

# Quantification of epicardial fat volume using low-dose cardiac scan in patients with low calcium score

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**Background:** We investigated the accuracy of quantifying epicardial adipose tissue volume (EATV) using low-dose cardiac scan (EATV<sub>cardiac scan</sub>) and evaluated its clinical utility in predicting coronary heart disease in patients with low or mild calcification.

**Methods:** In total, 204 patients with clinical symptoms of coronary heart disease and coronary artery calcium score (CACS) of <100 AU were enrolled in this retrospective study. After obtaining EATV<sub>cardiac scan</sub> and EATV measured using computed tomography angiography (EATV<sub>CTA</sub>), the agreement between the two measurements was evaluated using Pearson correlation coefficient and Bland-Altman analysis. Multivariate logistic regression was used to analyze the utility of EATV in predicting plaque and vulnerable plaque. Receiver operating characteristic curves were constructed.

**Results:** The mean EATV<sub>cardiac scan</sub> (101.51±41.57 cm<sup>3</sup>) and EATV<sub>CTA</sub> (104.57±41.34 cm<sup>3</sup>) of all patients were similar, and the two measurements were strongly correlated (r=0.9596, P<0.001). The difference between EATV<sub>cardiac scan</sub> and EATV<sub>CTA</sub> was –3.0549, with only 4.9% (10/204) of patients having values outside the 95% confidence interval (CI) range (-26.15 to 20.04; P for agreement =0.0003). Further, a significant agreement was observed between EATV<sub>cardiac scan</sub> and EATV<sub>CTA</sub> in 126 patients with plaques, with an estimated difference of –3.354, and 6.35% (8/126) of patients had values outside the 95% CI range (-31.37 to 24.66; P for agreement =0.0095). After adjustment for age and sex, EATV<sub>cardiac scan</sub> and EATV<sub>CTA</sub> were significantly associated with plaque (all P values <0.001), and the areas under the curve (AUCs) were 0.662 and 0.670 (P=0.4331), respectively. In contrast, EATV<sub>cardiac scan</sub> and EATV<sub>CTA</sub> were not associated with vulnerable plaque (P>0.05), with AUCs of 0.550 and 0.530, respectively (P=0.2157).

**Conclusions:** The study results indicate that  $EATV_{cardiac scan}$  and  $EATV_{CTA}$  are equivalent. In addition, both methods provide comparable values for predicting coronary arteriosclerosis in patients with low-to-mild calcification (CACS of <100 AU).

Keywords: Epicardial adipose tissue volume; low-dose cardiac scan; vulnerable plaque; tomography; radiography

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#### Introduction

Epicardial adipose tissue (EAT), a visceral thoracic adipose tissue located in the pericardium, is a biochemically and metabolically active tissue. The primary function of EAT is to store lipids as energy reserves. However, EAT also has an immune function, releasing hormones and inflammatory cytokines that have inflammatory effects on coronary arteries (1). Under pathological conditions in humans, EAT recruits inflammatory cells and induces apoptosis in intraplaque smooth muscle cells through a series of pathways. These pathways promote the formation of large lipid pools, thin fibrous caps, and punctate calcifications as well as lead to an increase in plaque volume. This gradually increases the rate of positive remodeling, eventually resulting in the formation of vulnerable plaques (2,3). The sudden rupture and shedding of vulnerable plaques is the main cause of several acute coronary syndromes, such as unstable angina and acute myocardial infarction, and even sudden death (4).

The American Heart Association recommends the use of statins for treating patients with a medium-to-high coronary artery calcium score (CACS) of  $\geq$ 100 AU. However, for patients with low-to-mild calcification (CACS <100 AU), no definite guidelines have been recommended yet, and treatment depends on the individual status of the patient (5,6). Because patients with vulnerable plaques in coronary arteries often have mild calcification scores (CACS <100 AU), their symptoms may not receive the timely attention of their physicians, eventually resulting in the development of acute coronary syndrome.

Recently, EAT volume (EATV) has been recognized as an independent predictor of vulnerable plaques in coronary arteries and is believed to have strong predictive ability (3,7). Multislice spiral computed tomography (CT) has become the preferred method for measuring EATV because of its high spatial resolution, high scanning speed, and reproducibility (8,9). Most studies on the association between EATV and coronary arteriosclerosis have relied on coronary CT angiography (CTA) (10,11). However, the large dosage of radiation and the requirement for injection of contrast agents are major concerns for coronary CTA. Recently, low-dose CT has been widely used to screen for diseases of the lung and other organs. It provides high spatial resolution, which is adequate to resolve small features of pericardial fat, without using radiographic contrast agents (12,13). We hypothesized that EATV can be measured using low-dose cardiac nonenhanced scan

(EATV<sub>cardiac scan</sub>), with accuracy and validity comparable to those of EATV measured using CTA (EATV<sub>CTA</sub>), making the method a viable alternative diagnostic tool for patients with mild calcification.

To address this hypothesis, we compared the accuracies of low-dose cardiac scan and coronary CTA for the quantification of EATV. Low-dose cardiac scan refers to the application of a low radiation dose during cardiac scan using a coronary calcium integral scan scheme for continuous transverse scans. We also evaluated the clinical utility of EATV<sub>cardiac scan</sub> in predicting coronary heart disease in patients with low-to-mild calcification (CACS <100 AU). The application of this technology will enable the early clinical evaluation of plaques and their stabilization using interventional therapy, thereby greatly reducing the occurrence of acute coronary syndrome. We present the following article in accordance with the STRAD reporting checklist (available at https://qims.amegroups.com/article/view/10.21037/qims-22-664/rc).

## **Methods**

#### Patients and sampling criteria

The study was conducted in accordance with the Declaration of Helsinki (as revised in 2013). The study was approved by Ethics Committee of the Fifth Affiliated Hospital of Southern Medical University and individual consent for this retrospective analysis was waived. In this study, we retrospectively screened 266 patients with clinical signs (chest pain, epigastric pain, or shortness of breath) of coronary heart disease and low-to-mild calcification (CACS <100 AU) who consecutively underwent low-dose cardiac scan and coronary CTA between June 1, 2020, and December 31, 2021. All scans were performed at the Department of Imaging Diagnostics of the Fifth Affiliated Hospital of Southern Medical University. The following patients were excluded from this study: (I) patients who were pregnant or lactating (n=1); (II) had previously undergone cardiac surgery (n=24), including coronary stent implantation, coronary artery bypass surgery, or pacemaker implantation; (III) had a history of other severe heart diseases (n=15), including valve disease, cardiomyopathy, pericardial effusion, or myocardial infarction; (IV) had an allergy to contrast medium (n=1); (V) had severe hepatic and renal insufficiency (n=4); (VI) had severe thyroid disease (n=1); (VII) had severe arrhythmia (n=3); or (VIII) had scans of poor image quality that interfered with coronary 2596

artery assessment (n=13). The remaining 204 patients [aged 32–90 years; 100 (48%) men] were enrolled in this study. The patients' selection was shown in the Figure S1.

As clinically indicated, written informed consent was obtained from all patients to undergo CT scan and CAT, and individual consent for this retrospective analysis was waived. All data for this study were analyzed anonymously.

## CT scans

All scans were performed using a Philips Brilliance 256-slice iCT scanner. The resting heart rate of the patients should be <80 beats/min before the examination. Patients with an elevated heart rate (>80 beats/min) were given metoprolol (25 mg) 60 min before the examination. All patients were sublingually administered with nitroglycerin (0.5 mg) 5 min before the examination dilate the coronary arteries.

The low-dose cardiac scan was performed using a coronary calcium integral scan scheme for continuous transverse scans combined with retrospective electrocardiogram (ECG) gating. Data were collected during the 60–80 RR period. The scanning parameters were as follows: tube voltage of 120 kV, tube current of 50 mA, and gantry rotation time of  $0.35 \text{ s/360}^{\circ}$ . The slice thickness was 2.5 mm, and the reconstruction interval was 2.5 mm. The scanning range extended from the tracheal bifurcation to the cardiac septum, with a scan time of 0.7 s, matrix of  $512 \times 512$ , and field of view (FOV) of 250 mm. Based on the dose-length product, the mean effective radiation dose was determined as 0.8 mSv in each patient.

The CTA was generally applied in patients immediately after the low-dose cardiac scan. For CTA, we used a retrospective ECG-gated scanning method. The scanning parameters were as follows: tube voltage of 120 kV, tube current of 550 mA, detector spacing of 128 × 0.625 mm, slice thickness of 0.90 mm, spacing of 0.45 mm, pitch of 0.18, and FOV of 250.0 mm, matrix of 512×512, and iDose4 levels of 3°-4°. We adjusted the tube current, tube voltage, iDose4 level, cardiac convolution function, contrast agent volume, and flow rate according to the patient's body mass index (BMI). Based on the dose-length product, the mean effective radiation dose was estimated to be 8 mSv in each patient. The scanning range extended up to the tracheal carina and down to the top of the left hepatic lobe. The contrast agent iopromide (370 mg/mL) was injected via the antecubital vein at a rate of 5 mL/sand total dose of 50-60 mL using a 20G intravenous indwelling needle of a double-barrel high-pressure syringe. After injecting the

contrast agent, 30 mL of normal saline was injected with the same proportion. We used automatic tracking scanning technology and considered the ascending aortic root as the observation area under a trigger threshold of 110 HU.

Using the contrast medium tracking technology, 8 seconds after the contrast medium injection, we start monitoring the CT value at the aortic root every 1.1 seconds. When the CT value in the sensing area reaches or exceeds the threshold of 110 HU, 6 seconds later, we started the coronary scan of the heart. During the scan process, ECG gating equipment was used to monitor patient heart rate changes.

## Soft plaque classification

Based on the 18-segment model of the Society of Cardiovascular Computed Tomography (14), we used CTA to measure the number of plaques in 18 coronary arteries. Two board-certified radiologists with 7 and 10 years of experience, respectively, independently evaluated the results of cardiac scans using curved multiplanar reconstructions and cross-sectional images. Any discrepancies were discussed and resolved. Using CTA scans, we assessed atherosclerotic plaques in the coronary arteries of all patients. Based on their physical characteristics, we used the following four degrees of calcification: dense calcium plaque (density of >350 HU), fibrous plaque (density of 131-350 HU), fibrofatty plaque (density of 31-130 HU), and necrotic core plaque (density of -30 to 30 HU) (15). Patients were categorized into the plaque group if any of these plaques was detected in the coronary artery, whereas those without any plaques were included in the nonplaque group.

High-risk coronary plaques exhibited one or more of the following four morphological characteristics: low-attenuation density (with average plaque attenuation of <30 HU and area of >1 mm<sup>2</sup>), positive remodeling plaque (with a ratio of the diameter of plaque to the mean of proximal and distal normal diameters of >1.1), spotty calcification (showing focal calcification within the coronary artery wall, with a maximum diameter of <3 mm in any direction), and napkin ring sign (with low-attenuation density of <30 HU in the central area of the plaque and slightly higher density, which was <130 HU, in the periphery). Patients with coronary plaques exhibiting two or more high-risk morphological features were defined as having vulnerable plaques (6,15).

# EATV measurement

We measured and analyzed EATV using Philips workstation

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Figure 1 Epicardial adipose tissue segmentation on cardiac plain scan (A: cardiac scan in the axial position, B: cardiac scan in the sagittal position, C: EATV<sub>cardiac scan</sub> calculation diagram) and epicardial adipose tissue segmentation on CTA (D: CTA in the axial position, E: CTA in the sagittal position, F: EATV<sub>CTA</sub> calculation diagram). EATV<sub>cardiac scan</sub>, epicardial adipose tissue volume from low-dose cardiac scan; CTA, computed tomography angiography.

Volumer software. The threshold density for adipose tissue was set at -190 to 30 HU. The measurement ranged from the origin of the left pulmonary artery at the midpoint of the transverse pericardium to the lower edge of the left ventricular apex. The software automatically identified adipose tissue, obtained a three-dimensional image of epicardial fat, and then calculated its volume (14) (*Figure 1*). Both the assessors of the low-dose cardiac scan and the assessors of the CTA were unavailable to the clinical information of the patients. Also, the assessors of the low-dose cardiac scan did not know the CTA results.

Considering the allergy to contrast agent for several patients, all patients would sign a content to the CAT measure and had a skin test of contrast agent before CTA.

# CACS

In accordance with the Agatston score, we defined the total

calcium score as the sum of the scores of each coronary artery. We used the following four categories of CACS: no calcification (CACS =0), slight calcification ( $1 \le CACS < 100$ ), mild-to-moderate calcification ( $100 \le CACS < 400$ ), and severe calcification (CACS  $\ge 400$ ) (16).

#### Statistical analysis

Continuous variables are represented as the mean  $\pm$  standard deviation or median (25<sup>th</sup> and 75<sup>th</sup> quartiles), as appropriate. Student's t-test or Wilcoxon test was used to compare data between groups. Categorical variables are represented as frequency and percentages. We used chi-square test to determine differences between two groups. Pearson correlation coefficient was used to evaluate the strength of correlation between EATV<sub>cardiac scan</sub> and EATV<sub>CTA</sub>. Bland-Altman test was performed to determine consistency between these two measurements. A multiple logistic regression model

<b>Table 1</b> Characteristics of patients with plaque vs. without plaque and patients with vulnerable vs. non-vulne
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Characteristics	Without plaque (n=78)	1 1	1	Vulnerable plaque (n=68)	Non-vulnerable plaque (n=58)	P value
EATV <sub>Cardiac scan</sub> (cm <sup>3</sup> )	86.46±26.60	110.83±46.27	<0.001*	111.38±36.91	110.18±55.62	0.889
EATV <sub>CTA</sub> (cm <sup>3</sup> )	89.03±26.08	114.18±45.97	<0.001*	114.53±39.11	113.77±53.25	0.929
Females	26 (33.33)	72 (57.14)	0.001*	35 (51.47)	37 (63.79)	0.164
Age, year	52.01±10.06	64.53±11.16	<0.001*	64.69±11.28	64.34±11.10	0.863
BMI (kg/m²)	24.38±3.62	23.93±5.48	0.523	23.48±4.17	24.47±6.70	0.313
Hemoglobin (g/L)	135.26±20.92	129.74±19.27	0.056	131.21±17.43	128.03±21.26	0.359
Total cholesterol (mmol/L)	4.85±1.13	4.79± 1.17	0.719	4.84±1.10	4.72±1.26	0.569
LDL (mmol/L)	2.77±0.97	2.82 ±1.03	0.717	2.85±1.01	2.78±1.06	0.671
HDL (mmol/L)	1.25±0.32	1.23±0.36	0.626	1.22±0.35	1.24±0.37	0.720
TG (mmol/L)	1.88±1.09	1.93±1.85	0.825	1.96±1.57	1.90±2.16	0.852
Hypertension	39 (50.00)	79 (62.70)	0.074	43 (63.24)	36 (62.07)	0.893
Diabetes	11 (14.10)	26 (20.63)	0.239	11 (16.18)	15 (25.86)	0.181
Dyslipidemia	46 (58.97)	79 (62.70)	0.596	43 (63.24)	36 (62.07)	0.893

Data are expressed as mean  $\pm$  standard deviation or n (%). \*P<0.05. EATV<sub>Cardiac scan</sub>, low-dose cardia plain scan to examine epicardial fat volume; EATV<sub>CTA</sub>, epicardial fat volume was quantified by coronary CTA; BMI, body mass index; LDL, low density lipid; HDL, high density lipid; TG, triglyceride.

was used to identify the potential predictors of coronary and vulnerable plaques. The receiver operating characteristic (ROC) curve was constructed to evaluate the predictive efficacy of  $EATV_{cardiac\ scan}$  and  $EATV_{CTA}$  for coronary and vulnerable plaques. Furthermore, the areas under the curve (AUCs) were calculated and compared for the two EATV measurements.

All statistical analyses were performed using statistical software packages SPSS (version 25.0; IBM Corp.) and MedCalc (version 18; MedCalc Software). A P value of <0.05 was considered to indicate statistical significance.

## **Results**

In total, 204 patients with suspected coronary heart disease underwent low-dose CT and coronary CTA to obtain EATV<sub>cardiac scan</sub> and EATV<sub>CTA</sub>, respectively (*Table 1*). Among all patients, 126 (61.8%) were diagnosed with coronary plaques; they were more likely to be women and were older than those without plaques (P<0.05 for both comparisons). Patients with coronary plaques had a more prevalent history of hypertension (P=0.893) and lower hemoglobin levels (P=0.359) than those without plaques; however, the difference was not statistically significant.

Further, patients with plaques had significantly higher EATV<sub>cardiac scan</sub> and EATV<sub>CTA</sub> than those without plaques (P<0.001 for both). Moreover, 54% [68] of patients with plaques showed vulnerable plaques. However, no significant differences were observed in sex (P=0.164); age (P=0.863); BMI (P=0.313); laboratory measurements (all P values >0.05); or history of hypertension (P=0.893), diabetes (P=0.181), or dyslipidemia (P=0.893) between patients with vulnerable and nonvulnerable plaques.

The two EATV measurements, EATV<sub>cardiac scan</sub> and EATV<sub>CTA</sub>, were strongly correlated with each other among all patients (r=0.960, P<0.001; *Figure 2A*), particularly among patients with coronary plaques (r=0.952, P<0.001; *Figure 2B*). Bland–Altman plots (*Figure 2C*) revealed that the mean difference between EATV<sub>cardiac scan</sub> and EATV<sub>CTA</sub> was -3.05 among all patients, and only a small number of patients (10/204, 4.9%) had values outside the 95% confidence interval (CI) range (-26.15 to 20.04, P for agreement =0.0003). A similar significant agreement was observed between EATV<sub>cardiac scan</sub> and EATV<sub>CTA</sub> among patients with plaques, with an estimated difference of -3.354, and 6.35% (8/126) of patients had values outside the 95% CI range (-31.37 to 24.66, P for agreement =0.0095) (*Figure 2D*).



**Figure 2** Correlation between EATV<sub>Cardiac scan</sub> and EATV<sub>CTA</sub> measured among 204 patients (r=0.960 and P<0.001) (A) and among 126 patients with plaques (r=0.952 and P<0.001). (B) Consistent Bland-Altman plots of EATV<sub>cardiac scan</sub> and EATV<sub>CTA</sub> measured among 204 patients (C) and among 126 patients with plaques (D). EATV<sub>cardiac scan</sub>, epicardial adipose tissue volume from low-dose cardiac scan; CTA, computed tomography angiography.

The results of univariate and multivariate logistic regression models revealed a significant association of  $EATV_{cardiac \ scan}$  (P<0.001) and  $EATV_{CTA}$  (P<0.001) with coronary plaques (Table 2). After adjustment for age and sex, the odds ratio for coronary plaques (Table 2) was 1.019 (95% CI: 1.010-1.029; P<0.001) and 1.020 (95% CI: 1.011-1.030; P<0.001), respectively. However, among patients with plaques, neither of the two EATV measurements was significantly associated with vulnerable plaques (P=0.903 for EATV<sub>Cardiac scan</sub> and P=0.932 for EATV<sub>CTA</sub>; *Table 3*). The results of ROC analysis were consistent with those of logistic regression. In particular, the ROC curves revealed that  $EATV_{cardiac \ scan}$  and  $EATV_{CTA}$  were predictors of coronary plaques in patients with suspected plaques; however, we could not distinguish patients with vulnerable plaques from those with nonvulnerable plaques (Figure 3). The AUC of EATV<sub>cardiac scan</sub> for coronary and vulnerable

plaques was 0.662 and 0.550, respectively, whereas that of EATV<sub>CTA</sub> was 0.670 and 0.530, respectively. However, EATV<sub>cardiac scan</sub> and EATV<sub>CTA</sub> showed similar inefficiency in diagnosing coronary plaques (P=0.433) and distinguishing vulnerable plaques (P=0.216).

#### Discussion

EATV measurement using coronary CTA for predicting coronary heart disease has gained nationwide popularity in recent years. However, this use of CTA remains limited because of the side effects of radiation and contrast media (17). Our retrospective analysis of dually scanned patients provides quantitative evidence with an intrinsic control that EATV measurements using low-dose cardiac scans and CTA were consistent, equally accurate, and significantly and strongly correlated in patients with low-to-

Table 2 The risk	k factors evaluation	of coronary pl	aque by using	logistic regression	n model

Diels featore	Crude model		Model I		Model II	
Risk factors	OR (95% CI)	P value	OR (95% CI)	P value	OR (95% CI)	P value
EATV <sub>Cardiac scan</sub> (cm <sup>3</sup> )	1.018 (1.009–1.027)	<0.001*	1.019 (1.010–1.029)	<0.001*	_	-
EATV <sub>CTA</sub> (cm <sup>3</sup> )	1.019 (1.009–1.028)	<0.001*	_	-	1.020 (1.011–1.030)	<0.001*
Females	2.667 (1.481–4.803)	0.001*	2.986 (1.599–5.577)	0.001*	2.980 (1.591–5.580)	0.001*
Age, year	1.114 (1.077–1.152)	<0.001*	1.137 (1.090–1.186)	<0.001*	1.137 (1.090–1.187)	<0.001*

Model I and model II: adjusted for age and gender. \*P<0.05. CI, confidence interval; EATV<sub>cardiac scan</sub>: low-dose cardia plain scan to examine epicardial fat volume, EATV<sub>CTA</sub>, epicardial fat volume was quantified by coronary CTA.

Table 3 The risk factors evaluation of vulnerable coronary plaque by using logistic regression model

Dials factors	Crude model		Model I		Model II	
Risk factors	OR (95% CI)	P value	OR (95% CI)	P value	OR (95% CI)	P value
EATV <sub>Cardiac scan</sub> (cm <sup>3</sup> )	0.999 (0.992–1.007)	0.884	0.999 (0.991–1.008)	0.903	-	_
EATV <sub>CTA</sub> (cm <sup>3</sup> )	1.000 (0.992–1.007)	0.926	-	-	1.000 (0.992–1.008)	0.932
Females	1.661 (0.812–3.400)	0.165	1.681 (0.807–3.504)	0.166	1.681 (0.807–3.505)	0.166
Age, year	0.997 (0.966–1.029)	0.862	1.003 (0.969–1.038)	0.868	1.003 (0.969–1.038)	0.878

Model I and model II: adjusted for age and gender. \*P<0.05. CI, confidence interval; EATV<sub>Cardiac scan</sub>, low-dose cardia plain scan to examine epicardial fat volume; EATV<sub>CTA</sub>, epicardial fat volume was quantified by coronary CTA.



**Figure 3** ROC curves of EATV<sub>cardiac scan</sub> and EATV<sub>CTA</sub> for diagnosing coronary (A) and vulnerable plaques (B). The AUC of the ROC curve for diagnosing coronary plaques was 0.662 for EATV<sub>cardiac scan</sub> and 0.670 for EATV<sub>CTA</sub> (P=0.4331). The AUC of the ROC curve for diagnosing vulnerable plaques was 0.550 for EATV<sub>cardiac scan</sub> and 0.530 for EATV<sub>CTA</sub> (P=0.2157). ROC, receiver operating characteristic; EATV<sub>cardiac scan</sub>, epicardial adipose tissue volume from low-dose cardiac scan; CTA, computed tomography angiography; AUC, areas under curve.

mild calcification (CACS <100 AU). This finding suggests that low-dose cardiac scans can be used as a preferred alternative to coronary CTA for diagnosing coronary plaques in patients with mild coronary calcification.

Recently, several studies have used non-CTA methods to measure EATV (14,18,19). Accordingly, we used lowdose chest CT scans to measure EATV and found that these values were significantly and strongly correlated with those measured using CTA. Our result is consistent with that of the study by Cheng et al., who retrospectively evaluated the efficacy of noncontrast CT scans for EATV measurements in 40 Chinese patients and revealed that these values were strongly correlated with those measured using CTA (19). Similar evidence regarding the associations between EATV and the progression of coronary artery calcification has been reported (15,20,21). However, these investigators used conventional doses during cardiac scans. Furthermore, a study involving 117 patients in Nagayama, Japan (14), revealed a close agreement between EATV measured using ECG noncontrast CT and that measured using CTA. However, in a study measuring pericardial fat area around the left and right main coronary artery initial segments using low-dose chest CT (18), the authors reported a modest correlation (r<0.73) between the pericardial fat area and epicardial fat volume in both segments. Our findings suggest that compared with CTA, a low-dose cardiac scan in patients with a low calcium score provides a clinical diagnosis with reduced radiation dose but similar diagnostic efficiency.

Quantification of EATV using coronary CTA has become a recognized method. However, several investigators believe that EATV measured using this technique underestimates the real volume because of the volume effect between the high-density coronary contrast agent and the low-density fat shadow around the coronary arteries (14). Even under a low-dose condition (with a tube voltage of 120 kV and tube current of 50 mA), different tube voltages could show differences in estimated fat density around the coronary arteries (22,23), which makes it impossible to exclude the possibility of EATV underestimation. Thus, these two types of CT imaging techniques have the potential to underestimate EATV.

Low-dose chest CT has become an important method for the early diagnosis of chest diseases (12,13), with a growing popularity because of limited patient exposure to radiation (24,25). Among our patients with mild calcification (CACS <100 AU), we revealed that the EATV measured using both low-dose cardiac scan and coronary CTA were independently associated with coronary arteriosclerosis. Vascular inflammation is a key factor in atherosclerotic plaque formation and plaque rupture (26). It has been reported that EAT with a larger volume contains more immature adipocytes, which exacerbate the inflammation of the vessel wall and instability of intimal plaques by releasing inflammatory factors (3,27), resulting in acute coronary syndrome. Both Gao et al. [2022] and Nerlekar et al. [2017] (3,28) reported that EATV was significantly associated with vulnerable plaques. Notably, among our patients with mild calcification (CACS <100 AU), the proportion of patients with vulnerable plaques was higher than that of patients with nonvulnerable plaques. Although this difference was not statistically significant, these patients were more likely to develop acute coronary syndrome. A previous study suggests that vulnerable plaques increase the risk of major adverse cardiac events by 4-5-fold (29). In this study, EATV measured using both low-dose cardiac scan and CTA had equivalent predictive value for coronary arteriosclerosis. Moreover, we found no significant difference in AUC between the two methods.

Although the quantification of EATV using coronary CTA has been widely recognized, other methods are in their initial stage. Considering the increasing attention and benefits of CT using a low radiation dose and low contrast agent, we believe that the measurement of EATV using this method is useful for the early clinical treatment and stabilization of plaques, particularly in patients with mild calcification (CACS <100 AU).

This study has several limitations. First, for measuring EATV, the same adipose threshold (-190 to -30 HU) was set for both low-dose EATV cardiac scan and coronary CTA. This choice might have introduced a bias by measuring lower values using low-dose cardiac scan. Several researchers have already used the ordered subset expectation maximization algorithm to improve the quality of low-dose CT images (30), thereby providing an approach to improve the accuracy of the total EATV measurements. Second, various studies have indicated the correlation between pericoronary adipose tissue (PCAT) and coronary arteriosclerosis (3,16,31). The current study is a part of a series of future studies in which we plan to combine EATV and PCAT to detect vulnerable coronary plaques. Third, the accurate measurement of pericardial adipose volume currently requires a long time in manually controlled offline analysis. To shorten the measurement time in the future, the continuous advancement of artificial intelligence applications in the field of medical imaging may provide promising alternatives to current practices (32). Finally, this study is a single-center study with a small sample size; thus, the findings warrant further evaluation with larger sample sizes.

EATV can be measured using low-dose cardiac scans with accuracy comparable to that of coronary CTA. In addition, the two methods provide comparable values for predicting coronary arteriosclerosis in patients with low-tomild calcification (CACS <100 AU).

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# Footnote

*Reporting Checklist:* The authors have completed the STARD reporting checklist. Available at https://qims.amegroups.com/article/view/10.21037/qims-22-664/rc

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# Supplementary



Figure S1 Flow diagram.