

The diagnostic performance of whole-body MRI in the staging of lymphomas in adult patients compared to PET/CT and enhanced reference standard—systematic review and meta-analysis

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Background: Morphology highlighted by diffusion weighted imaging (DWI) is the basis of whole-body MRI (wbMRI). The aim of this study was to analyze current knowledge on the diagnostic performance of wbMRI in the pretreatment staging of patients with lymphoma.

Methods: A search for original articles reporting the diagnostic performance (sensitivity, specificity) of pretreatment (first staging or staging in relapsed patients after complete remission) wbMRI in nodal and extranodal involvement by extracranial lymphoma and the agreement of stage by the Cotswolds-modified Ann Arbor classification in adult patients compared to the reference standard (PET/CT or enhanced reference standard) was conducted in PubMed, EMBASE, Cochrane Library, ClinicalTrials.gov.

Results: Altogether 15 studies with 519 patients were included in the meta-analysis. The pooled sensitivity and specificity for nodal involvement were 0.93 (95% CI: 0.90 to 0.96) and 0.99 (95% CI: 0.98 to 1.00). For nodal staging, most studies used the size criterion of 10 mm in the short diameter (n=10) and the absence of prominent fatty hilum (n=4). Restricted diffusion on diffusion-weighted imaging as a sign of nodal involvement was either not used (n=5), used for detection (n=4), semi-quantitatively (n=4), or quantitatively (n=1). Only one study (7) relied solely on restricted diffusion as the main criterion for nodal involvement. The pooled sensitivity and specificity for extranodal involvement were 0.89 (95% CI: 0.79 to 0.98) and 0.99 (95% CI: 0.99 to 1.00). Seven studies considered diffuse splenic involvement when its long or vertical axis was greater than 13 cm regardless of the patient's physiognomy. The pooled agreement in staging (Cohen's kappa) was almost perfect (0.90, 95% CI: 0.84 to 0.95).

Discussion: The sensitivity and specificity of wbMRI in the assessment of the nodal and extranodal involvement by lymphoma is high. The agreement of wbMRI with the reference standard is almost perfect.

Keywords: Lymphoma; staging; agreement; whole-body MRI (wbMRI); PET/CT; meta-analysis

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Introduction

Malignant lymphoma is the sixth most common malignancy and the most common malignancy of the hematopoietic system. Lymphomas represent heterogeneous group of neoplasms with different clinical behavior from indolent to very aggressive diseases. They are traditionally divided into Hodgkin's lymphoma and non-Hodgkin lymphomas. Overall, lymphomas have 5-year survival rates between 63 and 91 percent (1,2).

Treatment of lymphomas is based on their histological (or genetic) type, stage, prognostic indices, and overall status of the patient (1). The staging considers the location and extent of the disease and the presence of clinical symptoms. The original Ann Arbor staging system was later updated by Cotswolds modification and in 2014, it was modified to reflect the widespread use of PET/CT as the Lugano classification (3). The principal groups (I to IV), remained unchanged between the original and Cotswoldsmodified Ann Arbor system. In avid lymphomas, PET/ CT is the workhorse for imaging of involved nodal areas and extranodal organs (2,4). In lymphomas known to have variable FDG uptake, purely morphological assessment mostly by CT or MRI is used instead (2,5).

Cross-sectional imaging has become the standard for staging, for the assessment of interim response, and after completion of chemotherapy (6). Later, patients require follow-up examinations, and some remain in watchful waiting, undergoing repeated scans. Although PET/CT is the mainstay in staging and response assessment, wholebody MRI (wbMRI) has previously been tested, whether it could be an alternative without the risk of radiation and its stochastic effects-carcinogenesis in later life (7). MRI is a safe imaging method, which is widely available, and its risks are, when observing contraindications, negligible. Therefore, it is vital to summarize current knowledge on the diagnostic performance of wbMRI in patients with lymphoma as a starting point for redefining its role, recommended imaging protocols, and interpretation of the images.

WbMRI acquires structural images that are highlighted by diffusion weighted imaging (DWI). DWI is acquired at different (low and high) b values that indicate the sensitivity to diffusion: higher b values sense smaller diffusion distances in slower moving molecules (in cellular tissues) at the expense of lower signal. Apparent diffusion coefficient (ADC), which is calculated from the decrease of signal intensity with increasing b value, is a quantifiable measure of diffusion. DWI with background body signal suppression (DWIBS) using short inversion time inversion recovery echo-planar imaging shows high signal in a tumoral mass. DWIBS allows better differentiation between reactive and diseased lymph nodes (8). The quantification of DWIBS measurements may be limited by signal decay caused by motion (in the mediastinum) and low agreement of absolute cut-off values of ADC among different studies.

The aim of this systematic review and meta-analysis was to summarize current knowledge on the diagnostic performance of pretreatment (first staging or staging in relapsed patients after complete remission) wbMRI in patients with extracranial lymphoma and the agreement of staging by the Cotswolds modification of the Ann Arbor classification in adult patients compared to the reference standard (PET/CT or enhanced reference standard).

We present the following article in accordance with the PRISMA reporting checklist (available at https://dx.doi. org/10.21037/qims-21-649).

Methods

A PRISMA checklist for Diagnostic Test Accuracy reporting was used.

A search for original articles written in the English language was performed in the following databases and registers: PubMed, EMBASE, Cochrane, clinicaltrials.gov on 12th May 2021 with the following search criteria:

PubMed

("whole body" [All fields]) and ("lymphoma" [All fields]) AND (("diffusion" [all fields]) OR ("DWI" [all fields])) AND (mri [all fields]) AND (PET [all fields]) NOT ("brain" [all fields]); 67 results.

EMBASE

'whole body' AND 'lymphoma' AND ('diffusion' OR 'dwi')



Figure 1 PRISMA 2020 flow diagram for systematic reviews.

AND 'mri' AND 'pet' NOT 'brain'; 141 results.

Cochrane Library

Whole body lymphoma MRI PET; 4 results.

ClinicalTrials.gov

Whole body lymphoma MRI PET, Adult, Older Adult; 14 studies.

Eligible studies met the following criteria: (I) adult patients; (II) pretreatment staging—newly diagnosed or relapsed after complete remission; (III) wbMRI included diffusion-weighted imaging (DWI); (IV) had a defined reference standard (PET/CT or enhanced reference standard); (V) reported sensitivity and/or specificity for nodal and/or extranodal staging and/or agreement with the reference standard; (VI) reported or allowed calculation of SE or 95% CI. We excluded studies that dealt with a primarily organ-specific type of lymphoma (primary central nervous system lymphoma, gut). The diagnosis of lymphoma and its type was based on histopathology. The search flow is depicted in *Figure 1*. The results of the search were independently analyzed by two reviewers (LL, AB), who in case of mismatch discussed the reasons for inclusion or exclusion of an individual study. A total of 15 articles were selected for the final analysis.

The risk of bias was assessed using a QUADAS-2 tool as low, high, or unknown in consensus (*Figure 2*).

Articles included in the analysis were reviewed for inclusion criteria, patient characteristics, imaging protocols, and the reference standard used. Diagnostic performance for nodal and extranodal involvement was extracted where the data was available. Sensitivities and specificities with their 95% CIs and SEs were either retrieved or calculated from the presented data. Agreement between wbMRI and the reference standard in the stage assignment according to the Cotswolds modification of the Ann Arbor classification was calculated using Cohen's kappa statistics based on the study data or retrieved if presented with its 95% CI and SE.

Statistical analysis was performed in R (R Core Team, R foundation, Vienna, Austria). For pooling of the data, we used R package *metafor*, the inverse variance method, the DerSimonian and Laird estimator for tau², double



Figure 2 Risk of bias assessed using the QUADAS-2 tool. +, low; -, high; ?, unknown.

arcsine transformation of the data (Freeman-Tukey), and random effects model with Hartung-Knapp adjustment. Heterogeneity among studies was assessed using Cochran's Q and I² statistics. Forrest and funnel plots were generated using *forrest.meta* and *funnel* functions, respectively. Funnel plot asymmetry was calculated using Egger's test. Possible bias was also assessed by plain visual analysis of the Forrest plots and a leave-one-out analysis. A P-value below 0.05 was considered significant.

Results

All included studies originated from a single institution and apart from two (9,10), all were prospective with 15 to 140 patients (Σ 519) enrolled (*Table 1*).

All wbMRI studies acquired at least two b values. The acquisition was performed in the transverse plane except for one study (22), which acquired head and neck in the

transverse plane and the rest of the body in the coronal plane. Two studies (7,11) used respiratory triggering for DWI. One study (11) involved only DWI imaging without morphological sequence.

The most commonly used morphological sequences were the STIR followed by T2 and T1 performed under free breathing, with breath-hold or respiratory-triggered. In one study (21) only, patients were given contrast material i.v. Occasionally, special acquisitions were performed for the neck and lungs (*Table 2*).

The most common risk of bias was identified in the timing of wbMRI (risk of bias in 1 study; unknown risk in 4 studies) (*Figure 2*).

For nodal staging, most studies used the size criterion of 10 mm in the short diameter (n=10) and the absence of prominent fatty hilum (n=4). Measurement of long axis was used in three studies. Restricted diffusion on diffusionweighted imaging as a sign of nodal involvement was either

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	Veer	Four los est o estad	Other share to us a	Age, mean ± SD [range],	Detiente		Lymphoma types	
Author	rear	Enroiment period	Study type	years	Patients	NHL	Aggressive NHL	HL
Lin (11)	2010	6/2008-2/2009	Prospective	48 [23–79]	15	15	15 (15 DLBCL)	0
Abdulqadhr (12)	2011	3/2008-11/2009	Prospective	47 [18–78]	31	23	18 (13 DLBCL)	8
Gu (13)	2011	11/2008–4/2010	Prospective	50±17 [20-80]	17	15	4 (3 DLBCL)	2
van Ufford (14)	2011	8/2008-10/2009	Prospective	39±8 [33–44]—HL; 61±13 [22–81]—NHL	22	20	9 (7 DLBCL)	2
Stéphane (15)	2013	6/2008-10/2009	Prospective	51 [18–84]	23	18	18 (16 DLBCL)	5
Ferrari (16)	2014	4 months	Prospective	41 [23–81]	27	14	7 (5 DLBCL)	13
Mayerhoefer (7)	2014	8/2011-1/2014	Prospective	58±16 [19–88]	140	118	34 (31 DLBCL)	22
Azzedine (17)	2015	6/2011-12/2012	Prospective	42 [22–75]	23	14	7 (7 DLBCL)	9
Tsuji (9)	2015	-	Retrospective	60±11 [36–78]	28	28	17 (17 DLBCL)	0
Albano (18)	2016	11/2013–12/2014	Prospective	42 [15–86]	68	31	16 (16 DLBCL)	37
Balbo-Mussetto (10)	2016	2/2010-5/2014	Retrospective	49 [20–76]	41	27	10 (9 DLBCL)	14
Gamal (19)	2020	5/2018-1/2020	Prospective	[16–60]	32	10	7	22
Kharuzhyk (20)	2020	2015–2018	Prospective	45±17	92	45	35 (26 DLBCL)	47
Latifoltojar (21)	2020	6/2012-11/2015	Prospective	32 [22–87]	22	8	8 (8 DLBCL)	14
Hong (22)	2021	6/2013-4/2015	Prospective	55±14 [26-82]	30	30	0	0

Table 1 Patient characteristics in each study included in the meta-analysis

SD, standard deviation, NHL, non-Hodgkin lymphoma; HL, Hodgkin lymphoma; DLBCL, diffuse large B-cell lymphoma.

not used (n=5), used for detection (n=4), semi-quantitatively (n=4), or quantitatively (n=1). Only one study (7) relied solely on restricted diffusion as the main criterion for nodal involvement.

Seven studies considered diffuse splenic involvement when its long or vertical axis was greater than 13 cm and two studies (12,14) used signal intensity of the spine on DWI as a comparator for extranodal involvement (*Table 3*).

Sensitivity for nodal involvement was available in 9 studies. The pooled estimate was 0.93 (95% CI: 0.90–0.96) with low heterogeneity $I^2=0.0\%$ (0.0–64.8%); P<0.977 (*Figure 3*). Funnel plot and Egger's test did not indicate asymmetry of the distribution of the results among studies (P=0.14, Figure S1). A leave-one-out sensitivity analysis is shown on Figure S2.

Specificity for nodal involvement was available in 8 studies. The pooled estimate was 0.99 (95% CI: 0.98–1.00) with low heterogeneity I^2 =0.0% (0.0–67.6%); P=1.0 (*Figure 4*). Funnel plot and Egger's test did not indicate asymmetry of the distribution of the results among studies (P=0.62, Figure S3). A leave-one-out sensitivity analysis is shown on Figure S4.

Sensitivity for extranodal involvement was available in 10 studies. The pooled estimate was 0.89 (95% CI: 0.79–0.98) with moderate heterogeneity I²=53.0% (95% CI: 3.7–77.0%); P<0.0001 (*Figure 5*). Funnel plot and Egger's test did not indicate asymmetry of the distribution of results among studies (P=0.86, Figure S5). A leave-one-out sensitivity analysis is shown on Figure S6.

Specificity for extranodal involvement was available in 8 studies. The pooled estimate was 0.99 (95% CI: 0.99–1.00) with low heterogeneity $I^2=0.0\%$ (0.0–67.6%); P=1.00 (*Figure 6*). Funnel plot and Egger's test did not indicate asymmetry of the distribution of results among studies (P=0.67, Figure S7). A leave-one-out sensitivity analysis is shown on Figure S8.

The agreement in the stage according to the Cotswoldsmodified Ann Arbor system pooled from 12 studies was 0.90 (95% CI: 0.84–0.95), with low heterogeneity of I^2 =0.0% (95% CI: 0.0–58.3%), P=0.60 (*Figure 7*). Funnel plot and Egger's test did not indicate asymmetry of the distribution of results among studies (P=0.75, Figure S9). Most studies (n=11) reported agreement in the principal stages, one study (22) included E and S modifiers, where present.

			5			MRI						Ē	TCT		
Author	Year	Field (T)	Manufacturer	DWI	b values (s/mm²)	STIR	12	1	Gd	Time (min)	MBq	CT dose	CECT	Days between PET and MRI	- Reference standard
Lin	2010	1.5	Siemens	TRA RT	50, 400, 800				No	30-45	5 MBq/kg	Low	8	4 (range, 1–12)	PET/CT
Abdulqadhr	2011	1.5	Philips	TRA	0, 1,000	COR RT	(lesions)	COR BH	No	50	5 MBq/kg	Std	No	6 pts: same day2t pts: 7.4±6.6	5ERS - imaging, biopsy, clinical staging, FU 9.3 months (6–14 months)
Gu	2011	ო	Philips	TRA	0, 1,000	TRA	TRA		No	48±4	4.8 MBq/kg	Std	No	2±1 (≤1 week)	PET/CT
van Ufford	2011	1.5	Siemens	TRA	0, 1,000	COR		COR	No	45–55	3 MBq/kg	Low	No	within 15 days	PET/CT
Stéphane	2013	1.5	Philips	TRA	0, 1,000	yes (ns)		yes (ns)	No	40	5 MBq/kg	Low	No	3.5 (range, 1–9)	PET/CT
Ferrari	2014	1.5	Philips	TRA	0, 500	COR (BH)		COR (BH)	No	20-25	370-550 MBq (3.7 MBq/kg)	Low	No	Within 10 days	PET/CT
Azzedine	2015	с у	Philips	TRA	0, 1,000		COR		° Z	44	5 MBq/kg	Std	No	I	Nodal involvement – PET/CTStaging - ERS – imaging, physical examination, bone marrow aspiration and biopsy
		1.5	Siemens	TRA	0, 1,000		COR (TrueFisp)		No	121					
Mayerhoefer	2015	ი	Siemens	TRA (RT)	50, 400, 1,000			TRA	No	20-30	270–340 MBq (by BW)	Std	Yes	≤7 days	ERS - imaging, biopsy, follow-up
Tsuji	2015	с	GE	TRA	0, 1,000		COR		No	35	185 MBq	Low	Yes	I	PET/CT
Albano	2016	1.5	Philips	TRA	0, 800	COR (RT)		COR (BH)	No	2329	3.7 MBq/kg	Low	No	I	PET/CT
Balbo- Mussetto	2016	1.5	Philips	TRA	0, 1,000	COR	COR	COR	No	45	BW-related dose	I	No	I	ERS - biopsy, PET/CT, clinical FU, histology, imaging FU
Gamal	2020	1.5	Philips	TRA	0, 1,000	COR		COR	No	20	5.5 MBq/kg	Std	No	Within 10 days	ERS - imaging, histology, FU 10 months
Kharuzhyk	2020	1.5	GE	TRA	0, 800	COR	TRA RT (chest)	TRA	No	~42	291±49 MBq	Std	No	7±11	ERS - imaging, biopsy, FU 6 months
Latifoltojar	2020	ი	Philips	TRA (0, 100, 300 1,000	ć	COR	COR	20 mL @3mL/s ²	~40	5.5 MBq/kg	Std	No	10 (range, 0–44)	ERS – PET/CT, FU
Hong	2021	ი	Philips	TRA, COR	0, 800	TRA, COR (RT)			°N N	26-28	I	I	I	I	ERS - imaging, clinical staging, FU imaging (116±65 days), histopathology, patients' clinical course
¹ , this report hold; TrueFis standard: FU	ed value sp, stea follow-	is like dy stat up: ~.	ly erroneous; ² , te balanced ser rouch estimate:	Gadote quence : data	rate meglu (Siemens) not availal); CECT, (); Me: BW, b	tarem [®]). DV contrast-en	VI, diffus ihanced	ion-weiç CT; std	ghted ime , standar	aging; STIR, shc d; TRA, transv	ort-tau ii erse pla	iversion ane; CC	r recovery; RT, res)R, coronal plane	piratory trigger; BH, breath- ; ERS, enhanced reference

A single study (21) that reported agreement based on the Lugano criteria, was not included. A leave-one-out sensitivity analysis is shown on Figure S10.

Altogether, the sensitivity analysis did not reveal any significant bias with any of the included studies.

Discussion

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In this meta-analysis, we summarized the diagnostic performance of wbMRI in the pretreatment assessment of nodal and extranodal involvement by lymphoma and its agreement with FDG PET/CT or enhanced reference standard (including FDG PET/CT) in the staging. We showed that the pooled sensitivity for nodal and extranodal involvement is 0.93 and 0.89 while the specificity is nearly 1.0. The agreement in staging (Cohen's kappa) is almost perfect.

Diffusion-weighted imaging with background suppression (DWIBS) is the mainstay of whole-body MR imaging not only in lymphoma but also in other cancers (23,24). WbMRI can be reliably performed both at 1.5T and 3T scanners that provide sufficient field homogeneity. The suppression of background signal is performed by inversion pulse to null the signal of adipose tissue. DWI measures the restriction of random Brownian motion that occurs in tissues with a high cellular component where diffusion is hindered by cellular membranes (25). In the analyzed studies, wbMRI was performed during free breathing in most of them. Respiratory triggering used in two studies (7,11) results in a better depiction of mediastinal and hilar lymph nodes. However, the scan time is usually prolonged by a factor of 2.5. FDG-PET provides different metrics which is a glycolytic activity (25).

For nodal staging, most studies used the size criterion of 10 mm in the short diameter and the absence of prominent fatty hilum. Smaller lymph nodes may be considered if they exhibit other malignancy features including the absence of fatty hilum, local grouping, atypical localization, topographical relationship with involved organs, or show highly restricted diffusion compared to other structures at the same level—usually, the spinal cord was chosen as the comparator (20). Inguinal, iliac, and axillary lymph nodes frequently present with restricted diffusion, so in these regions, attention must be paid to exclude fatty hilum in the measurement of their short axis. It is important to notice that from the studies reporting the sensitivity for nodal involvement <0.9, there were two relying both on the morphological criteria and semiquantitative assessment of

mass lesion or signal abnormalities Area of abnormal SI on T1 and ocal abnormal signal intensity detected by identification of a STIR, focal restricted diffusion STIR: lesions were Splenic involvement [1 and STIR or DWI] Diameter >13 cm, ocal abnormality T2 and 3 DWI SI > SI spinal cord; DWI SI > spinal cord; SI abnormalities or mass lesions Abnormal SI on ADC focal increase in SI¹ ocal increase in SI¹ Extranodal involvement DVI × STIR and T1: abnormal SI, mass detected by identification of a (excluding benign eg. cysts) T2 and STIR: lesions were mass lesion or signal ę area o Table 3 Comparison of criteria for nodal and extranodal involvement among the included studies T1 and STIR: abnormalities abnormal SI Morphology ADC SI < SI muscle DWI SI > SI spinal Detection cord M Nodal involvement × location; central necrosis T2; clustered small lymph nodes; on STIR or SI < surroundings on 2011 LA >10 mm, SI > surroundings Morphology 2010 SA >10 mm 2011 SA >10 mm SA >10 mm unusual 2011 Year Table 3 (continued) Abdulqadhr /an Ufford Author Ľ gu

Table 3 (cont	inued)				
Author	Nodal involvement		Extranodal involvement		-Colonic involvement
	Morphology	DWI	Morphology	DWI	
Stéphane	2013 SA >10 mm SA >15 mm for axillary and femoral except LNN with fatty hilum and thin cortex	Visual analysis (except axillary and femoral LNN), ADC<0.75×10 ⁻³ mm²/s	×	Diffusion signal abnormality	Longest diameter >13 cm (without liver cirrhosis)
Ferrari	2014 SA >10 mm	Detection	T1 or STIR: altered signal	DWI SI > SI surrounding tissues	Altered signal in T1 or STIR, DWI SI > surrounding tissues
Azzedine	2015 LA >10 mm	DWI SI > SI of the muscle on the same image slice	×	Areas of restricted diffusion	Diameter >13 cm; areas of abnormal SI on DWI
Mayerhoefer	r 2015 x	restricted diffusion	×	Restricted diffusion	SI inhomogeneity or well-circumscribed lesions with restricted diffusion
Tsuji	2015 -	I	1	I	I
Albano	2016 LA >15 mm (excl. fatty hilum and thin cortex)	ADC <0.8×10 ⁻³ mm²/s	Focal lesions >1cm, signal abnormalities	Areas of restricted diffusion	Focal lesion or max. diameter >13 (excl. in cirrhosis)
Balbo- Mussetto	2016 SA >10 mm: (neck and mediastinum SA >15: abdomen unusual location, necrotic	DWI SI > SI spinal cord	×	Abnormal SI relative to surrounding tissue; focally increased SI ¹	Focally increased SI
Gamal	2020 SA >10 mm	×	T1 or STIR: altered signal	DWIBS SI > SI surrounding tissues	Altered signal in T1 or STIR, DWI SI > surrounding tissues (kidney), max. diameter > 13 cm
Kharuzhyk	2020 SA >10 mm (excl. fatty hilum, thin parenchyma); SA ≤10 mm: round shape, the absence of hilum, with local grouping, and localization in atypical regions	×	Areas of pathological SI	×	Vertical size >13 cm
Latifoltojar	2020 SA >10 mm	×	Specific for each organ: abnormal moderate-high SI infiltration, abnormal focal SI	Specific for each organ: abnormal moderate-high SI infiltration, abnormal focal SI	Moderate-high SI infiltration in continuum with an adjacent mass; low SI (relative to spleen) discrete foci within spleen
Hong	2021 SA >10 mm, loss of fatty hilum, heterogeneity	×	STIR: focal or diffuse abnormal SI; asymmetrical enlargement of paired organs	Focal increase in DWI SI ¹	Focal or diffuse abnormal SI on STIR, max. diameter >13 cm
¹ , in tissues short axis; L	with normally impeded diffusion. SI, sigi A, long axis; T2, T2 weighted sequence; 5	nal intensity; DWI, diffus STIR, short tau inversion	ion-weighted imaging; ADC, app. recovery; T1, T1 weighted sequer	arent diffusion coefficient; nce.	x, not used; -, not reported; SA,

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Study						Sens	itivity	95%-CI	Weight
Lin 2010				- :			0.80	[0.71; 0.87]	3.0%
Azzedine 2014							0.85	[0.78; 0.90]	4.8%
Latifoltojar 2020		-					0.86	[0.75; 0.93]	4.2%
Balbo-Musseto 2016							0.92	[0.88; 0.95]	9.1%
Kharuzhy 2020							0.93	[0.90; 0.94]	21.6%
Mayerhoefer 2015					ł		0.94	[0.91; 0.96]	32.0%
Stéphane 2013					e		0.96	[0.90; 0.98]	5.1%
Gu 2011					a -		0.96	[0.91; 0.98]	3.8%
Albano 2016					-		0.98	[0.96; 0.99]	16.4%
Random effects model Prediction interval				\diamond	>		0.93	[0.90; 0.96] [0.90; 0.96]	100.0%
0	.6	0.7	0.8	0.9	1	1.1			

Figure 3 Forrest plot of the sensitivity of wbMRI in the detection of nodal involvement by lymphoma. 95% CI, 95% confidence interval.

Study				Spe	cificity	95%-CI	Weight
Stéphane 2013		<u> </u>			0.97	[0.94; 0.98]	5.0%
Albano 2016		+-			0.98	[0.96; 0.98]	15.4%
Kharuzhy 2020					0.99	[0.98; 1.00]	21.4%
Balbo-Musseto 2016		-			0.99	[0.98; 1.00]	9.7%
Lin 2010					1.00	[0.97; 1.00]	3.5%
Mayerhoefer 2015		-+			1.00	[1.00; 1.00]	34.2%
Azzedine 2014					1.00	[0.99; 1.00]	5.6%
Latifoltojar 2020					1.00	[0.99; 1.00]	5.3%
Random effects model		\diamond			0.99	[0.98; 1.00]	100.0%
Prediction interval		_				[0.98; 1.00]	
I		1	I	1			
0.9	0.95	1	1.05	1.1			

Figure 4 Forrest plot of the specificity of wbMRI in the detection of nodal involvement by lymphoma. 95% CI, 95% confidence interval.

Study		Sens	itivity		Sensitivity	95%-Cl	Weight
Azzedine 2014 Kharuzhy 2020 Abdulqadrh 2011 Albano 2016 Stéphane 2013 Mayerhoefer 2015	_	-	 + 	-	0.62 0.70 0.75 0.92 0.96 0.97	[0.46; 0.76] [0.61; 0.79] [0.30; 0.95] [0.85; 0.96] [0.78; 0.99] [0.92; 0.99]	7.4% 14.9% 7.6% 13.9% 7.8% 17.2%
Balbo-Musseto 2016 Latifoltojar 2020 Gu 2011 Lin 2010					0.97 1.00 1.00 1.00	[0.86; 1.00] [0.70; 1.00] [0.87; 1.00] [0.84; 1.00]	11.2% 7.1% 6.8% 6.1%
Random effects model Prediction interval	0.4	0.6	0.8	> 	0.89	[0.79; 0.98] [0.64; 1.00]	100.0%

Figure 5 Forrest plot of the sensitivity of wbMRI in the detection of extranodal involvement by lymphoma. 95% CI, 95% confidence interval.

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Study			Specifici	y 95%–Cl	Weight
Kharuzhy 2020	-		0.9	7 [0.95; 0.99]	19.8%
Stéphane 2013		-	1.0	0 [0.98; 1.00]	5.5%
Mayerhoefer 2015		+	1.0	0 [1.00; 1.00]	34.4%
Albano 2016		-i	1.0	0 [0.99; 1.00]	16.0%
Abdulgadrh 2011	-		1.0	0 [0.88; 1.00]	5.8%
Latifoltojar 2020		— H	1.0	0 [0.98; 1.00]	5.2%
Balbo-Musseto 2016		-	1.0	0 [0.99; 1.00]	9.9%
Lin 2010	-		1.0	0 [0.95; 1.00]	3.3%
Random effects model		\diamond	0.9	9 [0.99; 1.00]	100.0%
Prediction interval		-		[0.98; 1.00]	
0.8	0.9	1	1.1		



Study	Agreement	95%-CI	Weight
van Ufford 2011	0.69	[0.46; 0.92]	3.4%
Kharuzhyk 2020 —	0.78	[0.69; 0.89]	17.2%
Lin 2010 *	- 0.82	[0.52; 1.00]	2.1%
Gu 2011	- 0.83	[0.60; 1.00]	2.7%
Abdulqadrh 2011	- 0.87	[0.72; 1.00]	5.4%
Tsuji 2015	- 0.90	[0.77; 1.00]	5.0%
Mayerhoefer 2015	0.92	[0.86; 0.97]	29.7%
Azzedine 2014	- 0.94	[0.82; 1.00]	4.3%
Ferrari 2014	- 0.95	[0.85; 1.00]	5.2%
Hong 2021	- 0.96	[0.88; 1.00]	6.0%
Balbo–Musseto 2016	1.00	[1.00; 1.00]	12.2%
Stéphane 2013	1.00	[1.00; 1.00]	6.9%
Random effects model	0.90	[0.84; 0.95]	100.0%
Prediction interval]	[0.84; 0.95]	
0.4 0.5 0.6 0.7 0.8 0.9	1 1.1		

Figure 7 Forrest plot of the agreement of wbMRI and the reference standard in the stage. 95% CI, 95% confidence interval.

DWI or ADC (11,17).

Extranodal involvement was based on focal changes on T1, T2, or STIR of non-benign nature. Focal DWI increase compared to the surrounding tissue is required in organs that normally exhibit restricted diffusion. To assess diffuse infiltration, signal intensity on DWI can also be visually compared to other organs at the same level such the spinal cord or other surrounding tissues. The signal intensity on DWIBS of a single organ is different between adjacent stations because of corrections of field homogeneity and shimming. The diagnostic performance of wbMRI is limited in the detection of small pulmonary infiltrates and diffuse splenic involvement. Seven studies considered diffuse splenic involvement when its long or vertical axis was greater than 13 cm regardless of the patient's physiognomy. The normal size of the spleen is significantly influenced by body weight and sex and its upper 95% confidence limits exceed 13 cm in men taller than 170 cm (26). Twelve studies included SI abnormities on morphological and/or DWI sequences.

In all but one study, DWI with background suppression was performed without respiratory compensation which prolongs the examination. Because of respiratory and cardiac motion, DWI is less efficient in the evaluation of hilar, mediastinal, or pulmonary involvement. Most studies performed DWI imaging in the axial plane, only one in the coronal plane. Imaging in the transverse plane is obviously more suitable for the construction of fusion images with transverse anatomical acquisitions such as STIR, T2, or T1 that resemble that of PET/CT. According to our experience, fast STIR and T2 sequences can be performed even without respiratory compensation while T1 requires breath-hold at the thoracic and abdominal stations.

So why has not wbMRI become the preferred method

for pretherapeutic lymphoma staging? Kharuzhyk et al. have shown that wbMRI and PET/CT in the nodal and extranodal involvement have comparable diagnostic accuracy (20). We believe that the main considerations are the higher complexity and time demand for wbMRI. The mean time needed to perform wbMRI was 35±15 min. This requires that one hour is reserved for an examination which is from the reimbursement point of view equal to an examination that requires half an hour. Another advantage of PET/CT is the benefit of functional information in the standardized assessment of the treatment response, which has been firmly and clearly established in the form of the Deauville criteria (27). We believe that there is still unexplored potential of wbMRI in the quantification of the treatment response using T1 and T2 mapping, susceptibility weighted imaging, and even fat fraction (13).

Study limitations. A major limitation of this meta-analysis is the disproportion in lymphoma types considered (*Figure 2*). Secondly, there was heterogeneity in MRI imaging protocols and MRI scanners (field strength, manufacturer). Thirdly, stage agreement was based on the Cotswoldsmodified Ann Arbor classification because only one study reported using the more recent Lugano criteria. Lastly, some studies used only PET/CT as the reference standard while the majority used enhanced reference standard, which included histology, and follow-up examinations.

In conclusion, the sensitivity of wbMRI in the assessment of the nodal and extranodal involvement by lymphoma is above 0.93 and 0.89 while the specificity is nearly 1.0. Agreement in the staging is almost perfect with Cohen's kappa of 0.9. Further studies are needed to develop more accurate criteria for the involvement of lymph nodes especially in difficult areas such as in the mediastinum and pulmonary hili. Also, the criteria for diffuse splenic involvement require the attention of further studies.

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Footnote

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Ethical Statement: The authors are accountable for all aspects of the work in ensuring that questions related to the accuracy or integrity of any part of the work are appropriately investigated and resolved.

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Figure S1 Funnel plot of the distribution of the sensitivity of wbMRI in the detection of nodal involvement by lymphoma.



Figure S2 Sensitivity of wbMRI in the detection of nodal involvement by lymphoma shown on a leave-one-out sensitivity analysis.



Figure S3 Funnel plot of the distribution of the specificity of wbMRI in the detection of nodal involvement by lymphoma.

Study	E	Estimate [95% CI]
Kharuzhy 2020	H	1.00 [1.00, 1.00]
Albano 2016	·	0.99 [0.98, 1.00]
Azzedine 2014	·	0.99 [0.98, 1.00]
Latifoltojar 2020	•	0.99 [0.98, 1.00]
Balbo-Musseto 2016	·	0.99 [0.98, 1.00]
Lin 2010	⊢	0.99 [0.98, 1.00]
Mayerhoefer 2015	•i	0.99 [0.98, 1.00]
Stéphane 2013	•••••	0.99 [0.98, 1.00]
	0.98 0.99 1 1.01	
	Specificity	

Figure S4 Specificity of wbMRI in the detection of nodal involvement by lymphoma shown on a leave-one-out sensitivity analysis.



Figure S5 Funnel plot of the distribution of the sensitivity of wbMRI in the detection of extranodal involvement by lymphoma.



Figure S6 Sensitivity of wbMRI in the detection of extranodal involvement by lymphoma shown on a leave-one-out sensitivity analysis.



Figure S7 Funnel plot of the distribution of the specificity of wbMRI in the detection of extranodal involvement by lymphoma.

Study	I	Estimate [95% CI]
Kharuzhy 2020	H a ri	1.00 [1.00, 1.00]
Stéphane 2013	·1	0.99 [0.98, 1.00]
Mayerhoefer 2015	·	0.99 [0.98, 1.00]
Albano 2016	•	0.99 [0.98, 1.00]
Abdulqadrh 2011		0.99 [0.98, 1.00]
Latifoltojar 2020		0.99 [0.98, 1.00]
Balbo-Musseto 2016	• 	0.99 [0.98, 1.00]
Lin 2010	 i	0.99 [0.98, 1.00]
	0.98 0.99 1 1.01	
	Specificity	

Figure S8 Specificity of wbMRI in the detection of extranodal involvement by lymphoma shown on a leave-one-out sensitivity analysis.





Figure S9 Funnel plot of the distribution of the agreement of wbMRI and the reference standard in the stage.



Figure S10 Agreement of wbMRI and the reference standard in the stage shown on a leave-one-out sensitivity analysis.