



Model development and validation of noninvasive parameters based on coronary computed tomography angiography to predict culprit lesions in acute coronary syndromes within 3 years: value of plaque characteristics, hemodynamics and pericoronary adipose tissue

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Background: Machine learning (ML) is combined with noninvasive parameters from coronary computed tomography angiography (CTA) to construct predictive models to identify culprit lesions that may lead to acute coronary syndrome (ACS).

Methods: We retrospectively analyzed 132 patients with ACS at the Fourth Affiliated Hospital of Harbin Medical University who had coronary CTA between 3 months and 3 years before the ACS event, with a total of 240 lesions. Lesions from 2020 (n=154) were included in the training set, and lesions from 2021 (n=86) were included in the test set for internal validation. We evaluated the role of plaque characteristics, hemodynamic parameters and pericoronary adipose tissue (PCAT) attenuation from CTA in identifying culprit ACS lesions. In the training set, logistic regression was used to screen CTA-derived parameters with P values <0.05 for the model construction. Logistic regression, random forest, Bayesian and K-nearest neighbor algorithms were used to build classification models, and their performance was assessed using the test set. The following models were established to evaluate the effectiveness of different combinations of models to identify culprit lesions: Model 1 was established for plaque characteristics; Model 2 was established for hemodynamic parameters; Model 3 was established for PCAT attenuation; Model 4 was established for plaque characteristics and hemodynamic parameters; and Model 5 was established for plaque characteristics, hemodynamic parameters and PCAT attenuation.

Results: A total of ten high-risk factors were screened for the ML model construction, and the ML model based on the logistic regression algorithm had the best performance among the four algorithms (accuracy =0.721; sensitivity =0.892; specificity =0.592; positive prediction =0.623; and negative prediction =0.879). In this model, the minimum lumen area, positive remodeling and lesion-specific fat attenuation index (FAI) were the risk factors significantly associated with the culprit lesion. Analysis of the effect of different

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combinations of models to identify culprit lesions showed that Model 5 had the best predictive effect (AUC =0.819 and 95% CI: 0.722–0.916).

Conclusions: ACS can be predicted using ML based on CTA parameters. Compared to other models, the model combining plaque characteristics, hemodynamic parameters and PCAT attenuation performed best in predicting the culprit lesion.

Keywords: Acute coronary syndrome; computed tomography angiography; machine learning; computed tomography-derived fractional flow reserve (FFRCT); pericoronary adipose tissue

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Introduction

Acute coronary syndrome (ACS) is a disease mainly caused by atherosclerosis (more than 90%), which is characterized by an acute onset and many complications. Therefore, it is necessary to focus on atherosclerosis for this disease (1). Most ACS is not due to obstructive coronary disease but rather rupture of vulnerable plaques (2), indicating that it is important to identify vulnerable plaques for patients. Coronary computed tomography angiography (CTA) provides plaque information in a noninvasive imaging modality (3,4), providing clinical predictive value through quantification and analysis of plaques to identify adverse plaques. In addition, the advent of coronary computed tomography-derived fractional flow reserve (FFRCT) enables coronary CTA to combine detailed anatomical and physiological information in a single standard examination (5,6), which can further reflect the presence of ischemic symptoms at the lesion site. However, plaque rupture is a complex clinical process, and the advent of a plaque to rupture and cause ACS is affected by many factors. Vascular inflammation is a key factor leading to the formation and rupture of atherosclerotic plaques, which can lead to the occurrence of ACS (7). A correlation between inflammation and pericoronary adipose tissue (PCAT) has been established; pro-inflammatory factors are released from the inflamed vessel wall and propagate in a paracrine manner toward PCAT, which inhibits local adipogenesis in PCAT, and this process is detectable in CTA by quantifying the fat attenuation index (FAI) (8-10).

Previous studies have shown that adding noninvasive hemodynamic parameters to anatomical and plaque characteristics improves the prediction of culprit lesions (11), and PCAT features have also been used to predict ACS (12). However, the predictive value of combining plaque

characteristics, noninvasive hemodynamic parameters and PCAT for ACS has not been investigated. The use of machine learning (ML) on the basis of imaging can provide incremental value in cardiovascular disease diagnosis, facilitating faster and more accurate diagnosis and decision-making, thereby significantly reducing the burden of disease (13-15). Therefore, the present study used machine learning to develop and validate models of culprit lesions based on plaque characteristics, hemodynamic parameters and PCAT attenuation of CTA to identify culprit lesions that cause subsequent ACS in the next 3 months to 3 years. The present study is performed in accordance with the TRIPOD reporting checklist (available at <https://qims.amegroups.com/article/view/10.21037/qims-22-1045/rc>).

Methods

Study population

The study population was retrospectively recruited from the Fourth Affiliated Hospital of Harbin Medical University (HeiLongJiang Province, China) and included patients with well-documented ACS [unstable angina (UA), ST-elevation myocardial infarction (STEMI), and non-ST-elevation myocardial infarction (NSTEMI)] who underwent CTA at our hospital 3 months to 3 years ago due to symptoms, such as chest pain with suspected coronary artery disease (CAD). The diagnosis of ACS was based on the guidelines published by the 2020 ESC on the management of acute coronary syndromes (16). The patients included in this study had no clinically typical symptoms and definite evidence of ACS at the time of CTA examination. Invasive coronary angiography (ICA) was performed at the time of ACS, and culprit and nonculprit lesions were identified by interventional cardiologists who were unaware of the CTA

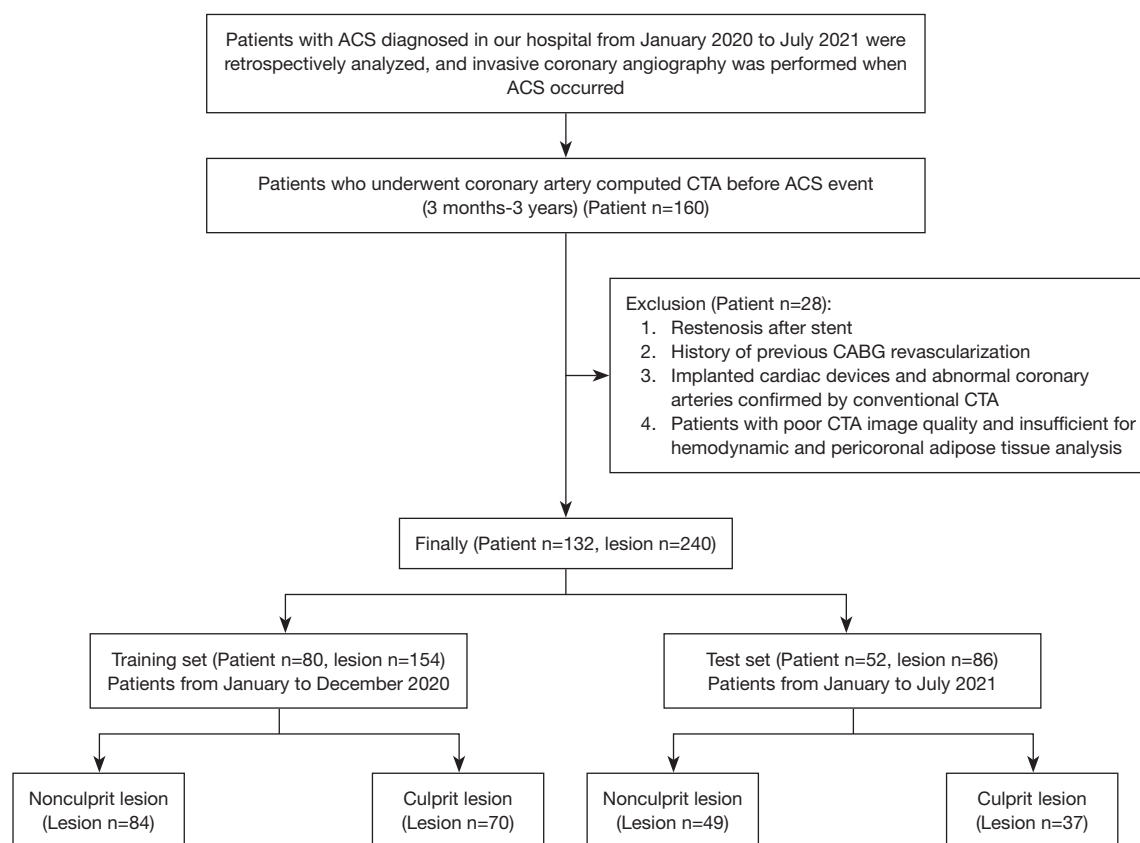


Figure 1 Flowchart of the study. CTA, computed tomography angiography; ACS, acute coronary syndrome; CABG, coronary artery bypass grafting.

evaluation results. The exclusion criteria were as follows: (I) restenotic lesions after stenting at the time of ACS occurrence; (II) history of coronary artery bypass grafting (CABG) revascularization before ACS occurred; (III) implanted cardiac devices and abnormal coronary arteries confirmed by conventional CTA; and (IV) patients with poor-quality CTA images insufficient for hemodynamic and PCAT analysis. A total of 132 patients with 240 lesions were included in the present study. The lesions of patients from January to December 2020 ($n=154$) were included in the training set, and the lesions of patients from January to July 2021 ($n=86$) were included in the test set in chronological order. The flow chart of the study design is shown in *Figure 1*. The present study was conducted in accordance with the Declaration of Helsinki (as revised in 2013), and it was approved by the Medical Ethics Committee of The Fourth Affiliated Hospital, Harbin Medical University (No. 2022-SCILLSC-11). Individual consent for this retrospective analysis was waived.

CTA acquisition

All scans were performed on a Toshiba 320-row computed tomography scanner (Aquilion ONE, Toshiba, Tokyo, Japan). A prospective ECG gating protocol was used for the CTA scan with the following scan parameters: tube voltage was 100 or 120 kV; tube current was determined by body mass index (300–500 mA); and time resolution was 275 ms. Prior to contrast injection, the control heart rate was <80 beats/min, and patients with high heart rates underwent CTA after heart rate stabilization or were considered for beta blockers at the discretion of the treating physician. Then, 60–70 mL of iodine contrast medium (350 mg/mL iodine-containing ethanol solution) was injected at a flow rate of 4.5–5 mL/s. The reconstructed image matrix was 512×512 with a layer thickness of 0.5 mm and increments of 0.25 mm.

Coronary plaque analysis

All patient images were retrospectively analyzed using

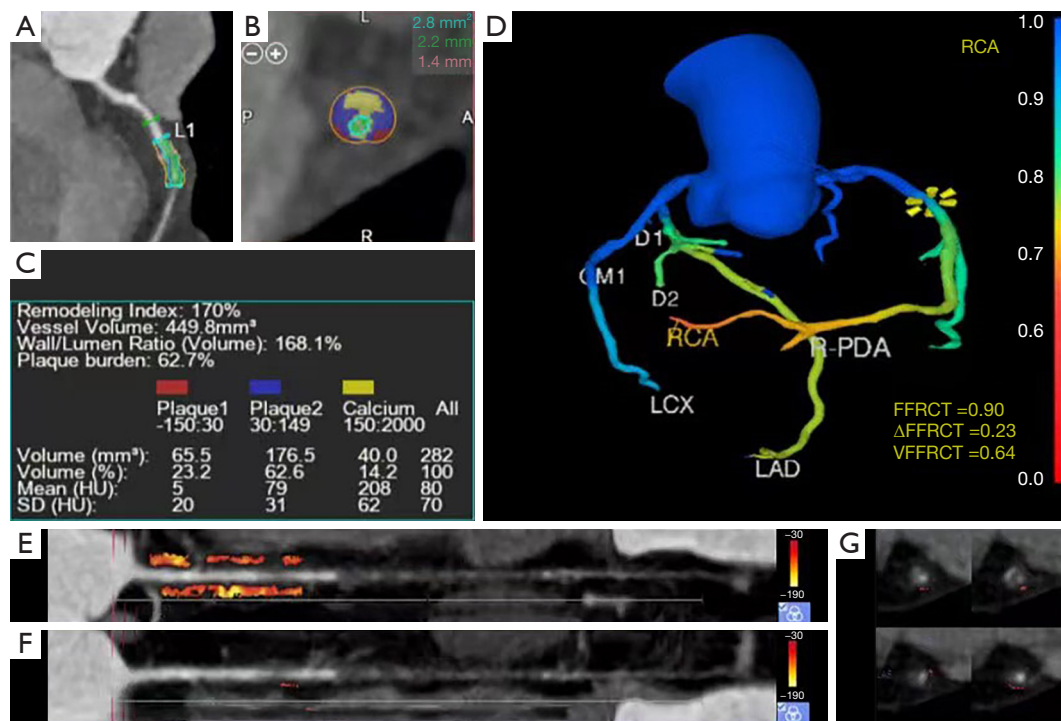


Figure 2 Representative cases. (A) Curved projection reformation map. The lesion area is located between the two blue lines. The green line is the reference point, and the red line is the narrowest position of the lesion. (B) Cross-sectional view of the narrowest position of the lesion. The green area is the lumen and represents the MLA, and the red area is the LAP. The blue area is the FP, and the yellow area is the CP. (C) Plaque analysis map. (D) Hemodynamic characteristic map. (E) Proximal FAI map of the lesion. (F) Lesion-specific FAI measurement map. (G) Cross-sectional view of lesion-specific FAI. Figure shows a typical case of the culprit lesion of ACS. CTA showed RCA lesion diameter stenosis of 58%, lesion length of 1.7 mm, distance from the opening of 45.05 mm, MLA of 2.8 mm², remodeling index of 1.7, wall-to-lumen ratio of 1.68 and plaque load of 62.7% as well as LAP, FP, CP and TP volumes of 65.5, 176.5, 40 and 282 mm³, respectively, with no spotty calcification. FFRCT =0.9, Δ FFRCT =0.23, VFFRCT =0.64. The proximal FAI was -67, and the lesion-specific FAI was -45. At 283 days after CTA, the patient presented with ACS. DS, diameter stenosis; MLA, minimal lumen area; LAP, low attenuation plaque; FP, fibrous plaque; CP, calcified plaque; TP, total plaque; FAI, fat attenuation index; CTA, computed tomography angiography; ACS, acute coronary syndrome; RCA, right coronary artery; FFRCT, computed tomography-derived fractional flow reserve; Δ FFRCT, Delta FFRCT; VFFRCT, vessel FFRCT.

semiautomatic plaque analysis software (Vitrea version 7.6; Vital Images). The software automatically extracted the coronary artery tree and automatically identified the inner and outer diameters of the lumen, and we performed manual correction when identifying errors (Figure 2A-2C). Plaque morphological features, including vessel location, diameter stenosis (DS), length, distance from the ostium, minimal lumen area (MLA) and spotty calcification, were measured (17). Low attenuation plaque (LAP) volume, fibrous plaque (FP) volume (medium attenuation plaque), calcified plaque (CP) volume and total plaque (TP) volume were also measured (17). Plaque burden (11), wall-to-lumen volume ratio, remodeling index and positive

remodeling were quantitatively calculated. A total of 13 plaque parameters were analyzed. The detailed parameter definitions are provided in the Appendix 1.

Analysis of hemodynamic parameters of coronary CTA

For the hemodynamic analysis, a software model based on computational fluid dynamics (Shukun Technology) was used. In each subject, the fractional flow reserve at the lesion site was calculated (expressed as FFRCT), and the vessel FFRCT (VFFRCT) was defined as the minimum value of the distal FFRCT of the vessel encompassing the entire coronary artery (18). Δ FFRCT was defined as the

subtraction value of the proximal and distal FFRCT of the lesion (19) (*Figure 2D*).

PCAT attenuation analysis

We recorded the proximal 40 mm segments of the three major coronary arteries [left anterior descending artery (LAD), left circumflex artery (LCX) and right coronary artery (RCA)] containing lesions (RCA analyzed vessels 10–50 mm from the ostium), and we defined PCAT as the radial distance from the vessel wall equal to the vessel diameter for all voxels in the range of –190 to –30 HU (20). PCAT attenuation was calculated from the average attenuation of perivascular adipose tissue, and the fat attenuation index (FAI) was determined by quantifying weighted perivascular fat attenuation after adjustment for technical parameters. We used dedicated analysis software (Shukun Technology) to measure the proximal FAI of the vessel where the lesion was located (*Figure 2E*). In addition, we measured lesion-specific FAI (21), which was measured proximal and distal 5 mm from the center of the lesion as well as 10 mm in length and 2 mm from the outer diameter of the vessel (*Figure 2F,2G*).

Machine learning model construction, validation and performance

In the development cohort, logistic regression analysis was performed to identify factors associated with culprit lesions, and parameters with $P < 0.05$ were included in the model construction (*Appendix 1*). Logistic regression (LR), random forest (RF) (22), Bayesian (23) and K-nearest neighbor (KNN)(22) algorithms were applied in the training set to build models. The area under the receiver operating characteristic (ROC) curve (AUC) was used as an indicator of the predictive performance of the model. Decision curve analysis (DCA) was used to elucidate the overall benefit of different predictive models. The nomogram of the combined model was established to predict the future incidence of ACS culprit lesions in patients with coronary artery disease.

Statistical analysis

Statistical analysis was performed using R software (version 4.1.0) and SPSS Statistics 25.0, and statistical significance was defined as two-sided $P < 0.05$. Continuous variables with normal distribution are expressed as the mean \pm standard deviation (SD), and nonnormal distributions are expressed

as the median (25th and 75th). Categorical variables are expressed as number [n (%)]. *T* tests, Mann-Whitney U tests and chi-square tests were used to compare baseline characteristics of the cohorts.

Results

Baseline characteristics of patients

In this single-center retrospective study, a total of 160 patients with ACS who had both prior CTA images and concurrent ICA examinations were included according to previous inclusion criteria. The following patients were excluded: eight patients with restenosis after stenting, five patients who had undergone CABG surgery, four patients with implanted cardiac devices or containing abnormal coronary arteries, three patients with poor image quality and eight patients who could not be identified by software and measured by FFRCT or FAI. Ultimately, a total of 132 patients with 240 lesions (107 culprit lesions and 133 nonculprit lesions) were included in the present study. The training set included 154 lesions (70 culprit lesions and 84 nonculprit lesions), and the test set included 86 lesions (37 culprit lesions and 49 nonculprit lesions). The average interval between coronary CTA scan and ACS was 525.50 (329.00–758.75) days (*Table 1*). The baseline characteristics of the patients did not significantly differ between the training set and test set (all $P > 0.05$).

Comparison of CTA parameters for culprit and nonculprit lesions

Based on the training set, we compared the differences in plaque characteristics, hemodynamic parameters and PCAT attenuation between culprit and nonculprit lesions (*Table 2*). Compared to nonculprit lesions, culprit lesions had a smaller MLA, longer lesion length and larger LAP, FP and TP volumes (all $P < 0.05$). In terms of hemodynamic parameters, the culprit lesions had lower VFFRCT values and higher Δ FFRCT values (both $P < 0.01$), while there was no significant difference in FFRCT values between culprit and nonculprit lesions ($P = 0.191$). Regarding the comparison of PCAT attenuation, both proximal FAI and lesion-specific FAI in culprit lesions were higher than those in nonculprit lesions [-86.81 ± 10.50 vs. -90.33 ± 10.00 HU ($P = 0.036$) and -77.67 ± 11.8 vs. -85.80 ± 10.10 HU ($P < 0.001$), respectively]. The results of the comparison of CTA parameters for the test set are shown in *Table 2*.

Table 1 Characteristics of the patients

Patients	Total (N=132)	Training (N=80)	Test (N=52)	P
Age (years)	63.70 (8.80)	64.10 (8.74)	63.10 (9.01)	0.510
Male	71 (53.8)	38 (47.5)	33 (63.5)	0.106
BMI (kg/m ²)	25.30 (3.10)	25.60 (3.03)	24.80 (3.11)	0.145
The average interval between CTA and ACS (days)	525.50 [329.00, 758.75]	520.00 [365.00, 736.00]	557.00 [203.00, 802.00]	0.234
Cardiovascular risk factors				
Hypertension	90 (68.2)	59 (73.8)	31 (59.6)	0.130
Hyperlipidemia	66 (50.0)	44 (55.0)	22 (42.3)	0.212
Diabetes mellitus	52 (49.4)	32 (40.0)	20 (38.5)	>0.999
Smoking	46 (34.8)	27 (33.8)	19 (36.5)	0.887
History of drinking	22 (16.7)	11 (13.8)	11 (21.2)	0.381
Clinical presentation				0.542
UA	100 (75.8)	58 (72.5)	42 (80.8)	
NSTEMI	17 (12.9)	12 (15.0)	5 (9.6)	
STEMI	15 (11.4)	10 (12.5)	5 (9.6)	

Table represents the baseline information for total patients, training set patients and test set patients. P values represent the difference between the training and test sets. Values are mean (SD), n (%), or median [25th, 75th]. BMI, body mass index; CTA, computed tomography angiography; ACS, acute coronary syndrome; UA, unstable angina; NSTEMI, non-ST-segment elevation myocardial infarction; STEMI, ST-segment elevation myocardial infarction.

CTA lesion characteristics to estimate the risk of culprit lesions

In the training set, univariate logistic regression analyses were performed to identify plaque characteristics, hemodynamic parameters and PCAT attenuation from CTA lesions associated with culprit lesions (Table 3) as well as to calculate odds ratios (ORs) expressed with 95% confidence intervals (CIs). The following ten high-risk factors ($P < 0.05$) were identified (Table 3): DS, lesion length, MLA, low-attenuation plaque, fibrous plaque, positive remodeling, VFFRCT, Δ FFRCT, proximal FAI and lesion-specific FAI. The above parameters were used to construct a predictive model for ACS culprit lesions.

Develop predictive models for ACS culprit lesions using machine learning

Based on machine learning, a multiparameter combined model with 10 lesion features was constructed. The measured AUC values were used to compare the ability of the models constructed by the four algorithms to

distinguish the culprit lesions (Figure 3A, 3B). During the training process, the AUC values of the LR model, RF model, Bayesian model and KNN model were 0.809 (95% CI: 0.739–0.878), 0.990 (95% CI: 0.976–1.000), 0.693 (95% CI: 0.612–0.775), and 0.710 (95% CI: 0.628–0.793), respectively. In the test set, the LR model, RF model and Bayesian model had better predictive performance than the KNN model with AUC values of 0.819 [95% CI: 0.722–0.916], 0.754 (95% CI: 0.646–0.861), 0.754 (95% CI: 0.650–0.857) and 0.700 (95% CI: 0.586–0.815), respectively. It is worth noting that although the AUC value of the RF model was significantly higher than that of the LR model during training [AUC: 0.990 (95% CI: 0.976–1.000) *vs.* 0.809 (95% CI: 0.739–0.878)], the result was the opposite in the test set [AUC: 0.754 (95% CI: 0.646–0.861) *vs.* 0.819 (95% CI: 0.722–0.916)], which indicated that the RF model was overfitting during training.

In the DCA curve (Figure 3C, 3D), excluding the overfitting of the RF model in the training set, the LR model had the highest clinical application value and the best overall benefit of the model followed by the Bayesian model (Figure 3D). In the performance comparison of the

Table 2 Comparison of CTA parameters between culprit and nonculprit lesions

Characteristics	Training (N=154)			Test (N=86)			P
	Nonculprit (N=84)	Culprit (N=70)	P	Nonculprit (N=49)	Culprit (N=37)	P	
Vessel location			0.348			0.737	0.811
LAD	30 (35.7)	33 (47.1)		17 (34.7)	15 (40.5)		
LCX	25 (29.8)	18 (25.7)		17 (34.7)	10 (27.0)		
RCA	29 (34.5)	19 (27.1)		15 (30.6)	12 (32.4)		
DS	0.54 [0.38, 0.68]	0.65 [0.50, 0.77]	0.001	0.56 [0.45, 0.63]	0.64 [0.56, 0.86]	0.004	0.646
Lesion length	9.90 [7.40, 12.60]	12.10 [8.68, 17.10]	0.003	9.90 [7.50, 13.00]	13.9 [9.50, 18.10]	0.009	0.616
Distance from ostium	42.00 [32.10, 61.90]	43.70 [32.60, 59.10]	0.949	42.80 [36.90, 61.50]	44.5 [32.40, 60.40]	0.622	0.666
MLA	4.55 [3.10, 7.03]	2.90 [1.42, 5.25]	0.002	4.70 [3.10, 6.10]	2.50 [0.90, 4.00]	0.002	0.603
Low attenuation plaque	18.50 [12.70, 39.30]	28.30 [15.60, 42.70]	0.036	22.40 [13.60, 35.20]	28.60 [18.20, 53.80]	0.048	0.381
Fibrous plaque	46.40 [30.20, 72.40]	66.90 [46.00, 104.00]	0.003	51.80 [30.60, 85.40]	74.00 [46.00, 146.00]	0.009	0.346
Calcified plaque	35.60 [13.70, 62.50]	36.60 [11.40, 72.50]	0.795	25.90 [9.80, 48.40]	40.00 [20.90, 49.50]	0.186	0.282
Total plaque volume	104.00 [65.80, 159.00]	129.00 [82.20, 230.00]	0.039	107.00 [59.00, 148.00]	151.00 [94.00, 232.00]	0.015	0.845
Positive remodeling	23 (27.4)	31 (44.3)	0.043	10 (20.4)	12 (32.4)	0.310	0.171
Wall to lumen volume ratio	1.55 [1.12, 2.50]	1.80 [1.45, 2.30]	0.088	1.66 [1.12, 2.42]	2.12 [1.68, 3.08]	0.005	0.352
Plaque burden	0.61 (0.13)	0.65 (0.11)	0.080	0.60 (0.13)	0.68 (0.12)	0.003	0.668
Spotty calcification	12 (14.3)	16 (22.9)	0.245	8 (16.3)	4 (10.8)	0.677	0.508
FFRCT	0.92 [0.84, 0.97]	0.89 [0.82, 0.96]	0.191	0.94 [0.90, 0.97]	0.88 [0.73, 0.93]	0.001	0.841
VFFRCT	0.82 [0.72, 0.89]	0.71 [0.64, 0.85]	0.004	0.83 [0.75, 0.89]	0.69 [0.62, 0.79]	<0.001	0.784
Δ FFRCT	0.05 [0.02, 0.11]	0.08 [0.03, 0.20]	0.009	0.06 [0.03, 0.09]	0.10 [0.04, 0.18]	0.047	0.971
Proximal FAI	-90.33 (10.00)	-86.81 (10.50)	0.036	-87.53 (8.61)	-83.78 (8.37)	0.046	0.026
Lesion specific FAI	-85.80 (10.10)	-77.67 (11.80)	<0.001	-79.43 (11.90)	-69.14 (12.40)	<0.001	<0.001

Table shows the comparison of the differences in CTA parameters for the culprit lesions and nonculprit lesions in the training and test sets, and the p values in the last column represent the comparison of the differences between the training and test set data. Values are mean (SD), n (%), or median [25th, 75th]. CTA, computed tomography angiography; LAD, left anterior descending artery; LCX, left circumflex artery; RCA, right coronary artery; DS, diameter stenosis; MLA, minimal lumen area; FFRCT, computed tomography-derived fractional flow reserve; Δ FFRCT, delta FFRCT; VFFRCT, vessel FFRCT; FAI, fat attenuation index.

four models (*Table 4*), the LR model had the best predictive performance with an accuracy, sensitivity, specificity, positive prediction and negative prediction 0.721, the 0.892, 0.592, 0.623 and 0.879, respectively. Combining the above factors, the logistic regression model had the best overall prediction performance, and the algorithm was selected for

ML model construction.

Evaluation and application of the ML model

We assessed the risk of ACS for each parameter in a combined prediction model containing ten parameters

Table 3 Plaque characteristics, hemodynamic parameters and PCAT attenuation of CTA predict the risk of culprit lesions

Characteristics	OR	95% CI	P
Plaque characteristics			
Vessel location LAD	Reference		
Vessel location LCX	0.65	0.30–1.43	0.29
Vessel location RCA	0.60	0.28–1.27	0.18
DS	20.13	3.33–121.76	<0.001
Lesion length	1.07	1.01–1.12	0.01
Distance from ostium	1.00	0.99–1.01	0.61
MLA	0.85	0.76–0.95	<0.001
Low attenuation plaque	1.02	1.00–1.03	0.03
Fibrous plaque	1.01	1.00–1.02	<0.001
Calcified plaque	1.00	1.00–1.00	0.80
Total plaque volume	1.00	1.00–1.00	0.11
Positive remodeling	2.11	1.08–4.13	0.03
Wall to lumen volume ratio	1.07	0.84–1.35	0.60
Plaque burden	10.19	0.72–143.83	0.09
Spotty calcification	1.78	0.78–4.07	0.17
Hemodynamic parameters			
FFRCT	0.15	0.01–3.55	0.24
VFFRCT	0.03	0.00–0.37	0.01
ΔFFRCT	250.99	5.12–12,295.67	0.01
PCAT attenuation			
Proximal FAI	1.03	1.00–1.07	0.04
Lesion specific FAI	1.07	1.04–1.11	<0.001

OR, odds ratio; CI, confidence interval; PCAT, pericoronary adipose tissue; CTA, computed tomography angiography; LAD, left anterior descending artery; LCX, left circumflex artery; RCA, right coronary artery; DS, diameter stenosis; MLA, minimal lumen area; FFRCT, computed tomography-derived fractional flow reserve; ΔFFRCT, delta FFRCT; VFFRCT, vessel FFRCT; FAI, fat attenuation index.

(Appendix 1). In this model, MLA was a protective factor for ACS (OR =0.81, 95% CI: 0.68–0.95, P=0.01). Of note, higher values indicated lower risk of the lesion becoming a culprit lesion. Positive remodeling and lesion-specific FAI were risk factors for culprit lesions (OR =3.06, 95% CI: 1.32–7.37, P=0.01; OR =1.10, 95% CI: 1.05–1.16, P<0.001, respectively) (Figure S1). In the nomogram (Figure 4), the visualization predicted the probability of future culprit

lesions. The optimal cutoff value of the model was 0.408. When the Pr(label) value was greater than or equal to 0.408, the lesion prediction outcome was the culprit lesion, and when the Pr(label) value was less than 0.408, the lesion prediction outcome was the nonculprit lesion.

Comparison of the effects of different classification models in predicting ACS culprit lesions

In the test set, ten prediction parameters were formed into the following models according to categories to evaluate the plaque characteristics, hemodynamic parameters and PCAT attenuation for predicting the value of ACS: Model 1 was established for plaque characteristics; Model 2 was established for hemodynamic parameters; Model 3 was established for PCAT attenuation; Model 4 was established for plaque characteristics and hemodynamic parameters; and Model 5 was established for plaque characteristics, hemodynamic parameters and PCAT attenuation.

Among the three single-category models (Models 1–3), the ROC curve showed that the prediction effect of the plaque characteristics (Model 1) (AUC =0.793) was better than that of Model 2 (AUC =0.738) and Model 3 (AUC =0.715). Combining hemodynamic parameters and plaque features (Model 4) did not significantly improve prediction (AUC =0.783), but the combined model (Model 5) had the best prediction performance for culprit lesions (AUC =0.819) (Figure 5A). The DCA curve showed that Model 5 patients had the greatest net benefit followed by Model 4 patients (Figure 5B). The calibration curves for the different models are shown in Figure S2.

Discussion

The present study used ML to investigate the diagnostic performance of CTA-derived plaque characteristics, hemodynamics and PCAT attenuation in predicting culprit ACS lesions. In the present study, a simple random grouping was not used due to an insufficient sample size, but the patients were divided into training and test sets based on the year of enrollment, which more objectively reflected the generalization of the constructed model. The present results showed that there were significant differences in MLA, lesion length, LAP volume, FP volume, TP volume, VFFRCT, proximal FFRCT, proximal FAI and lesion-specific FAI between the culprit and nonculprit lesions (all P<0.05). Ten high-risk factors (all P<0.05) were screened from 18 CTA-derived parameters by logistic regression for

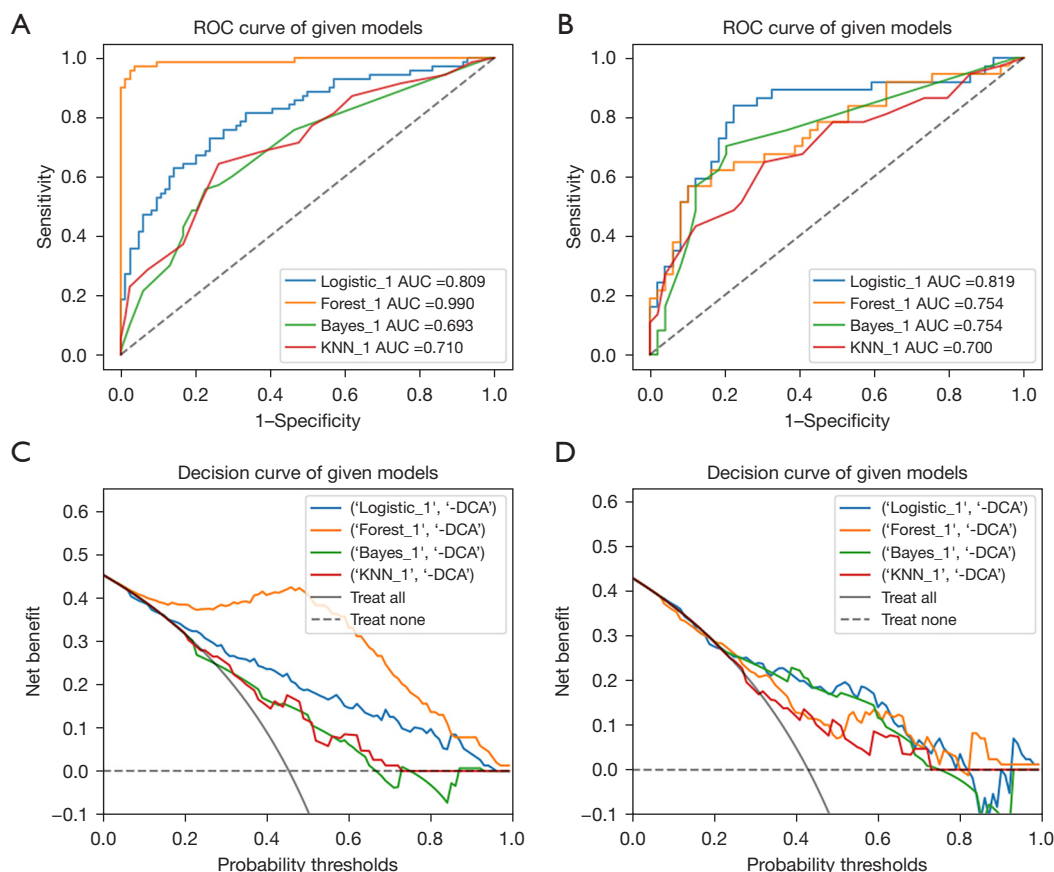


Figure 3 Comparison of the performance of the logical regression model, random forest model, Bayesian model and K-nearest neighbor model in predicting culprit lesions of ACS. ROC curve of four models in the training set (A) and test set (B) for predicting the culprit lesion of ACS. DCA curves of the four models in the training set (C) and test set (D). Blue lines, orange lines, green lines and red lines represent the logical regression model, random forest model, Bayesian model and K-nearest neighbor model, respectively. The ROC curve of the logical model shows that the AUC values of the training set and the test set are 0.809 and 0.819, respectively. The DCA curve shows the clinical utility of the model by comparing the net gain at different threshold probabilities. The solid gray line represents the assumption that all lesions are the culprit lesions of ACS, while the dashed gray line represents the assumption that no lesions are the culprit lesions of ACS. ACS, acute coronary syndrome; ROC, receiver operating characteristic; DCA, decision curve analysis; AUC, area under the ROC curve; KNN, K-nearest neighbor.

ML model construction. The results showed that the ML model based on the LR algorithm was the best model. The comparison results of the combined models of different classifications showed that Model 5 had the best prediction effect (AUC = 0.819).

Previous studies have suggested that ACS is associated with atherosclerotic plaque vulnerability (24). Identified high-risk plaque characteristics of CTA include LAP, spotty calcification, positive remodeling and napkin ring sign, and these characteristics are associated with the occurrence of ACS (25). Lee *et al.* (19) analyzed the predictive value of

adverse plaque characteristics and hemodynamic parameters for ACS, and they reported that the relative importance of Δ FFRCT is higher than that of FFRCT, agreeing with the present results. In the present study, when adverse plaque and hemodynamic characteristics were added to the prediction model, the AUC continued to improve. The present study further investigated the predictive value of PCAT attenuation.

In addition to plaque characteristics and hemodynamic parameters, the discovery of PCAT attenuation provides more comprehensive inflammatory information for the

Table 4 Performance metrics for the four models in the training and test sets

Model characteristics	Training				Test			
	LR	RF	Bayesian	KNN	LR	RF	Bayesian	KNN
Accuracy	0.740	0.955	0.675	0.662	0.721	0.640	0.733	0.674
Sensitivity	0.714	0.914	0.557	0.514	0.892	0.676	0.622	0.649
Specificity	0.762	0.988	0.774	0.786	0.592	0.612	0.816	0.694
positive prediction	0.714	0.985	0.672	0.667	0.623	0.568	0.719	0.615
negative prediction	0.762	0.933	0.677	0.660	0.879	0.714	0.741	0.723
AUC (95% CI)	0.809 (0.739–0.878)	0.990 (0.976–1.000)	0.693 (0.612–0.775)	0.710 (0.628–0.793)	0.819 (0.722–0.916)	0.754 (0.646–0.861)	0.754 (0.650–0.857)	0.700 (0.586–0.815)

LR, logistic regression; RF, random forest; KNN, K-nearest neighbor; AUC, area under the ROC curve; CI, confidence interval; ROC, receiver operating characteristic.

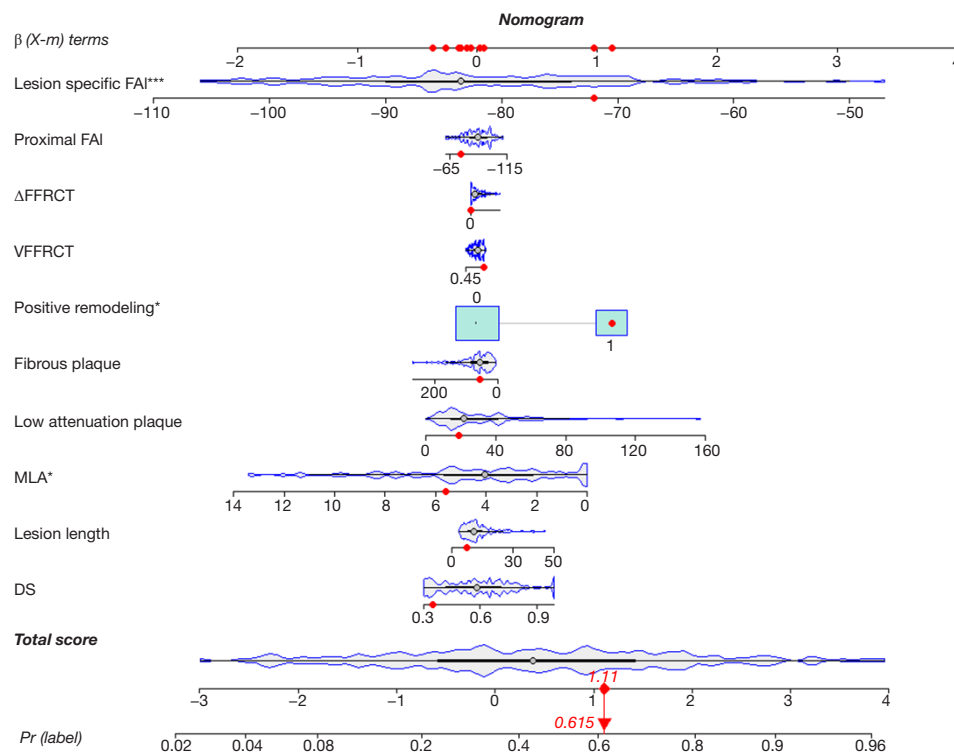


Figure 4 Predicted nomogram of culprit lesions that lead to ACS in the future. The red dot shows a 60-year-old male with a proximal LCX lesion. The nomogram indicated a DS of 35%, lesion length of 7.4 mm, MLA of 5.6 mm², LAP volume of 18.9 mm³, fibrous plaque volume of 57.8 mm³, RI \geq 1.1, VFFRCT of 0.95, Δ FFRCT of 0.01, proximal FAI of -74, lesion specific FAI of -72 and total score of 1.11. It was predicted that the lesion has a 0.615 chance of becoming a culprit lesion. In this case, the lesion became the culprit lesion of ACS after 512 days. In positive remodeling, 0 represents RI <1.1, and 1 represents RI \geq 1.1. *, P=0.01; ***, P<0.001. DS, diameter stenosis; MLA, minimal lumen area; LAP, low attenuation plaque; ACS, acute coronary syndrome; LCX, left circumflex artery; FFRCT, computed tomography-derived fractional flow reserve; Δ FFRCT, Delta FFRCT; VFFRCT, vessel FFRCT; FAI, fat attenuation index; RI, remodeling index.

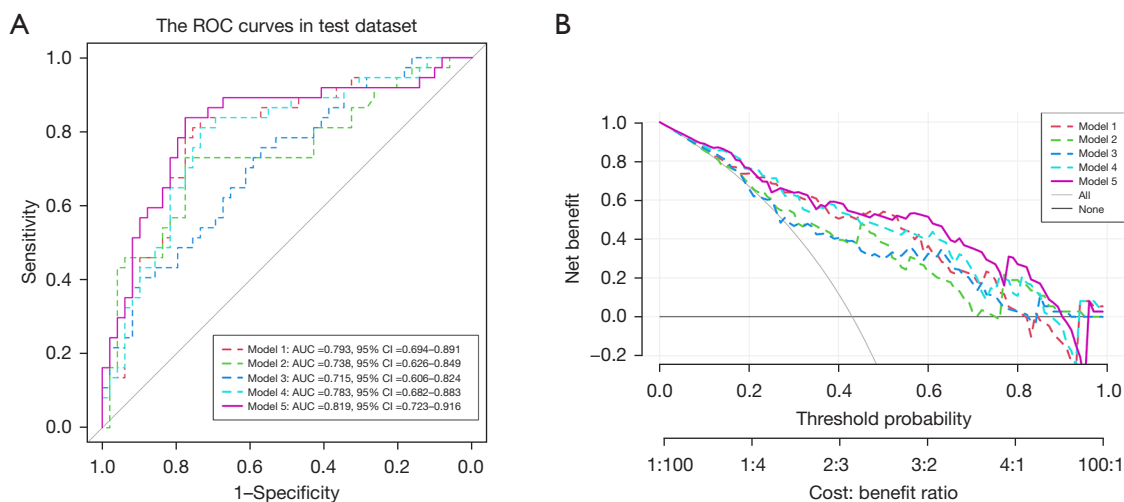


Figure 5 Comparison of different classification models for predicting culprit lesions in ACS. The ROC curve (A), DCA curve (B) and model annotations of the five models. Model 1 included plaque characteristics. Model 2 included hemodynamic parameters. Model 3 included PCAT attenuation. Model 4 included Model 1 plus hemodynamic parameters. Model 5 included Model 4 plus PCAT attenuation. ACS, acute coronary syndrome; ROC, receiver operating characteristic; DCA, decision curve analysis; PCAT, pericoronary adipose tissue; AUC, area under the curve.

lesion characteristics (9). Goeller *et al.* (26) reported that PCAT attenuation is increased around culprit lesions compared to nonculprit lesions, suggesting that FAI may help identify vulnerable plaques. Based on the level of the lesion, the present study measured the FAI of the proximal vessel where the lesion was located and the lesion-specific FAI to predict whether the lesion would become the culprit lesion for ACS. According to the logistic regression analysis, both proximal and lesion-specific FAI were risk factors for secondary ACS (proximal FAI: OR =1.03, P=0.04; lesion-specific FAI: OR =1.07, P<0.001), and the lesion-specific FAI had a higher value in predicting culprit lesions in the ML model (OR =1.1, P<0.001).

Plaque characteristics, hemodynamic parameters and PCAT attenuation all reflect the characteristics of lesions and provide corresponding clinical information for disease prediction. These parameters are all noninvasive parameters and do not require additional invasive examinations, thereby reducing harm to patients. In the present study, the plaque characteristics model (Model 1) outperformed Model 2 and Model 3, which may be due to the excessive number of parameters included in the plaque characteristics category. To the best of our knowledge, this study is the first to propose using ML combined with three-category CTA parameter characteristics to predict ACS culprit lesions based on lesion level. The present study investigated

the direct correlation between the CTA parameter characteristics of each lesion and the culprit lesion to improve the identification of culprit lesions in patients prone to ACS. Early identification of culprit lesions will aid in timely preventive measures and interventions for treatment.

Limitations

The present study had some limitations. First, the present study was limited by retrospective study data, which may lead to inevitable bias. Further efforts to collect prospective data are necessary. Second, this was a single-center, single-vendor study. The prediction of ACS by different image acquisition parameters and different computed tomography scanners requires further study. Third, due to technical limitations, we measured the lesion-specific FAI in an area including 2 mm of vessel wall expansion, and it is necessary to exclude the 1 mm area around the vessel wall (which may include the effect of the eccentric plaque) for further validation. Fourth, the ACS patients in the present mainly had unstable angina pectoris, indicating that additional patients with culprit lesions of myocardial infarction need to be verified in the future. Fifth, the present study analyzed ACS culprit lesions, and due to the limited number of patients, we were unable to analyze the CTA parameter

characteristics for UA, NSTEMI, and STEMI subgroups to predict disease, indicating that further studies are needed. Sixth, the retrospective nature of the present study made it difficult to control the status of drug use from early CTA examination to ACS. However, changes in drug therapy during the clinical process were based on the actual patient situation, which is uncontrollable and unavoidable.

Conclusions

Using machine learning based on CTA parameters can predict ACS. Compared to other combined models, the model combining plaque characteristics, hemodynamic parameters and PCAT attenuation performed best in predicting culprit lesions of ACS.

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Footnote

Reporting Checklist: The authors have completed the TRIPOD reporting checklist. Available at <https://qims.amegroups.com/article/view/10.21037/qims-22-1045/rc>

Conflicts of Interest: All authors have completed the ICMJE uniform disclosure form (available at <https://qims.amegroups.com/article/view/10.21037/qims-22-1045/coif>). MZ is a current employee of GE Healthcare. The other authors have no conflicts of interest to declare.

Ethical Statement: The authors are accountable for all aspects of the work in ensuring that questions related to the accuracy or integrity of any part of the work are appropriately investigated and resolved. The study was conducted in accordance with the Declaration of Helsinki (as revised in 2013). The study was approved by the Medical Ethics Committee of The Fourth Affiliated Hospital,

Harbin Medical University (No. 2022-SCILLSC-11), and individual consent for this retrospective analysis was waived.

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Appendix 1 CTA interpretation and ICA analysis

Considering that the interval between CTA and ICA was too short to demonstrate predictive value, we excluded patients with an interval of less than 3 months. All scanned datasets were subjected to curved projection reformation and volume reformation through a dedicated postprocessing workstation (Vitrea, version 7.6; Vital Images). The CTA dataset was evaluated by two local observers with extensive experience in cardiac imaging who were unaware of the patient's clinical information, and lesions with DS $\geq 30\%$ were included in subsequent studies. ICA was performed by two experienced interventional cardiologists according to local criteria and identified culprit and nonculprit lesions. If there were culprit lesions on one vessel, the most severe stenosis was selected as the measurement lesion of the blood vessel. Thus, the culprit lesion also represented the culprit vessel.

Coronary plaque analysis

The MLA was the narrowest luminal area of the plaque. The distance from the ostium was defined as the distance from the narrowest point of the plaque to the opening of the vessel. Spotty calcification was defined as calcifications < 3 mm in diameter on multiple reconstructed images.

Regarding the definition of plaque components, plaques with CT attenuation < 30 Hounsfield units (HU) were defined as LAP. CT values between 30 and 149 HU were defined as FP, and CT values ≥ 150 HU were defined as CP. TP was calculated using the following formula: TP = CP + noncalcified plaque (NCP); where NCP = LAP + FP volume. Wall-to-lumen volume ratio was calculated using the following formula: wall-to-lumen volume ratio = wall volume/lumen volume; where the wall is the space between the inner and outer contours, the wall volume is the vessel volume minus the lumen volume and the vessel volume is the volume within the outer wall contour of the affected segment of the lesion. The remodeling index (RI) was the ratio of the vessel area of the lesion (the area within the outer contour) divided by the vessel area of the proximal reference point, with positive remodeling when $RI \geq 1.1$. Plaque burden was calculated using the following formula: plaque burden = plaque volume $\times 100\%$ / vessel volume.

Analysis of hemodynamic parameters based on CFD

For the hemodynamic analysis, a software model based on the principles of computational fluid dynamics (CFD) (Shukun Technology) was used as described previously, and the calculation of fractional flow reserve was performed by an independent blinded analyst on a conventional CTA dataset. The software calculated the ratio of coronary pressure drop (Pd) across a stenosis to intra-aortic pressure (Pa) as a surrogate measure of ischemia and allowed physicians to create a patient-specific coronary vascular tree model. FFRCT and VFFRCT ≤ 0.8 were considered abnormal. Vessels were excluded from the analysis when the vessel diameter was less than 1.5 mm for which FFRCT could not be calculated.

Machine learning

With the rapid development of artificial intelligence in the field of medical imaging, machine learning (ML) has been introduced into cardiovascular imaging as a field of computer science, helping clinicians diagnose diseases more quickly and accurately as well as helping clinicians to perform risk assessment and outcome prediction with high efficiency. In the present study, noninvasive parameters from CTA were used in combination with ML to improve the ability of outcome prediction. The predictive model of ACS was constructed based on the following ten risk factors: DS, lesion length, MLA, low attenuation plaque, fibrous plaque, positive remodeling, VFFRCT, Δ FFRCT, proximal FAI and lesion-specific FAI. The odds ratio of each parameter in the model is shown in *Figure 1*.

Logistic regression (LR), random forest (RF), Bayesian and K-nearest neighbor (KNN) algorithms were applied to build models. These algorithms can learn from the training set data to achieve the purpose of performing a given task and use the test set with no time overlap with the training set to validate the accuracy of the trained machine learning model.

Predictive value of machine learning for ACS

As an algorithmic tool, ML has been frequently used in medical research in recent years. We used ML to predict ACS in coronary artery disease and obtained good prediction results. During this process, we built the model using four ML algorithms to make the model predictions the best. In the present results, the ROC curve and DCA curve of the RF model in the training set were significantly higher than those in the test set (AUC: 0.990 [95% CI: 0.976-1] vs. 0.754 [95% CI: 0.739-0.878]). Because the difference was large, the RF model was rejected. If the branch of the decision tree model grows to far in the RF model, it may find irregularities in the training dataset, resulting in overfitting.

The final results showed that compared to the other candidate models in machine learning, the LR model provided better predictive performance in terms of discrimination and decision-making ability. Therefore, the ML model was a combined model based on the LR algorithm. At the same time, the prediction results of the ML combined model (Model 5) were better than those of the traditional classification prediction models (Models 1-4), but Model 1 had better prediction results than Model 2 and Model 3 in the single-classification model comparison, which may be due to the inclusion of too many parameters in the classification of plaque characteristics.

Variable	N	Odds ratio	p
DS	154	4.84 (0.22, 110.01)	0.32
Lesion.length	154	1.02 (0.90, 1.15)	0.78
MLA	154	0.81 (0.68, 0.95)	0.01
Low.attenuation.plaque	154	1.01 (0.98, 1.05)	0.35
Fibrous.plaque	154	1.00 (0.98, 1.02)	0.77
Positive.remodeling	0 100	Reference	
	1 54	3.06 (1.32, 7.37)	0.01
VFFRCT	154	1.35 (0.02, 96.86)	0.89
Δ FFRCT	154	1.85 (0.01, 592.75)	0.83
Proximal.FAI	154	0.99 (0.94, 1.04)	0.69
Lesion.specific.FAI	154	1.10 (1.05, 1.16)	<0.001

Figure S1 The risk of each parameter in the model built by machine learning. In positive remodeling, 0 represents RI <1.1, and 1 represents RI \geq 1.1. DS: diameter stenosis, MLA: minimal lumen area, FFRCT: computed tomography-derived fractional flow reserve, VFFRCT: vessel FFRCT, Δ FFRCT: Delta FFRCT, FAI: fat attenuation index, RI: remodeling index.

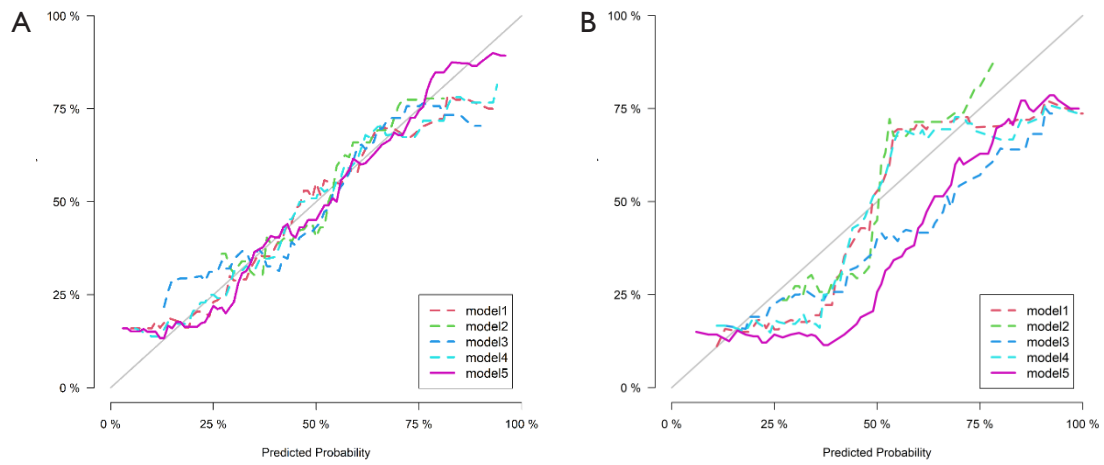


Figure S2 Calibration curves of different combination models in the training set (A) and test set (B). Model 1 includes plaque characteristics. Model 2 includes hemodynamic parameters. Model 3 includes PCAT attenuation. Model 4 includes plaque characteristics, hemodynamic parameters. Model 5 includes plaque characteristics, hemodynamic parameters and PCAT attenuation. Among the models, Model 5 was best calibrated in the training set and better calibrated in the test set. PCAT: pericoronary adipose tissue.