



The impact of paramagnetic rim lesions on cortical thickness and gray to white matter contrast in relapsing-remitting multiple sclerosis

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Background: Paramagnetic rim lesions (PRLs) on susceptibility magnetic resonance sequences have been suggested as an imaging marker of disease progression in multiple sclerosis. This retrospective cross-sectional study aimed to investigate the impact of PRLs on cortical thickness and gray matter (GM) to white matter (WM) contrast in relapsing-remitting multiple sclerosis (RRMS).

Methods: A total of 82 RRMS patients (40 patients with at least 1 PRL and 42 patients without PRL) and 43 healthy controls (HC) were included in this study. The T1-weighted images (T1WI) were processed with the FreeSurfer pipeline. GM to WM signal intensity ratio (GWR) was obtained from T1WI by dividing the GM signal intensity by the WM signal intensity for each vertex. Group differences in cortical thickness and GWR were tested on reconstructed cortical surface.

Results: Compared to HC, patients with PRL had thinner mean cortical thickness ($P<0.001$), higher mean GWR ($P=0.001$), and lower brain structure volumes (cortex volume, $P=0.001$; WM volume, $P<0.001$; deep GM volume, $P<0.001$). Vertex-based analysis found significant cortical thinning in several regions and increased GWR in a wider range of regions in patients with PRL. The two types of clusters had both overlapping regions and independent regions. However, in patients without PRL, only a few regions showed significant cortical thickness changes. Correlation analysis found that in patients with PRL, only PRL volume showed a significant negative correlation with mean cortical thickness ($P=0.048$), and PRL volume and count, non-PRL count, and total lesion volume were significantly and positively correlated with mean GWR ($P<0.05$).

Conclusions: There were significant changes in cortical thickness, GWR, and brain structure volume in RRMS patients with PRL that may contribute to further understanding of the pathological mechanisms underlying neurological tissue damage.

Keywords: Multiple sclerosis; paramagnetic rim lesion (PRL); cortical thickness; gray matter; tissue contrast

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Introduction

Multiple sclerosis (MS) is a disease characterized by inflammatory demyelinating lesions in the central nervous system (CNS) that cause structural and functional changes in the brain, including extensive cortical thinning, deep gray matter (DGM) atrophy, and abnormal functional connectivity (1-3). The cascade pathology of MS lesions leads to changes in neurons and microenvironment causing changes in gray matter (GM) and white matter (WM). Retrograde and anterograde degeneration resulting from focal axon transection and tissue damage caused by lesions may be the main contributors to morphological changes in the brain.

The pathophysiological mechanisms described above lead to structural changes in the brain that could be demonstrated by structural magnetic resonance imaging (MRI). Several previous studies have analyzed cortical thickness in MS patients and found cortical thinning in multiple regions, which could indicate the extent of neurodegenerative damage in patients with MS (4-7). However, detectable cortical thinning indicates that the damage is already in an irreversible state, so we hoped to find imaging metrics that are more sensitive to reflect structural brain damage.

In recent years, a relatively new method of measuring structural brain damage, which quantifies disease severity by focusing on the GM to WM signal intensity ratio (GWR), has been investigated in many diseases (8-10). The T1 relaxation time is influenced by the microstructural properties of the tissue and the cellular water/lipid content, thus exhibiting differences in T1 signal intensity between tissues, namely, low signal in GM and high signal in WM (11). Pathological processes in MS such as myelin degradation, axonal loss, and iron deposition affect tissue microstructure or cellular content and therefore lead to alterations in local or global T1 relaxation time (12,13). Contrast changes at the gray and WM borderline may be consistent with the pathological processes described above (14). Thus, GWR appears to sensitively reflect the pathophysiological changes of brain tissue in the early stages of disease progression and may reflect pathological mechanisms that precede the onset of cortical atrophy (15).

Relapsing-remitting MS (RRMS) is the most common MS subtype, but due to pathological heterogeneity, RRMS patients showed significant differences in imaging manifestations, treatment response, and prognosis (16,17). The accurate classification of RRMS is helpful for clinicians

to develop treatment options, which meets the current clinical needs. A subset of MS lesions is defined as chronic active lesions surrounded by activated macrophages and iron-rich microglia (18). Such lesions, which are confirmed by combined MRI/histopathologic studies to exhibit paramagnetic rim lesions (PRLs) on susceptibility magnetic resonance (MR) sequences, are associated with persistent neuroinflammation and tissue damage, leading to more severe disability (19). Therefore, investigating the impact of PRL on structural brain damage in RRMS patients could help to classify RRMS and assess the impact of persistent damage on pathophysiological changes in the brain.

In this study, we hypothesized that RRMS patients with PRL would have different degrees of structural brain alterations compared to patients without PRL. By comparing GWR and cortical thickness in patients with and without PRL, we hoped to find imaging metrics that would be sensitive to cortical damage in RRMS patients. Furthermore, we aimed to investigate whether the presence of PRL implies more severe cortical damage, which could contribute to the classification and precise treatment of RRMS patients. We present this article in accordance with STROBE reporting checklist (available at <https://qims.amegroups.com/article/view/10.21037/qims-23-1395/rc>).

Methods

Patient population

This retrospective study was conducted in accordance with the Declaration of Helsinki (as revised in 2013). This study was approved by the Institutional Review Board of Tongji Hospital affiliated with Tongji Medical College of Huazhong University of Science and Technology (ethical approval number: TJ-IRB202303157) and written informed consent was provided by all patients.

The inclusion criteria were patients who: (I) were diagnosed as RRMS, (II) had undergone MRI examinations that included T2 fluid-attenuated inversion recovery (FLAIR) images, T1-weighted images (T1WI), and 3-dimensional (3D) multi-echo gradient echo (mGRE) images, and (III) had not received steroid therapy within 4 weeks before the MRI scan. The Expanded Disability Status Scale (EDSS) scores were used clinically to assess the degree of disability. From May 2014 to May 2023, a total of 102 RRMS patients met the inclusion criteria. We excluded 20 patients according to the following exclusion criteria: (I) younger than 18 years old (n=6),

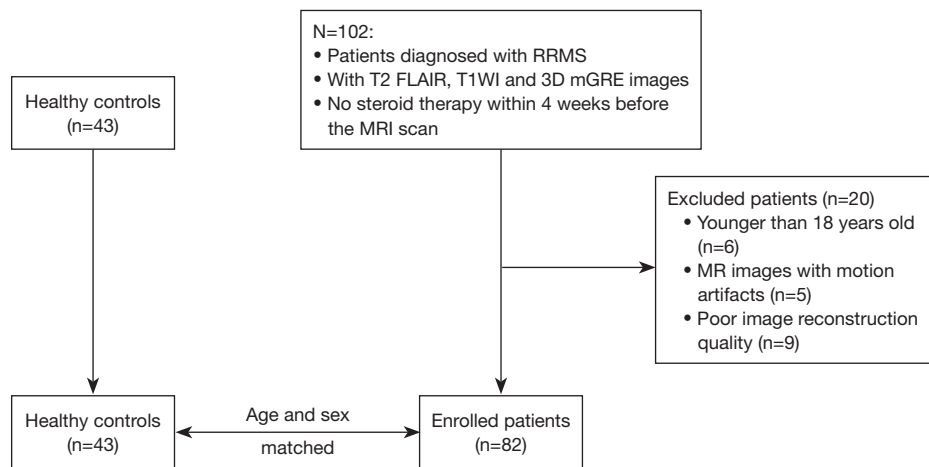


Figure 1 Flowchart showing participant selection criteria. RRMS, relapsing-remitting multiple sclerosis; FLAIR, fluid-attenuated inversion recovery; T1WI, T1-weighted images; mGRE, multi-echo gradient echo; MRI, magnetic resonance imaging; MR, magnetic resonance.

(II) MR images with motion artifacts ($n=5$), and (III) poor image reconstruction quality ($n=9$). Ultimately, 82 RRMS patients were included in the study. Healthy volunteers who underwent the physical examination at the hospital during the same period were recruited as the control group. Based on conventional MRI, healthy controls (HC) had no CNS diseases such as cerebrovascular disease, demyelinating and neurodegenerative diseases, brain tumor, or trauma. A total of 43 age- and gender-matched HC were included in the study. The flowchart for participant selection criteria is shown in *Figure 1*.

Image acquisition

MR images were obtained on a 3T MR scanner (Discovery MR750; GE Medical Systems, Waukesha, WI, USA) with a 32-channel head coil. The 3D T1WI before gadolinium-based contrast injection was acquired using the BRAIn Volume (BRAVO) sequence with the following parameters: repetition time (TR)/echo time (TE) = 8.16/3.18 ms, number of excitation (NEX) = 1, matrix = 256×256 , slice thickness = 1 mm, slice spacing = 1 mm, and field of view (FOV) = 256×256 mm². The acquisition parameters for 3D T2 FLAIR were as follows: TR/TE = 5,000/117 ms, NEX = 1, matrix = 256×256 , slice thickness = 1 mm, slice spacing = 1 mm, and FOV = 256×256 mm². The 3D mGRE was obtained with the following parameters: FOV = 240×240 mm², TR = 42.8 ms, TE1/ Δ TE = 4.5/4.9 ms, number of TEs = 8, matrix = 416×320 , readout bandwidth = 244 Hz/pixel, slice thickness = 2 mm, and flip angle = 20°.

Data processing

The reconstruction of quantitative susceptibility mapping (QSM) involved several steps. Firstly, nonlinear field map estimation was employed, followed by graph-cut-based phase unwrapping to estimate the total field (20). Subsequently, background field removal was performed using projection onto dipole fields (PDF) to obtain the local tissue field (21). The local field was then inverted using the morphology-enabled dipole inversion with automatic uniform cerebrospinal fluid (CSF) zero reference (MEDI+0) algorithm, which allowed for the determination of susceptibility distribution. To achieve this, the tissue field was deconvolved with the dipole kernel using Bayesian machine learning techniques (22). In this algorithm, the susceptibility value for the average ventricular CSF was set to zero (23).

The presence of PRL was determined by visual consensus between 2 neuroradiologists (with 5 and 13 years of experience, respectively) regarding the presence of a hyperintense rim completely or partially surrounding the edge of the chronic lesion on the QSM, visible on at least 2 contiguous sections. When there was a disagreement, a third neuroradiologist (with 10 years of experience) who was unaware of previous choice was called on to determine the lesion type. To exclude the influence of partial volume effects, only lesions ≥ 5 mm were included in the study (24). Then RRMS patients were divided into the PRL group and the non-PRL group based on the presence or absence of PRL.

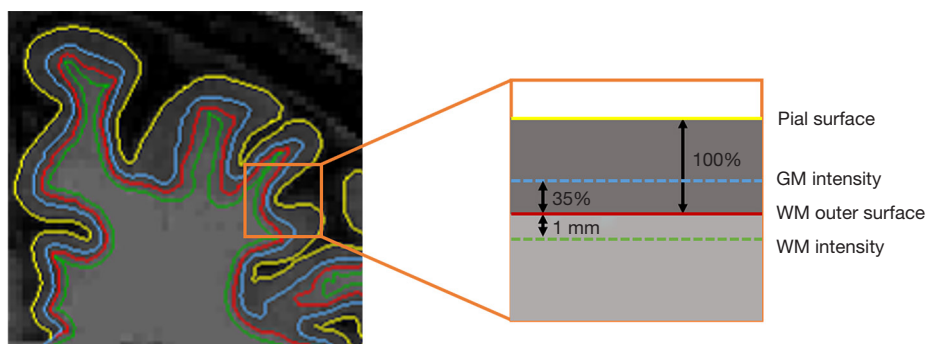


Figure 2 Schematic diagram for calculating GWR. The signal intensity of the GM was sampled from 35% of the total cortical thickness near the GM/WM boundary (blue surface), and the signal intensity of the WM was sampled at a constant distance of 1 mm subjacent to gray/white boundary of the surface (green surface). The GWR was calculated by dividing the GM signal intensity by the WM signal intensity. GM, gray matter; WM, white matter; GWR, GM to WM signal intensity ratio.

T2 FLAIR images were co-registered to the 3D T1WI. Lesions on T2 FLAIR and 3D T1WI were segmented by the Lesion Growth Algorithm (LGA) in the Lesion Segmentation Toolbox (LST) in SPM12 (<https://www.fil.ion.ucl.ac.uk/spm/>), with the Kappa value set to 0.3 (7,25,26). The segmented probability map was checked by a neuroradiologist (with 5 years of experience) and manual corrections were made for any inaccuracies. Then the segmented probability map of the lesion was used for lesion filling of T1WI by the “lesion filling” function of LST. The images were corrected for intensity nonuniformity prior to reconstruction of the cortical surface to reduce the effect of B1 and coil profile-induced nonuniformity (15). The T1WI were processed using the FreeSurfer (package 7.1.1; <http://surfer.nmr.mgh.harvard.edu>), to automatically reconstruct the cortical surface and measure the cortical thickness of the entire brain. We visually examined the cortical surface reconstructions of each participant without knowledge of any clinical outcomes and made manual corrections where necessary. Cortical thickness was defined as the closest distance from the gray/white boundary to the gray/CSF boundary at each vertex. We also recorded the volumes of cortex, WM, and DGM segmented by FreeSurfer. To correct for the difference in head size, the brain region volume of the participant was divided by the total intracranial volume (TIV) of that participant as a normalization process. Therefore, the normalized brain structure volumes were calculated in patients with PRL, patients without PRL, and HC, respectively.

GWR was calculated from the signal intensity of T1WI as another measure to assess pathophysiological changes

in RRMS patients. The signal intensity of the GM was sampled from 35% of the total cortical thickness near the GM/WM boundary, and the signal intensity of the WM was sampled at a constant distance of 1 mm subjacent to gray/white boundary of the surface (Figure 2) (27). The GWR for each vertex was obtained by dividing the signal intensity of the GM by the signal intensity of the WM. Similar to previous studies (8,10,14), whole-brain surface maps of cortical thickness and GWR were registered to the surface of the template and smoothed using a kernel with full-width-half-maximum (FWHM) of 10 mm.

Statistical analyses

The Chi-square test, one-way analysis of variance (ANOVA) test, and Mann-Whitney U test were used to compare the differences in clinical characteristics between groups. General linear model analysis with gender and age as covariates was used to compare differences in brain morphometric metrics (mean cortical thickness, mean GWR, normalized cortex volume, normalized WM volume, and normalized DGM volume) between the PRL group, the non-PRL group, and the HC group. Statistical difference maps were generated between the PRL group, the non-PRL group, and the HC group by comparing cortical thickness and GWR based on vertex-by-vertex general linear model analysis in FreeSurfer, using gender and age as covariates. Monte Carlo permutation cluster analysis ($P < 0.05$) with 1,000 permutations was applied for multiple comparisons correction. Finally, partial correlation analysis controlling for gender and age was used to analyze the relationship between MRI metrics (mean cortical thickness and GWR)

Table 1 Clinical characteristics of the participants

Metrics	PRL group (n=40)	Non-PRL group (n=42)	HC group (n=43)	P value
Gender, female	24 (60.0)	30 (71.4)	27 (62.8)	0.525 ^a
Age, years	38.35±10.72	33.43±10.91	34.26±10.47	0.089 ^b
Disease duration, years	4.00 (0.35, 8.00)	2.00 (0.23, 5.19)	–	0.138 ^c
EDSS	3.25 (2.00, 5.00)	3.00 (2.00, 3.50)	–	0.155 ^c
Total lesion volume, mL	13.162 (3.817, 19.949)	1.645 (0.416, 6.012)	–	<0.001 ^c
PRL count	3 (2, 10)	–	–	–
PRL volume, mL	1.461 (0.664, 5.029)	–	–	–
Non-PRL count	34 (16, 58)	9 (3, 14)	–	<0.001 ^c
Non-PRL volume, mL	7.416 (2.479, 14.358)	1.645 (0.416, 6.012)	–	<0.001 ^c

Data are presented as n (%), mean ± SD or median (IQR). ^a, the P value was obtained by the Chi-square test; ^b, the P value was obtained by one-way analysis of variance test; ^c, the P value was obtained by Mann-Whitney U test. PRL, paramagnetic rim lesion; HC, healthy controls; EDSS, Expanded Disability Status Scale; SD, standard deviation; IQR, interquartile range.

and clinical characteristics in the PRL group. $P < 0.05$ was considered statistically significant.

Results

Demographic and clinical characteristics

Table 1 shows the general characteristics of the participants. There were no participants with missing data for each variable of interest. There were 40 patients in the PRL group [PRL volume, median: 1.461 mL, interquartile range (IQR): 0.664–5.029 mL; non-PRL volume, median: 7.416 mL, IQR: 2.479–14.358 mL] and 42 patients in the non-PRL group (non-PRL volume, median: 1.645 mL, IQR: 0.416–6.012 mL). The PRL group had a larger total lesion volume and non-PRL volume compared to the non-PRL group ($P < 0.001$, $P < 0.001$, respectively). There was no statistically significant difference in gender and age among the PRL group, the non-PRL group, and the HC group ($P = 0.525$, $P = 0.089$, respectively). Moreover, there was no significant difference in disease duration and EDSS between the PRL group and the non-PRL group ($P = 0.138$, $P = 0.155$, respectively).

Mean cortical thickness and mean GWR and brain structure volume analysis

Compared to HC, the PRL group exhibited thinner mean cortical thickness and higher mean GWR ($P < 0.001$, $P = 0.001$). Furthermore, patients with PRL showed

significant reductions in normalized cortex volume, WM volume, and DGM volume ($P = 0.001$, $P < 0.001$, $P < 0.001$, respectively). Compared to HC, the non-PRL group had higher GWR and lower normalized DGM volume ($P = 0.019$, $P = 0.016$). In addition, significant differences in normalized WM volume and DGM volume were observed between patients with and without PRL ($P = 0.005$, $P = 0.001$) (Figure 3).

Cortical thickness analysis

RRMS patients with PRL showed multiple regional cortical thinning in the left and right hemispheres compared to HC (Figure 4). Table 2 summarizes the regions with significant cortical thinning. Certain regions, such as the parahippocampal, superior temporal, and fusiform, demonstrated symmetrical cortical thinning in the bilateral hemispheres, whereas other regions exhibited unilateral cortical thinning in each hemisphere. For example, the superior frontal was more affected in the left hemisphere, and the entorhinal in the right hemisphere showed regional cortical thinning. When comparing the non-PRL group to the HC group, significantly thinner cortical thickness was observed in the left superior frontal [cluster-wise P-value (CWP) = 0.038, cluster size of 221.19 mm²] and rostral middle frontal (CWP = 0.047, cluster size of 197.91 mm²) regions (Table S1). Only right parahippocampal showed significant cortical thinning in the PRL group compared to the non-PRL group (CWP = 0.020, cluster size of 282.55 mm²) (Table S2).

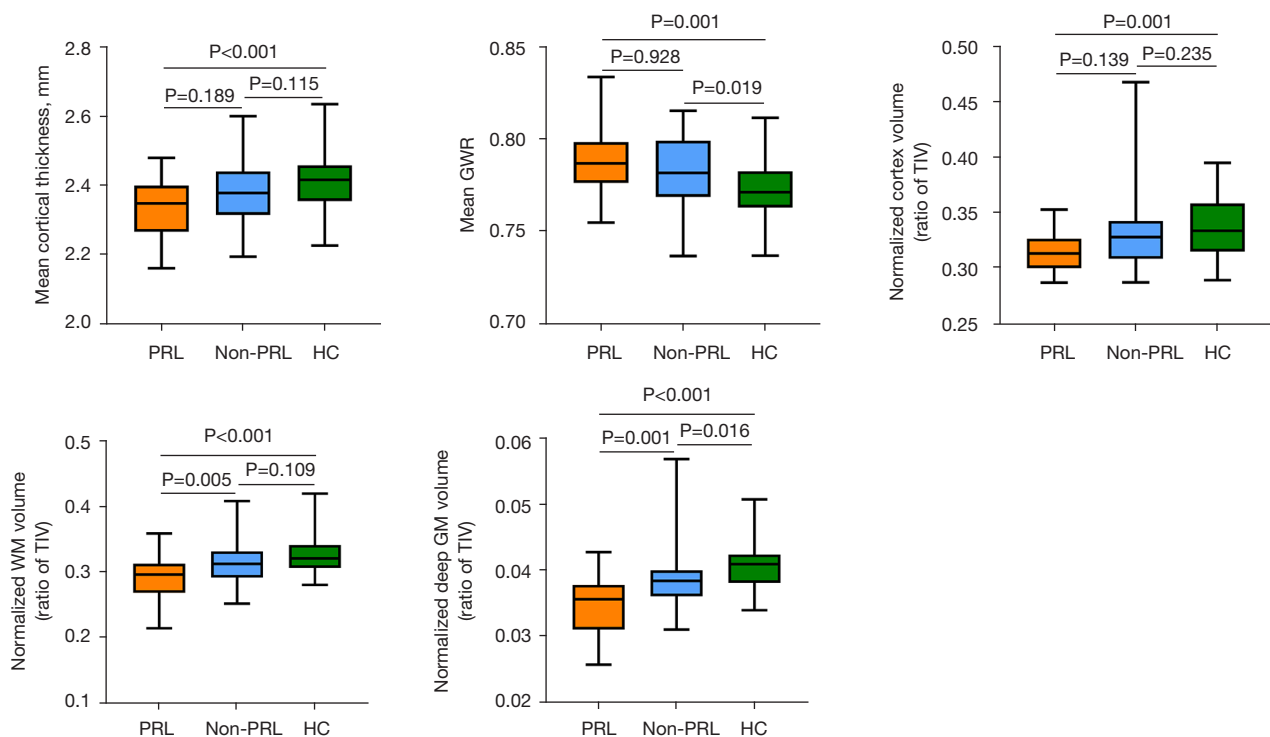


Figure 3 Comparison of mean cortical thickness, mean GWR, and normalized brain structure volume among PRL group, non-PRL group and HC group. PRL, paramagnetic rim lesion; HC, healthy controls; GWR, GM to WM signal intensity ratio; TIV, total intracranial volume; WM, white matter; GM, gray matter.

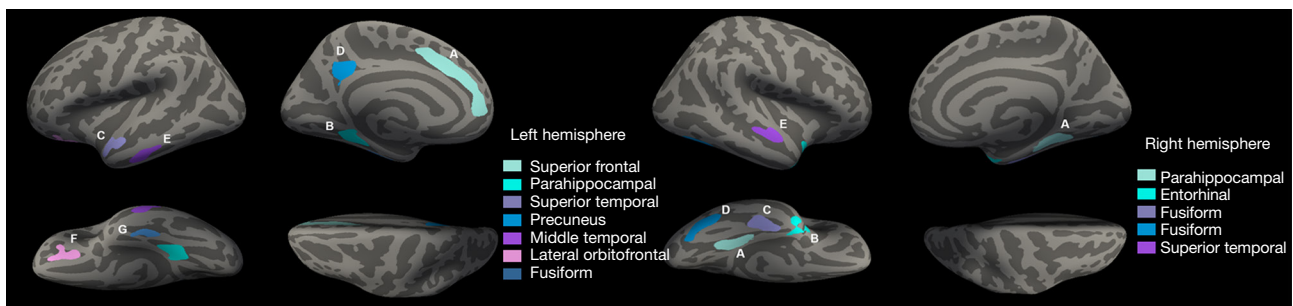


Figure 4 The regions with cortical thinning in the left and right hemispheres in the PRL group compared to the HC group. The highlighted regions in left hemisphere are: (A) superior frontal, (B) parahippocampal, (C) superior temporal, (D) precuneus, (E) middle temporal, (F) lateral orbitofrontal, (G) fusiform. The highlighted regions in right hemisphere are: (A) parahippocampal, (B) entorhinal, (C,D) fusiform, (E) superior temporal. PRL, paramagnetic rim lesion; HC, healthy controls.

GWR analysis

The PRL group exhibited extensive regions with increased GWR in the bilateral hemispheres when compared to the HC group (Figure 5). Table 3 summarizes the regions displaying significant increase in GWR. In the left hemisphere, clusters of increased GWR were located in

the fusiform, isthmus of cingulate, superior frontal, and pericalcarine. In the right hemisphere, clusters of increased GWR were located in the parahippocampal, isthmus of cingulate, superior frontal, and pars opercularis. In the comparison of the non-PRL group with the HC group, no significant region of increased GWR was found in either

Table 2 Regions with cortical thinning in the PRL group relative to the HC group

PRL group vs. HC group	Size (mm ²)	Talairach coordinates			CWP
		x	y	z	
Left superior frontal	1,030.00	-12.1	20.1	35.8	0.002
Left parahippocampal	517.18	-33.9	-38.2	-11.9	0.002
Left superior temporal	423.17	-50.0	-5.9	-18.1	0.002
Left precuneus	403.18	-14.8	-50.1	31.6	0.004
Left middle temporal	346.92	-55.0	-21.0	-24.2	0.006
Left lateral orbitofrontal	333.77	-20.3	22.9	-16.6	0.006
Left fusiform	214.68	-40.2	-23.5	-21.6	0.042
Right parahippocampal	593.00	34.4	-35.9	-13.0	0.002
Right entorhinal	488.18	27.7	3.0	-33.7	0.006
Right fusiform	466.03	41.9	-17.6	-22.8	0.006
Right fusiform	450.45	40.3	-64.4	-12.5	0.008
Right superior temporal	373.70	55.4	-6.6	-9.9	0.014

PRL, paramagnetic rim lesion; HC, healthy controls; CWP, cluster-wise P-value.

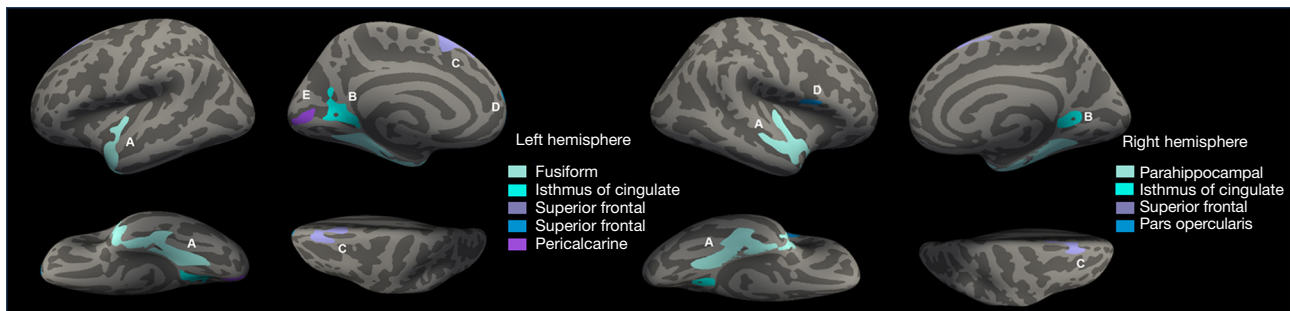


Figure 5 The regions with increased GWR in the left and right hemispheres in the PRL group compared to the HC group. The highlighted regions in left hemisphere are: (A) fusiform, (B) isthmus of cingulate, (C, D) superior frontal, (E) pericalcarine. The highlighted regions in right hemisphere are: (A) parahippocampal, (B) isthmus of cingulate, (C) superior frontal, (D) pars opercularis. GWR, GM to WM signal intensity ratio; PRL, paramagnetic rim lesion; HC, healthy controls; WM, white matter; GM, gray matter.

hemisphere. It is worth noting that some regions in the PRL group showed higher GWR compared to the non-PRL group, including left parahippocampal, right lingual, and entorhinal (Figure S1, Table 4).

Combined cortical thickness and GWR analysis

In order to visually assess the co-localization of cortical thickness changes and GWR changes, we put the clusters with thinner cortical thickness or higher GWR in the PRL group compared to the HC group in the same

inflated brain (Figure 6). The regions displaying increased GWR were more extensive than those exhibiting cortical thinning. Notably, there were regions in both hemispheres where cortical thinning and increased GWR overlapped. Furthermore, certain regions demonstrated either cortical thinning or increased GWR exclusively.

Correlation analysis between MRI metrics and clinical characteristics

Table 5 shows the results of the correlation analysis between

Table 3 Regions with increased GWR in the PRL group relative to the HC group

PRL group vs. HC group	Size (mm ²)	Talairach coordinates			CWP
		x	y	z	
Left fusiform	3,216.89	-35.1	-43.2	-9.8	0.002
Left isthmus of cingulate	859.63	-19.2	-49.8	0.2	0.002
Left superior frontal	669.82	-17.0	33.4	49.3	0.004
Left superior frontal	388.54	-16.6	60.8	4.9	0.020
Left pericalcarine	368.86	-12.0	-83.4	2.4	0.024
Right parahippocampal	3,527.08	34.0	-43.9	-7.6	0.002
Right isthmus of cingulate	412.90	20.0	-47.8	0.0	0.016
Right superior frontal	338.44	16.8	22.5	54.1	0.022
Right pars opercularis	213.13	52.1	10.2	2.4	0.047

GWR, GM to WM signal intensity ratio; PRL, paramagnetic rim lesion; HC, healthy controls; CWP, cluster-wise P-value; GM, gray matter; WM, white matter.

Table 4 Regions with increased GWR in the PRL group relative to the non-PRL group

PRL group vs. non-PRL group	Size (mm ²)	Talairach coordinates			CWP
		x	y	z	
Left parahippocampal	254.82	-34.5	-41.2	-10.1	0.026
Right lingual	516.09	32.6	-45.6	-6.4	0.012
Right entorhinal	422.65	24.9	-10.6	-32.9	0.018

GWR, GM to WM signal intensity ratio; PRL, paramagnetic rim lesion; CWP, cluster-wise P-value; GM, gray matter; WM, white matter.

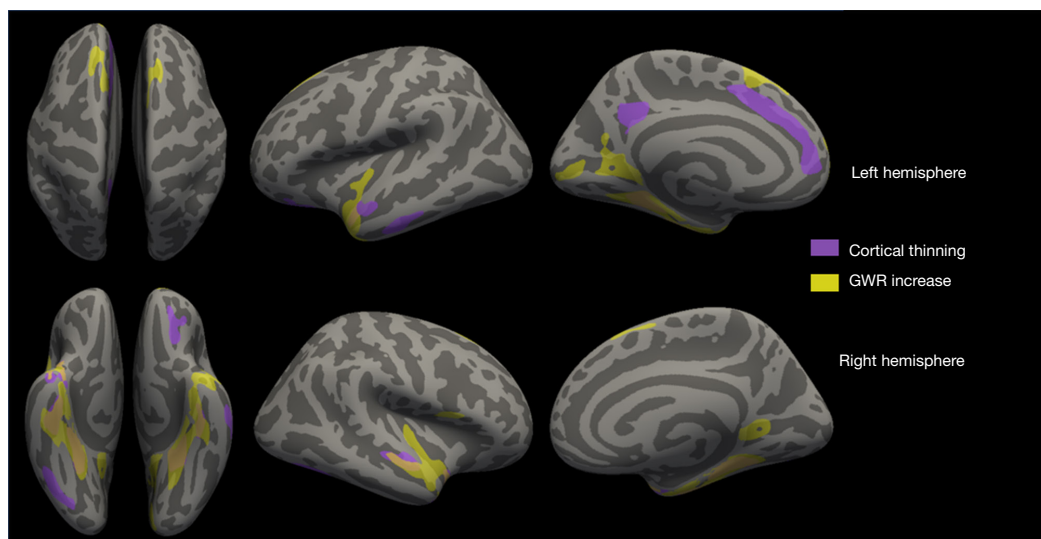


Figure 6 Inflated brain displaying regions of cortical thinning (purple regions) and regions of increased GWR (yellow regions) in the PRL group compared to the HC group. GWR, GM to WM signal intensity ratio; PRL, paramagnetic rim lesion; HC, healthy controls; WM, white matter; GM, gray matter.

Table 5 Correlation analysis for assessing the relationship between clinical characteristics and cortical thickness and GWR in the PRL group

Metrics	Mean cortical thickness		Mean GWR	
	r	P value	r	P value
PRL volume	-0.323	0.048	0.347	0.033
PRL count	-0.317	0.052	0.514	0.001
Non-PRL volume	0.011	0.948	0.291	0.076
Non-PRL count	-0.081	0.630	0.570	<0.001
Total lesion volume	-0.172	0.302	0.431	0.007
EDSS	-0.077	0.648	0.093	0.580
Disease duration	-0.145	0.384	0.034	0.841

r represents the partial correlation coefficient. GWR, GM to WM signal intensity ratio; PRL, paramagnetic rim lesion; EDSS, Expanded Disability Status Scale; GM, gray matter; WM, white matter.

mean cortical thickness and mean GWR and clinical characteristics in the PRL group. After controlling for gender and age, only PRL volume showed a significant negative correlation with mean cortical thickness ($r=-0.323$, $P=0.048$). There was a marginally negative correlation between PRL count and mean cortical thickness ($r=-0.317$, $P=0.052$). PRL volume, PRL count, non-PRL count, and total lesion volume exhibited a significant positive correlation with mean GWR ($r=0.347$, $P=0.033$; $r=0.514$, $P=0.001$; $r=0.570$, $P<0.001$; $r=0.431$, and $P=0.007$, respectively).

Discussion

In this study, we found that patients with PRL exhibited more significant cortical thinning, increased GWR, and structural brain atrophy. Vertex-based analysis revealed that RRMS patients with PRL showed significant cortical thinning in several regions and GWR increase in a wider range of regions. These two types of clusters displayed both overlapping and independent regions. In contrast, patients without PRL only showed some regions with cortical thinning. Correlation analysis further showed that only PRL volume was associated with mean cortical thickness in patients with PRL, whereas PRL volume, PRL count, non-PRL count, and total lesion volume were all positively correlated with mean GWR.

GWR, a relatively new MRI-based biomarker of tissue properties, shows potential in providing information about tissue damage caused by demyelinating lesions in the brain, complementing volumetric measurements. It has been used to reflect some of the pathologic mechanisms

of Alzheimer's disease, and manifested abnormality in some non-atrophic regions, which may reflect pathologic mechanisms that occur prior to cortical atrophy (8,15). In the present study, we observed several independent and co-localized regions of GWR abnormality and cortical thinning in RRMS patients with PRL. Notably, the extent of GWR abnormality appeared to be larger compared to cortical thickness abnormality. These findings suggest that GWR might serve as a more sensitive indicator of structural brain damage resulting from demyelination in the CNS. This metric has the potential to detect changes in microstructural properties that conventional cortical morphometry fails to capture. GWR reflects both pathological changes in the GM and subcortical WM. For example, demyelination, oligodendrocyte reduction, and axonal loss result in reduced WM signal intensity, whereas neuronal shrinkage and progressive neuronal loss lead to increased GM signal intensity, thus further resulting in higher GWR (28).

Numerous studies have investigated cortical changes in MS, but the underlying mechanisms of cortical atrophy are complex (29-31). Some studies have suggested that local cortical demyelination is the driving factor causing the loss of cortical tissue (32,33), whereas others have shown that degenerative damage caused by WM lesions plays a larger role in cortical atrophy (34-36). In contrast to previous research focusing on the impact of lesion location on the cortex, our study placed more emphasis on the damage to brain tissue caused by different lesion types. The PRLs were defined as chronic active MS lesions with iron-deposited microglia at the edge, and the release of toxins from these microglia to surrounding oligodendrocytes could limit

myelin regeneration in the lesion and further promote the demyelination process (37). Some studies have suggested that the presence of these lesions may lead to disease progression as well as functional impairment (24,38). Excess iron exacerbates oxidative stress, which, in turn, increases the release of inflammatory mediators by activating microglia and macrophages, resulting in demyelination and axonal damage (39,40). The above pathological alterations may be reflected in imaging indicators such as cortical thickness and GWR in RRMS patients with PRL.

There was also significant DGM atrophy and mean GWR increase as well as significant cortical thinning in a few regions in the non-PRL group compared to HC. However, patients without PRL appear to be the subtype of RRMS with relatively milder brain tissue damage compared to patients with PRL. A previous study reported greater lesion load and more severe brain atrophy in the PRL group than in the non-PRL group (38). MS patients with PRL had higher EDSS and pyramidal function system scores than MS patients without PRL (24). Consequently, it may be possible to classify RRMS patients based on the presence or absence of PRL, with special attention given to the patients with PRL who may exhibit more severe clinical disability.

According to the correlation analysis output, the PRL load played an important role in the cortical thickness development. Moreover, the increase of PRL load could also cause the increase of GWR. The changes observed in GWR may be attributed to Wallerian degeneration, retrograde neuroaxonal degeneration, and direct inflammatory damage to the lesion. The PRL which causes chronic progressive damage to brain tissue exacerbates these pathological processes, leading to altered signal intensity in GM and WM.

There were still some limitations in our study and we hope that this will stimulate future research endeavors to better understand and utilize GWR in the study of CNS demyelinating diseases. Firstly, our sample size was small, which limited our study to exploratory purposes only. Secondly, we only conducted cross-sectional studies to explore the impact of PRL on cortical thickness and GM to WM contrast in RRMS patients, and considered that GWR was a more sensitive indicator of pathological changes in the cortex and subcortical WM, which needs to be confirmed by longitudinal studies as well as pathological findings. In addition, there was a difference in the non-PRL volume between the PRL group and the non-PRL group, which may have impacted the outcome measures. Finally, our cohort included only RRMS, so conclusions about cortical

thickness and GWR may not be generalizable to patients with other types of MS.

Conclusions

Our study revealed regionally selective changes in GWR and cortical thickness specifically in RRMS patients with PRL, with the changes in GWR being more extensive. This suggests that GWR could serve as a significant biomarker for potential pathological changes in RRMS and provide further insights into the mechanisms of cortical damage caused by PRL. Moreover, the presence of PRL could potentially serve as a criterion for classifying RRMS, aiding in early and precise determination of the patient's brain injury pattern and facilitating personalized therapeutic interventions.

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Footnote

Reporting Checklist: The authors have completed the STROBE reporting checklist. Available at <https://qims.amegroups.com/article/view/10.21037/qims-23-1395/rc>

Conflicts of Interest: All authors have completed the ICMJE uniform disclosure form (available at <https://qims.amegroups.com/article/view/10.21037/qims-23-1395/coif>). All authors report this study has received funding from the National Natural Science Foundation of China (Grant Nos. U22A20354 and 81730049). The authors have no other conflicts of interest to declare.

Ethical Statement: The authors are accountable for all aspects of the work in ensuring that questions related to the accuracy or integrity of any part of the work are appropriately investigated and resolved. The study was conducted in accordance with the Declaration of Helsinki (as revised in 2013). The study was approved by the Institutional Review Board of Tongji Hospital affiliated with Tongji Medical College of Huazhong University of Science and Technology (ethical approval number: TJ-IRB202303157) and informed consent was provided by all individual participants.

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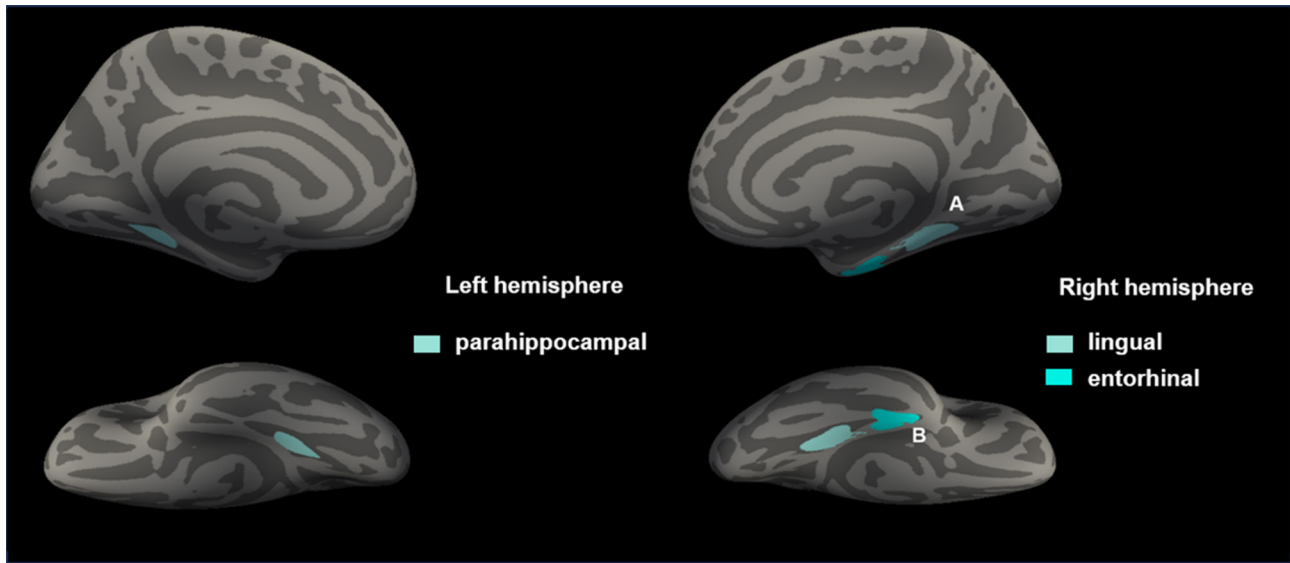


Figure S1 The regions with increased GWR in the left and right hemispheres in the PRL group compared to the non-PRL group. The highlighted region in left hemisphere is parahippocampal. The highlighted regions in right hemisphere are: (A) lingual, (B) entorhinal. GM, gray matter; WM, white matter; GWR, GM to WM signal intensity ratio; PRL, paramagnetic rim lesion.

Table S1 Regions with cortical thinning in the non-PRL group relative to the HC group

non-PRL group vs. HC group	Size (mm ²)	Talairach coordinates			CWP
		x	y	z	
Left superior frontal	221.19	-13.7	45.9	3.5	0.038
Left rostral middle frontal	197.91	-25.0	51.9	-5.3	0.047

CWP, cluster-wise P-value; PRL, paramagnetic rim lesion; HC, healthy controls.

Table S2 Regions with cortical thinning in the PRL group relative to the non-PRL group

PRL group vs. non-PRL group	Size (mm ²)	Talairach coordinates			CWP
		x	y	z	
Right parahippocampal	282.55	36.1	-34.7	-14.1	0.020

CWP, cluster-wise P-value; PRL, paramagnetic rim lesion.