**Figure S2** The decision curve of the 3 models in the test (A) and validation (B) cohorts.

**Table S1** The logistic regression parameters of the radiomics features

| Numbers | OR (95% CI)            | Z value | P value |
|---------|------------------------|---------|---------|
| X1      | 2.618 (0.540-2.701)    | 1.195   | 0.232   |
| X2      | 0.042 (0.000-266.155)  | -0.711  | 0.477   |
| X3      | 0.070 (0.000-1124.381) | -0.538  | 0.590   |
| X4      | 0.242 (0.045-1.294)    | -1.659  | 0.097   |
| X5      | 0.001 (0.000-1.938)    | -1.796  | 0.073   |
| X6      | 0.658 (0-5.655e+56)    | -0.006  | 0.995   |
| X7      | NA                     | NA      | NA      |
| X8      | 0.398 (0-4.481e+55)    | -0.014  | 0.989   |
| X9      | 2.048 (0.956-4.388)    | 1.844   | 0.065   |
| X10     | 10.535 (0.232-478.233) | 1.210   | 0.226   |
| X11     | NA                     | NA      | NA      |
| X12     | 1.335 (0.186-9.571)    | 0.288   | 0.774   |
| X13     | NA                     | NA      | NA      |
| X14     | 0.004 (0.000-1.318)    | -1.865  | 0.062   |

CI, confidence interval; NA, not applicable; OR, odds ratio.

**Table S2** The logistic regression parameters of the nomogram variables

| Variables            | OR (95% CI)         | Z value | P value |
|----------------------|---------------------|---------|---------|
| Radiomics score      | 2.923 (2.031-4.208) | 5.771   | <0.001  |
| Enhanced homogeneity | 2.287 (1.413-3.701) | 3.369   | 0.001   |

CI, confidence interval; OR, odds ratio.