



# Value of a combined magnetic resonance imaging-based radiomics-clinical model for predicting extracapsular extension in prostate cancer: a preliminary study

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**Background:** Extracapsular extension (ECE) of prostate cancer (PCa) is closely related to the treatment and prognosis of patients, and radiomics has been widely used in the study of PCa. This study aimed to evaluate the value of a combined model considering magnetic resonance imaging (MRI)-based radiomics and clinical parameters for predicting ECE in PCa.

**Methods:** A total of 392 PCa patients enrolled in this retrospective study were randomly divided into the training and validation sets at a ratio of 7:3. Radiologists assessed all lesions by Mehralivand grade. Radiomics features were extracted and selected to build a radiomics model, while clinical parameters were noted to construct the clinical model. The combined model was constructed by the integration of the radiomics model and clinical model. Meanwhile, the nomogram for predicting ECE was constructed based on the combined model. Then, the area under the receiver operating characteristic (ROC) curve (AUC), Delong test and the decision curve analysis (DCA) were used to compare the performance among the combined model, radiomics model, clinical model and Mehralivand grade.

**Results:** The AUC of the combined model in the validation set was comparable to that of the radiomics model [AUC =0.894 (95% confidence interval (CI): 0.837–0.950) *vs.* 0.835 (95% CI: 0.763–0.908), *P*>0.05]. In addition, the sensitivity of the combined model and radiomics model was 90.7% and 77.8%, with an accuracy of 81.4% and 76.3%, respectively. On the other hand, the AUCs of the Mehralivand grade of radiologists and clinical model were 0.774 (95% CI: 0.691–0.857) and 0.749 (95% CI: 0.658–0.840), respectively, in the validation set, which were lower than those in the combined model (*P*<0.05). The DCA implied that the combined model could obtain the maximum net clinical benefits compared with the clinical model, the Mehralivand grade and radiomics model.

**Conclusions:** The combined model has a satisfactory predictive value for ECE in PCa patients compared with the clinical model, Mehralivand grade of radiologists, and the radiomics model.

**Keywords:** Prostate cancer (PCa); extracapsular extension (ECE); Mehralivand grade; radiomics; nomogram

Submitted Dec 03, 2022. Accepted for publication Jun 07, 2023. Published online Jun 26, 2023.

doi: 10.21037/tcr-22-2750

**View this article at:** <https://dx.doi.org/10.21037/tcr-22-2750>

## Introduction

Prostate cancer (PCa) is a common genitourinary malignancy in men and the leading cause of cancer incidence and mortality (1). Radical prostatectomy (RP) is the preferred treatment for patients with localized PCa (2). While achieving the goal of tumor resection, the preservation of erectile function and urinary continence is also paramount. However, the choice of preserving the neurovascular bundle around the prostate depends on the presence of extracapsular extension (ECE) of PCa (3). ECE is closely associated with adverse pathologies such as positive surgical margins, biochemical recurrence and progression, and an increased risk of PCa-related mortality (4). Therefore, accurate preoperative prediction of ECE is a key step to optimize treatment for patients with PCa, and has an important impact on clinical decision making and prognosis of PCa patients.

From an image perspective, magnetic resonance imaging (MRI) can aid in diagnosing ECE by clearly displaying the anatomical morphology of the prostate and lesions with high soft tissue resolution (5). Due to the different signs of ECE on MRI images and the lack of standardized description of ECE, the diagnostic accuracy and sensitivity of different experienced radiologists vary greatly (6). Some scholars proposed to use structured reports to describe ECE, which mainly include Likert score, the European Society of Urogenital Radiology (ESUR) score, and the Mehralivand grade. Among them, Mehralivand grade had

the highest correlation with pathological ECE and the best diagnostic performance with its simplicity and little imaging features (7). Even so, Mehralivand grade is only dependent on the subjective assessment of radiologists by the relatively limited imaging features, and the diagnostic performance of ECE remains limited in practice (8).

Radiomics has been increasingly used in medical imaging as an emerging research technology in recent years. It enables the extraction of many diagnostic features (kurtosis, skewness, wavelet, etc.) from specific areas of the medical image through data characterization algorithms to make an objective and quantitative analysis of the images. Medical images can be transformed into minable data in the form of features by radiomics, which can provide valuable information for clinical decision-making (9,10). Relevant research results have shown that radiomics has broad application prospects in the detection, grading, and invasiveness prediction of PCa (11,12). Qi *et al.* (13) established a radiomics model in patients with prostate-specific antigen (PSA) level of 4–10 ng/mL, which could provide potential preoperative prediction for PCa patients and help to reduce unnecessary biopsies. A study conducted comparative analysis based on radiomics model and the Prostate Imaging Report and Data System (PI-RADS) score in PCa diagnosis and pathological grading, which verified the excellent diagnostic efficacy of radiomics model in distinguishing cancerous and non-cancerous prostate lesions and high or low grade PCa lesions (14). Previous findings also showed that radiomics features hold promise for the prediction of the therapy response in the radioligand therapy of PCa patients by positron emission tomography/computed tomography (PET/CT) (15,16). In summary, the potential application value of radiomics in ECE is promising. However, there are few studies on the applications of radiomics in the preoperative prediction of ECE in PCa patients.

This study aimed to evaluate the predictive value of a combined model of MRI-based radiomics and clinical variables for predicting ECE in PCa, and further compare it with the radiologists' assessments using Mehralivand grade. We present this article in accordance with the TRIPOD reporting checklist (available at <https://tcr.amegroups.com/article/view/10.21037/tcr-22-2750/rc>).

## Methods

### Patients

This study was conducted in accordance with the

### Highlight box

#### Key findings

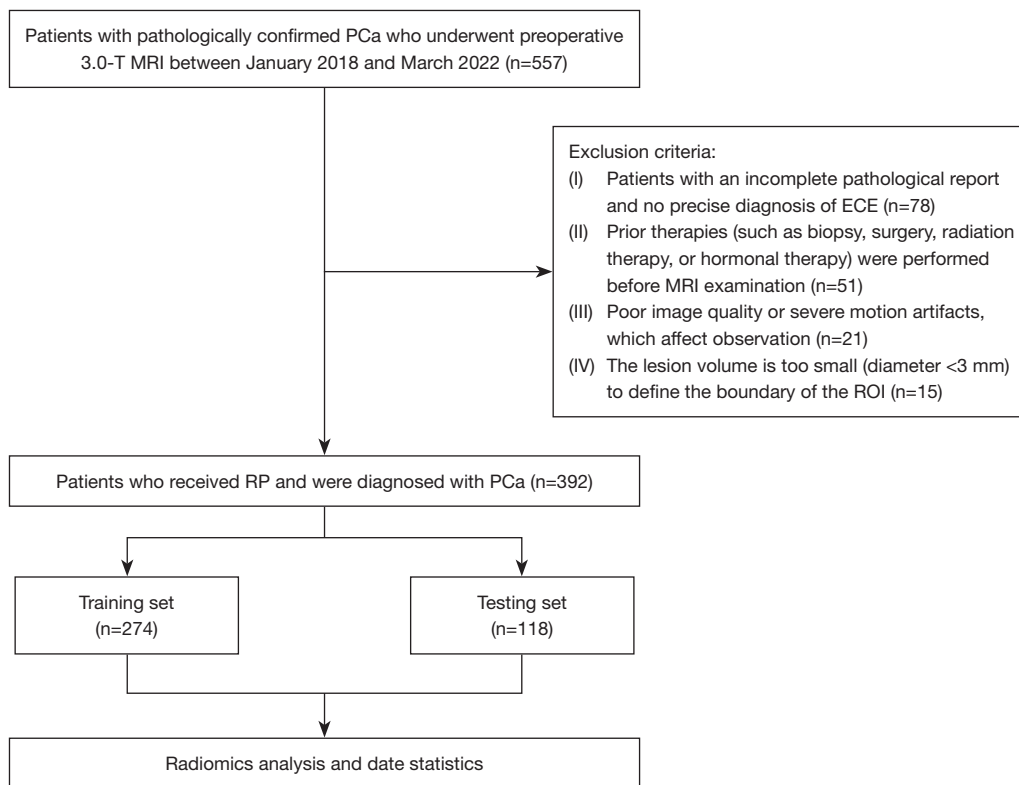
- We found that a combined model considering MRI-based radiomics and clinical variables had a satisfactory predictive value for ECE in PCa patients.

#### What is known and what is new?

- MRI and clinical variables are commonly used for clinical evaluation in the ECE of PCa, but there is a problem of misdiagnosis or missed diagnosis. There is a need for a more effective diagnostic method to predict ECE.
- In this study, we constructed a predictive model combining radiomics and clinical parameters and found its diagnostic efficacy to be superior to the clinical model, Mehralivand grade, and radiomics model.

#### What is the implication, and what should change now?

- The combined model we have constructed may help in the diagnosis of ECE in PCa patients, but still needs to be validated with large data.



**Figure 1** Flowchart of patient recruitment in this study. PCa, prostate cancer; ECE, extracapsular extension; MRI, magnetic resonance imaging; RP, radical prostatectomy; ROI, region of interest.

Declaration of Helsinki (as revised in 2013). This study was approved by the Ethics Committee of The First Affiliated Hospital of Soochow University (No. 262; 2021) and individual consent for this retrospective analysis was waived.

A total of 557 patients with pathologically confirmed PCa underwent preoperative 3.0-T MRI followed by RP between January 2018 to March 2022 at The First Affiliated Hospital of Soochow University, out of which 392 patients were retrospectively enrolled in this study. The inclusion criteria were as follows: (I) all patients received RP and had confirmed PCa; (II) patients with detailed and complete clinical data, imaging information, and pathological reports; and (III) prostate MRI was performed within one month before RP. The exclusion criteria were as follows: (I) patients with an incomplete pathological report and no precise diagnosis of ECE (n=78); (II) the patients who received prior therapies (such as biopsy, surgery, radiation therapy, or hormonal therapy) before MRI (n=51); (III) poor image quality or severe motion artifacts, which affect observation (n=21); and (IV) the lesion volume is too small (diameter <3 mm) to define the boundary of the region of

interest (ROI) (n=15). *Figure 1* shows a flowchart depicting the patient recruitment in this study.

The clinical variables, including age, PSA at admission, lesion location distribution, and biopsy Gleason group (GG) for each patient, were obtained from the medical records. Further, the PI-RADS v2.1 scores were assessed by radiologists (with more than 10 years of prostate MRI experience). The lesion location distribution included the peripheral zone (PZ), transitional zone (TZ), or PZ + TZ. The biopsy pathology GG was divided into five grades according to the 2014 International Society of Urological Pathology (ISUP) guidelines (17).

#### *Standard of reference*

The final histopathologic assessment after the RP procedure was defined as the standard reference. One dedicated pathologist (with more than 10 years of experience) blinded to the MRI reports reviewed all the specimens according to a standard protocol and filled out a structured pathological report per the clinical routine. The pathologist

**Table 1** Sequences and parameters of the MRI scans

Sequence	Repetition (ms)	Echo time (ms)	Layer thickness (mm)	Interlayer spacing (mm)	Field of view (mm × mm)
Axial T <sub>1</sub> WI	680.00	13.00	5	0.50	380×380
Axial T <sub>2</sub> WI	6,980.00	104.00	3	0	200×200
Sagittal T <sub>2</sub> WI	3,900.00	89.00	3	0.45	200×200
Coronal T <sub>2</sub> WI	3,500.00	85.00	3	0.60	220×220
DWI	5,000.00	72.00	3	0	288×288

MRI, magnetic resonance imaging; T<sub>1</sub>WI, T<sub>1</sub>-weighted imaging; T<sub>2</sub>WI, T<sub>2</sub>-weighted imaging; DWI, diffusion-weighted imaging.

then recorded the ECE status for each lesion. Another senior urologist (with more than 10 years of experience) coordinated the workflow to ensure the tumor depicted by the pathologist matched the lesion analyzed by the radiologist. Only lesions that were visible on MRI images were finally enrolled in subsequent analysis. According to the measure of ISUP (17), ECE is defined as the presence of tumors beyond the borders of the prostate.

### Scanning equipment and parameters

A 3.0-T superconducting MR scanner (Skyra; Siemens, Munich, Germany) with an abdominal 32-channel surface phased line coil was used to perform prostate MRI. Patients were taken in a supine position with the head advanced. The scanning sequence included axial T<sub>1</sub>-weighted imaging (T<sub>1</sub>WI), axial T<sub>2</sub>-weighted imaging (T<sub>2</sub>WI) (no fast-saturated), sagittal T<sub>2</sub>WI, coronal T<sub>2</sub>WI, and diffusion-weighted imaging (DWI) (b=100, 1,000, 1,500 s/mm<sup>2</sup>). Based on the DWI images of b=1,500 s/mm<sup>2</sup>, the apparent diffusion coefficient (ADC) icons were calculated by an extended single exponential fitting model. The specific scanning parameters were recommended by PI-RADS v2.1 (18). The detailed scan parameters are shown in *Table 1*.

### Mehralivand grade

Two radiologists (reader 1 and 2), with 6–8 years of prostate MRI experience, assessed ECE by Mehralivand grade based on T<sub>2</sub>WI, ADC, and DWI images without obtaining pathological results. The assessment of radiologist is mainly based on T<sub>2</sub>WI images, assisted by DWI and ADC images to determine the boundary between the lesion and the prostate capsule. If a patient has multiple lesions, each lesion of the patient is evaluated separately, and the highest grade among the multiple lesions is selected as the final

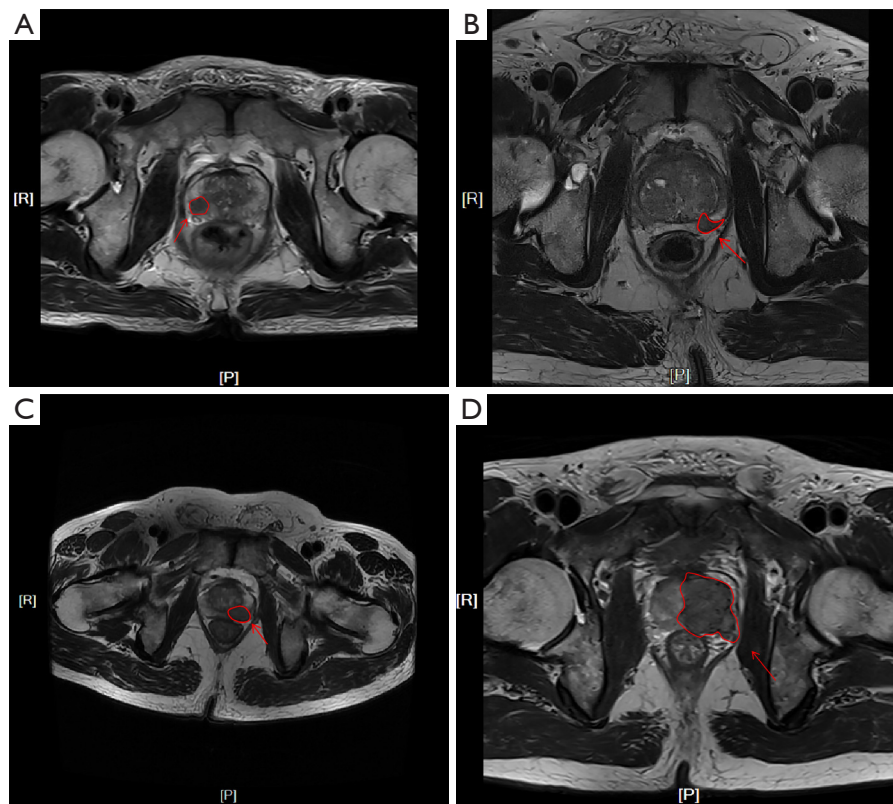
assessment of the patient.

A staging assessment of ECE was performed using a criteria-based grading system for the Mehralivand grade introduced by Mehralivand *et al.* (19). Imaging diagnosis of ECE was based on a four-level grading approach using capsular contact length (CCL) of 15 mm or greater, capsular irregularity or bulge, and frank breach of the capsule: (I) grade 0, no capsular contact or CCL less than 15 mm; (II) grade 1, either CCL of 15 mm or greater, or capsular irregularity or bulge; (III) grade 2, both CCL of 15 mm or greater, and capsular irregularity or bulge; and (IV) grade 3, frank breach of the capsule at MRI with tumor extension into the periprostatic space or invasion of adjacent anatomic structures. Each scoring example is shown in *Figure 2*.

### Radiomics analysis

#### Tumor segmentation

The axial T<sub>2</sub>WI, high b-value (1,500 s/mm<sup>2</sup>) DWI, and ADC images were the target for radiomics analysis. Firstly, different target images of the same patient were matched spatially by Elastix software package (v. 4.10, <http://elastix.isi.uu.nl/index.php>). Based on T<sub>2</sub>WI images, DWI and ADC images were registered successively, which could ensure that three sequences had the same resolution, field of vision and orientation. Secondly, the processed T<sub>2</sub>WI, DWI and ADC images (nii format) were imported into ITK-SNAP software (v. 4.7.2; <https://itk.org/>) for lesion segmentation. A radiologist with 6 years of prostate MRI experience (reader 3) manually outlined the ROI on the T<sub>2</sub>WI, ADC, and DWI images without obtaining pathological results. Then, the total volume of interest (VOI) of the tumor was obtained. Finally, the results of the segmentation were reviewed by a senior radiologist who had 12 years of prostate MRI experience (reader 4). For some controversial lesions, readers 3 and 4 determined after



**Figure 2** Each scoring example of Mehralivand grade on axial T<sub>2</sub>WI (A-D, the red circle is the outline of the lesion, and the red arrow indicates the contact relationship between the lesion and capsule). (A) grade 0, the lesion is located on the right of PZ, and there is still normal tissue between the lesion and capsule; (B) grade 1, the lesion is located on the left of PZ, and a CCL of 15 mm without capsular irregularity or bulge; (C) grade 2, the lesion is located on the left of PZ and a CCL >15 mm with capsular bulge; (D) grade 3, the lesion is located on the left of PZ + TZ and well-defined breach of the prostate capsule with tumor extension into periprostatic space. R, right; P posterior; T<sub>2</sub>WI, T<sub>2</sub>-weighted imaging; PZ, peripheral zone; TZ, transition zone; CCL, curvilinear contact length.

consultation.

To ensure the stability and repeatability of ROI, reader 4 randomly selected 50 lesions in the enrolled cases to draw ROI, and reader 3 randomly selected 50 lesions to repeat the ROI one month later. The inter-observer and intra-observer correlation coefficients were calculated.

### Feature extraction

Before feature extraction, the images of each patient were standardized to improve the texture recognition rate. The T<sub>2</sub>WI, DWI, and ADC images of each patient were firstly resampled to 1×1×1 cm<sup>3</sup> voxel sizes to normalize the voxel spacing. Then, the voxel intensity discretization was accomplished by fixing the bin width at 25 Hounsfield unit (HU) to reduce imaging noise and standardize the intensity. At last, Z-score normalization was carried out for

different sequences of each patient to reduce the impact of inconsistent image parameters on the changes of radiomics features, and the voxel intensity was converted into a distribution with a mean of 0 and a standard deviation of 1 (20). After image preprocessing completed, Feature Explorer (FAE, v.0.4.0), an open-source radiomics software based on pyradiomics software package (21), was used to extract features from VOI of each sequence. Based on T<sub>2</sub>WI, DWI, and ADC sequences, 851 radiomics features were extracted from the VOI of each sequence of each lesion separately. There were a total of 2,553 radiomics features, including 42 morphology features, 54 first-order statistics features, 15 neighboring gray level dependence matrix (NGLDM) features, 42 gray level dependence matrix (GLDM) features, 48 gray level size zone matrix (GLSZM) features, 48 gray level run length matrix (GLRLM) features,

72 gray level co-occurrence matrix (GLCM) features, and 2,232 wavelet transform features.

### Feature selection and radiomics model construction

All samples were randomly divided into a training set and validation set at a ratio of 7:3. To remove the unbalance of sample, up-sampling was performed by repeating random cases to make positive/negative samples balance. The Z-score method was applied to normalize the extracted features again by subtracting the mean value and dividing it by the standard deviation. The dimension reduction was then applied to the normalized features. The Pearson correlation coefficient (PCC) was estimated on each pair of two features, and the ones with a value larger than 0.9 were dropped. Analysis of recursive feature elimination (RFE) was used to select features, and the *F*-value of each feature was calculated based on the label. Only the top 20 features were reserved. Finally, the different classifiers, including least absolute shrinkage and selection operator (LASSO), decision tree (DT), logistics regression (LR), random forest (RF) and support vector machine (SVM), were trained on the selected features to build the radiomics model. The optimal model parameters were chosen by 10-fold cross-validation and finally the predictive value of the radiomics model was obtained through the linear combination of the coefficients weighted by the selected radiomics features, so as to quantify the diagnostic efficiency. All the experiments above were run in FAE (21).

### Construction of the clinical model and combined radiomics-clinical model

The clinical variables (including age, PSA at admission, lesion location, biopsy GG, and PI-RADS v2.1 score for each patient) were first evaluated by the univariate analysis. Then, the multivariate binary LR analysis was used to screen out independent risk factors from the significant clinical variables in the univariate analysis. The clinical model was built by the independent risk factors.

Moreover, a combined radiomics-clinical model was constructed by integrating the independent risk factors in clinical model and the predictive value of ECE in radiomics model. Meanwhile, the nomogram for the prediction of ECE was constructed based on the combined model.

### Statistical analysis

SPSS 25.0 and MedCalc 18.0 software were used for statistical analysis. The counting data were compared by

the chi-square test. The Shapiro-Wilk test was performed to test whether the measurement data was a normal distribution. Then, an independent sample *t*-test or Mann-Whitney *U* test was conducted. Parameters including the receiver operating characteristic (ROC) curve, the area under the curve (AUC), 95% confidence interval (CI), sensitivity, specificity, positive predictive value (PPV), negative predictive value (NPV), and accuracy were all used to evaluate the performance in above models. DeLong test was used to compare the AUCs among these models, and the Hosmer-Lemeshow test was used to verify the agreement between the combined model and the pathological results. Finally, decision curve analysis (DCA) was used to quantify the net clinical benefits of each predictive method. A  $P < 0.05$  was considered statistically significant.

## Results

### Baseline characteristics

A total of 392 PCa patients who received RP were enrolled in this study, with 180 (45.9%) lesions having pathologically confirmed ECE. General data of patients in the training set and validation set are summarized in *Table 2*. There was no statistical significance in the age, PSA, lesion location distribution, PI-RADS v2.1 score, Mehralivand grade, biopsy GG, and the final pathological result of ECE between the two groups ( $P > 0.05$ ).

### Performance of clinical model and Mehralivand grade

After univariate and multivariate binary LR analyses, PSA, lesion location, biopsy GG, and PI-RADS v2.1 score were all independent risk factors of ECE ( $P < 0.05$ ) (*Table 3*) and were used to build a clinical model. The AUC, sensitivity, specificity, and accuracy of the clinical model in the validation set were 0.749 (95% CI: 0.658–0.840), 87.0%, 56.3%, and 70.3%, respectively, which were shown in *Figure 3* and *Table 4*.

The inter-observer consistency for assessment of Mehralivand grade in terms of Kappa value was 0.887, indicating a strong consistency between readers 1 and 2. The Mehralivand grade of reader 1 was selected as the final for the following analysis. The AUC, sensitivity, specificity, and accuracy of radiologists' Mehralivand grade in the validation set were 0.774 (95% CI: 0.691–0.857), 70.4%, 76.6%, and 73.7%, respectively. The performance of the

**Table 2** General data of patients in the training set and validation set

Variables	Total	Training set	Validation set	P value
N (%)	392	274 (69.9)	118 (30.1)	–
Age (years), median [IQR]	70 [66, 75]	71 [66, 75]	72 [67, 75]	0.290*
PSA (ng/mL), median [IQR]	16.55 [9.26, 33.05]	15.89 [9.25, 29.91]	17.40 [9.45, 36.69]	0.378*
Lesion location distribution, n (%)				0.747 <sup>#</sup>
PZ	227 (57.9)	160 (58.4)	67 (56.8)	
TZ	113 (28.8)	80 (29.2)	33 (28.0)	
PZ + TZ	52 (13.3)	34 (12.4)	18 (15.3)	
PI-RADS v2.1 score, n (%)				0.295 <sup>#</sup>
2	38 (9.7)	24 (8.8)	14 (11.9)	
3	45 (11.5)	27 (9.9)	18 (15.3)	
4	85 (21.7)	62 (22.6)	23 (19.5)	
5	224 (57.1)	161 (58.8)	63 (53.4)	
Mehralivand grade of reader 1, n (%)				0.808 <sup>#</sup>
0	102 (26.0)	70 (25.5)	32 (27.1)	
1	105 (26.8)	72 (26.3)	33 (28.0)	
2	130 (33.2)	95 (34.7)	35 (29.7)	
3	55 (14.0)	37 (13.5)	18 (15.3)	
Mehralivand grade of reader 2, n (%)				0.454 <sup>#</sup>
0	111 (28.3)	71 (25.9)	40 (33.9)	
1	89 (22.7)	64 (23.4)	25 (21.2)	
2	118 (30.1)	85 (31.0)	33 (28.0)	
3	74 (18.9)	54 (19.7)	20 (16.9)	
Biopsy GG, n (%)				0.917 <sup>#</sup>
GG ≤3	249 (63.5)	175 (63.9)	74 (62.7)	
GG ≥4	143 (36.5)	99 (36.1)	44 (37.3)	
Final pathologic result of ECE, n (%)				1.000 <sup>#</sup>
ECE positive	180 (45.9)	126 (46.0)	54 (45.8)	
ECE negative	212 (54.1)	148 (54.0)	64 (54.2)	

\*, Mann-Whitney U test; <sup>#</sup>, chi-squared test. IQR, interquartile range; PSA, prostate specific antigen; PZ, peripheral zone; TZ, transition zone; PI-RADS, prostate imaging reporting and data system; GG, Gleason group; ECE, extracapsular extension.

Mehralivand grade in predicting ECE was shown in *Figure 3* and *Table 4*.

#### **Performance of radiomics model and combined model**

The reliability of the radiomics features was quantified by inter-observer (as determined by readers 3 and 4), and

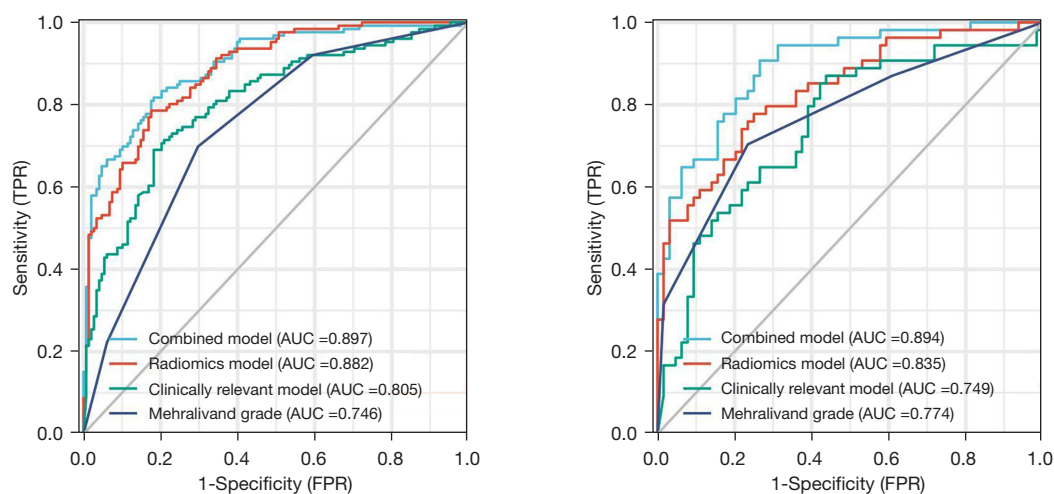
intra-observer statistics (as determined by reader 3 twice) tested based on all radiomics features. The mean inter-observer reliability was 0.805 (95% CI: 0.702–0.869), and the mean intra-observer reliability was 0.859 (95% CI: 0.784–0.913), indicating that the repeatability of feature extraction was fine.

After the features normalization of Z-score and the

**Table 3** Univariate and multivariate binary logistics regression analyses results of clinical variables

Variables	ECE positive (n=180)	ECE negative (n=212)	Univariate analysis		Multivariate binary logistics regression	
			$t/Z/\chi^2$	P value	Odds ratio (95% CI)	P value
PSA (ng/mL), median [IQR]	25.84 [13.4, 50.1]	12.16 [7.81, 20.6]	-4.567	<0.001*	1.017 (1.003–1.031)	0.015
Age (years), median [IQR]	72 [66, 76]	71 [66, 75]	-1.404	0.128*	–	–
PI-RADS v2.1 score, n (%)			82.108	<0.001 <sup>#</sup>	1.521 (1.069–2.165)	0.020
2	3 (1.7)	35 (16.5)				
3	8 (4.4)	37 (17.5)				
4	23 (12.8)	62 (29.2)				
5	146 (81.1)	78 (36.8)				
Biopsy GG, n (%)			49.270	<0.001 <sup>#</sup>	2.038 (1.135–3.661)	0.017
GG ≤3	81 (45.0)	168 (79.2)				
GG ≥4	99 (55.0)	44 (20.8)				
Lesion location distribution, n (%)			41.670	<0.001 <sup>#</sup>	1.287 (1.066–1.553)	0.024
PZ	96 (53.3)	131 (61.8)				
TZ	39 (21.7)	74 (34.9)				
PZ + TZ	45 (25.0)	7 (3.3)				

\*, Mann-Whitney U test; <sup>#</sup>, chi-squared test. ECE, extracapsular extension; CI, confidence interval; PSA, prostate specific antigen; IQR, interquartile range; PI-RADS, prostate imaging reporting and data system; GG, Gleason group; PZ, peripheral zone; TZ, transition zone.



**Figure 3** Comparisons of ROC curves among combined model, radiomics model, clinical model, and Mehralivand grade of radiologists in the training set (A) and validation set (B). TPR, true positive rate; FPR, false positive rate; ROC, receiver operating characteristic; AUC, area under the curve.

redundant features removal of RFE, different classifiers (including LASSO, DT, LR, RF, and SVM) were used to select the optimal radiomics model. The performance of the radiomics model using different classifiers in the training

set and validation set was shown in *Table 5*. Based on the validation set, the AUC of the radiomics model constructed by LASSO classifier was 0.835 (95% CI: 0.763–0.908), which was higher than that of other classifiers. And the



**Table 4** Performance of combined model, radiomics model, clinical model and Mehralivand grade of radiologists in the training set and validation set

Groups	AUC (95% CI)	Sensitivity (%)	Specificity (%)	PPV (%)	NPV (%)	Accuracy (%)	P value (vs. combined model)
Training set							
Combined model	0.897 (0.861–0.934)	81.7 (103/126)	81.8 (121/148)	79.2 (103/130)	84.0 (121/144)	81.8 (224/274)	–
Radiomics model	0.882 (0.844–0.921)	78.6 (99/126)	82.4 (122/148)	79.2 (99/125)	81.9 (122/149)	80.7 (221/274)	0.567
Clinical model	0.805 (0.753–0.857)	69.0 (87/126)	81.8 (121/148)	76.3 (87/114)	75.6 (121/160)	75.9 (208/274)	0.005
Mehralivand grade	0.746 (0.690–0.801)	69.8 (88/126)	70.3 (104/148)	66.7 (88/132)	73.2 (104/142)	70.1 (192/274)	<0.001
Validation set							
Combined model	0.894 (0.837–0.950)	90.7 (49/54)	73.4 (47/64)	74.2 (49/66)	90.4 (47/52)	81.4 (96/118)	–
Radiomics model	0.835 (0.763–0.908)	77.8 (42/54)	75.0 (48/64)	72.4 (42/58)	80.0 (48/60)	76.3 (90/118)	0.167
Clinical model	0.749 (0.658–0.840)	87.0 (47/54)	56.3 (36/64)	62.7 (47/75)	83.7 (36/43)	70.3 (83/118)	0.005
Mehralivand grade	0.774 (0.691–0.857)	70.4 (38/54)	76.6 (49/64)	71.7 (38/53)	75.4 (49/65)	73.7 (87/118)	0.010

AUC, area under the curve; CI, confidence interval; PPV, positive predictive value; NPV, negative predictive value.

**Table 5** Performance of the radiomics model using different classifiers in the training set and validation set

Classifiers	Training set			Validation set		
	AUC (95% CI)	Sensitivity (%)	Specificity (%)	AUC (95% CI)	Sensitivity (%)	Specificity (%)
LASSO	0.882 (0.844–0.921)	78.6	82.4	0.835 (0.763–0.908)	77.8	75.0
DT	1.000 (1.000–1.000)	100.0	100.0	0.619 (0.531–0.706)	51.9	71.9
LR	0.881 (0.843–0.921)	77.0	83.1	0.828 (0.754–0.902)	77.8	75.0
RF	1.000 (1.000–1.000)	100.0	100.0	0.804 (0.725–0.883)	70.4	76.6
SVM	0.879 (0.838–0.919)	78.6	84.5	0.826 (0.750–0.901)	79.6	75.0

AUC, area under the curve; CI, confidence interval; LASSO, least absolute shrinkage and selection operator; DT, decision tree; LR, logistics regression; RF, random forest; SVM, support vector machine.

sensitivity, specificity, and accuracy of radiomics model were 77.8%, 75.0%, and 76.3%, respectively (Figure 3 and Table 4). In the LASSO classifier analysis, 20 radiomics features were selected to build the final radiomics model. The chosen features incorporated nine from ADC, six from DWI, and five from T<sub>2</sub>WI, which were all shown in Table 6. Meanwhile, based on the validation set, the AUC of the radiomics model was significantly higher than that of the clinical model and Mehralivand grade (both P<0.05).

Finally, the AUC, sensitivity, specificity, and accuracy of the combined model in the validation set were 0.894 (95% CI: 0.837–0.950), 90.7%, 73.4%, and 81.4%, respectively. The performance of the combined model was listed in Figure 3 and Table 4. Based on the validation set, the predictive performance in the combined model

was comparable to the radiomics model (P>0.05, 0.894 vs. 0.835), but the sensitivity (90.7% vs. 77.8%) and accuracy (81.4% vs. 76.3%) were higher in the combined model. Meanwhile, the nomogram for the prediction of ECE was constructed based on the combined model, and a good agreement between the combined model and the pathological results was verified by the Hosmer-Lemeshow test (Figure 4). At last, the DCA implied that the combined model could obtain the maximum net clinical benefits compared with the clinical model, Mehralivand grade, and the radiomics model (Figure 5).

## Discussion

In this study, a combined model was constructed based on

**Table 6** Selected radiomics features in the radiomics model

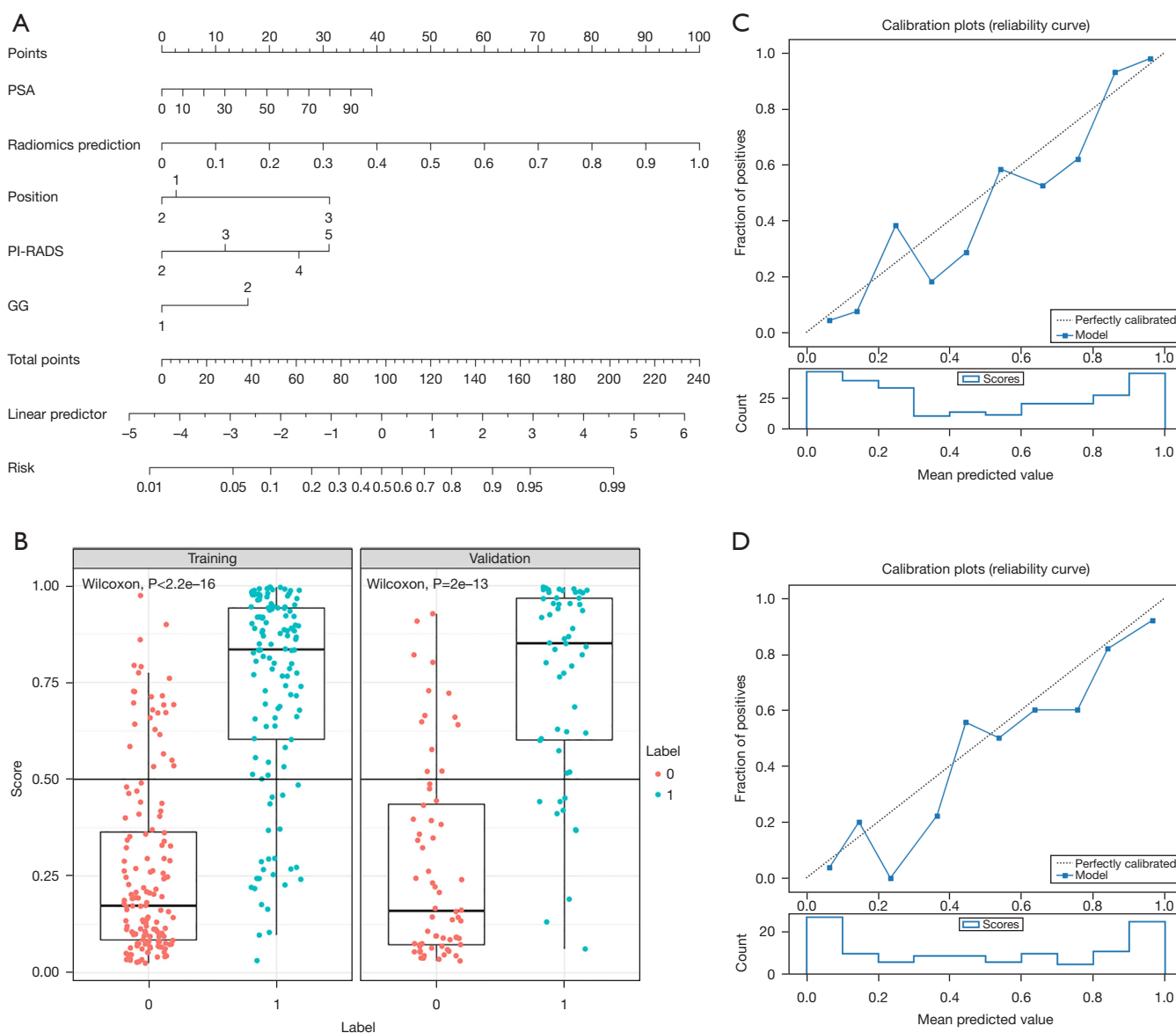
Sequence	Category	Radiomics features	Coefficient
ADC	GLCM	Correlation	0.613772031
	GLRLM	Run entropy	0.956982134
	First-order	Mean	0.136096474
	GLSZM	Small area emphasis	0
	GLSZM	Size zone nonuniformity normalized	-0.328943021
	First-order	Skewness	0.367917783
	GLCM	Maximum probability	-0.334694605
	First-order	10th percentile	-0.679633939
	First-order	Interquartile range	-0.39148876
DWI	GLDM	Busyness	0.258039214
	GLSZM	Size zone nonuniformity	0.676713449
	GLSZM	Low gray level zone emphasis	-0.627712659
	GLSZM	Small area high gray level emphasis	-0.059995032
	GLSZM	Small area emphasis	0.229409054
	GLSZM	Small area low gray level emphasis	0.047497771
T <sub>2</sub> WI	GLSZM	Small area low gray level emphasis	0.273222621
	First-order	Kurtosis	-0.128990984
	First-order	Skewness	0.197613557
	GLRLM	Long run high gray level emphasis	-0.401781693
	GLCM	MCC	0.303335205
ADC	GLCM	Correlation	0.613772031
	GLRLM	Run entropy	0.956982134
	First-order	Mean	0.136096474
	GLSZM	Small area emphasis	0
	GLSZM	Size zone nonuniformity normalized	-0.328943021
	First-order	Skewness	0.367917783
	GLCM	Maximum probability	-0.334694605

ADC, apparent diffusion coefficient; DWI, diffusion-weighted imaging; T<sub>2</sub>WI, T<sub>2</sub>-weighted imaging; GLCM, gray level co-occurrence matrix; GLRLM, gray level run length matrix; GLSZM, gray level size zone matrix; GLDM, gray level dependence matrix; MCC, Matthews correlation coefficient.

MRI radiomics and clinical variables for predicting the risk probability of ECE in PCa and developing an individualized and accurate diagnosis or treatment for PCa patients with better prognoses. The study has established the potential value of the combined model in predicting the ECE of PCa. The combined model performed well in the validation set with an AUC of 0.894, and offered the maximum net

clinical benefits among other models.

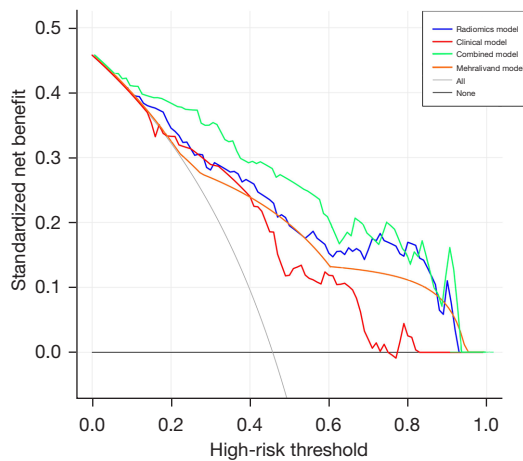
Previous studies have shown that ECE of PCa is closely related to the choice of treatment options and prognosis of patients, especially for disease recurrence and survival following RP (3,4,22). Once ECE is suspected, nerves and blood vessels may be removed to avoid an adverse prognosis (23). The age, PSA, lesion location distribution,



**Figure 4** Performance of the combined model (A-D). (A) The nomogram for the prediction of ECE constructed based on the combined model (GG value in the nomogram: value 1 represents GG  $\leq 3$ , value 2 represents GG  $\geq 4$ ; position value in the nomogram: value 1 represents PZ, value 2 represents TZ, value 3 represents PZ + TZ); (B) comparison of the predictive value in the combined model between the training set (left) and validation set (right); (C,D) calibration curve for combined model prediction of the consistency between the predicted results and pathological results in the training set (C) and validation set (D). PSA, prostate-specific antigen; PI-RADS, Prostate Imaging Report and Data System; GG, Gleason group; ECE, extracapsular extension; PZ, peripheral zone; TZ, transition zone.

percent of biopsy cores positive, biopsy GG, and clinical stage of PCa patients are all closely related to the prognosis of patients (24). Therefore, researchers have built clinical models based on clinical and pathological variables to evaluate preoperative ECE in patients with PCa, such as the Paitin table (25), the Cancer of the Prostate Risk

Assessment (CAPRA) score (26), and the Memorial Sloan Kettering Cancer Center (MSKCC) nomogram (27), etc. However, the diagnostic efficiency of the above models varied, with the AUC ranging from 0.609 to 0.805 (28). Krishna *et al.* (29) used PI-RADS v2 to assess ECE by measuring tumor size and CCL and analyzing the ADC



**Figure 5** The decision curve analysis among combined model, radiomics model, clinical model, and Mehralivand grade. The X-axis represents the threshold probability, and the Y-axis represents the net benefit. The decision curve shows that the incidence of ECE is in the range of 25% to 85%. ECE, extracapsular extension

icons of the lesion. The results found a strong correlation between the PI-RADS v2 score and ECE, with an AUC of 0.72. Matsuoka *et al.* also found that the PI-RADS score could improve the assessment of the clinical stage of the tumor and increase the consistency of ECE assessment among observers (30). Thus, in this study, the PI-RADS v2.1 score was included in clinical variables and it also verified as an independent risk factor of ECE. However, the AUC of the clinical model in the validation set was 0.749, and the accuracy was only 70.3%, roughly similar to the previous studies, indicating the limited value of the clinical model in practice.

Regarding the preoperative diagnosis of ECE in PCa patients, MRI has high diagnostic specificity but low sensitivity. The results also depend a lot on the different experiences of radiologists (31). PI-RADS v2.1 suggests some imaging signs of ECE, including lesion proximity to prostate capsular, irregular or thickened peripheral neurovascular bundles, bulge or disappearance of the capsule and extracapsular lesions, etc. (18). However, there is no definitive quantitative diagnosis of ECE, and PI-RADS v2.1 score alone has limited accuracy for assessing ECE. Recently, some studies have applied staging assessment for ECE (32,33). The Mehralivand grade is an objective and quantitative grading standard approach for the diagnosis of ECE proposed by Mehralivand *et al.* for the first time (19).

In this study, it had verified that there was a fair result in the diagnostic efficacy of the Mehralivand grade in the validation set. The AUC was 0.774, similar to that in Mehralivand *et al.*'s research (AUC =0.77). However, the sensitivity of the Mehralivand grade was slightly low (70.4%) in this study, which could lead to some missed diagnoses of ECE, resulting in untimely treatment.

The application of radiomics has shown good performance in the diagnosis of ECE. Ma *et al.* (34) constructed a LASSO regression model based on T<sub>2</sub>WI to predict ECE in PCa, and 17 radiomics features were finally selected. The AUC of the radiomics model was 0.883 in the validation set, with high sensitivity and specificity, which was better than the performance of the Likert score results in radiologists (AUC =0.600–0.697). In another study by Ma *et al.* (35), a radiomics model was also built based on T<sub>2</sub>WI to predict the occurrence of ECE in the unilateral prostate lobe. The results showed that the AUCs in the validation set was 0.821, further verifying the potential predictive value of radiomics in ECE. T<sub>2</sub>WI is a routine prostate MRI sequence, which can partly reflect the lesion's histopathological characteristics (36). Meanwhile, DWI and ADC are also commonly used functional sequences for prostate, which can provide more information to quantify tumor heterogeneity for the training of radiomics model, and texture features may be more helpful than grayscale-based statistical or morphological features in the diagnosis of ECE (37). Therefore, this study extracted features from T<sub>2</sub>WI, DWI, and ADC.

Different classifiers can produce differences in the results of radiomics model. This study showed that the LASSO analysis had the highest AUC among other classifiers based on the validation set, which was similar to the results of Ma *et al.* (35,36). According to the research, LASSO algorithm can ensure that all important radiomics features can not only be recognized effectively, but also avoid the overfitting problem of classification task (38). So that, it can get better results. In addition, RF, DT and other classifiers have good performance for nonlinear problems. But in the execution of multicollinearity tasks, they may have some problems such as difficulties in processing missing data, over-fitting and ignoring the correlation among each feature attribute, leading to unsatisfactory output results (39). For example, in this study, the AUCs of RF and DT classifiers in the training set were very high, reaching 1.000, but in the validation set, the AUCs were low, only 0.619–0.804, which may be due to the phenomenon of overfitting. Then, the

final selected radiomics model incorporated nine features from ADC, six from DWI, and five features from T<sub>2</sub>WI. Among this selected radiomics features, GLSZM features accounted for the largest proportion, which quantifies gray level zones in an image. A gray level zone is defined as the number of connected voxels that share the same gray level intensity, which reflects the heterogeneity on the medical image (40). The AUC of radiomics model in the validation set was 0.835, which further verified the predictive value of radiomics on ECE by a quantitative and objective method.

Moreover, a combined model was constructed by the PSA, biopsy GG score, lesion location distribution, PI-RADS v2.1 score, and the predictive value in radiomics model in this study. Based on the validation set, the AUC reached 0.894, which showed higher sensitivity and accuracy than the radiomics model, but the AUC value between them was still comparable ( $P > 0.05$ , 0.894 vs. 0.835). Xu *et al.* (41) built a combined nomogram based on multiparametric MRI by integrating a radiomics model and a clinical model (considering PSA and biopsy Gleason score) for preoperative prediction of ECE in PCa patients. Their results showed satisfactory diagnostic performance in ECE, with the AUCs of the radiomics model and combined nomogram being 0.865 and 0.857 for the validation set, respectively. The AUC was slightly higher in the radiomics model than in the combined nomogram, but the prediction efficiency was roughly consistent in these two models. The results in this study are slightly different from those of Xu *et al.* (41) This may be related to the different features extracted from different sequences and the differences between the clinical variables included in the combined model. So far, few studies have reported on the complementarity of clinical variables and radiomics in the prediction of ECE in PCa, so further research is also needed to verify these results.

This study also has some limitations. First, it is a retrospective single-center study without an independent external validation set to evaluate the model's generalization ability. Second, all ROIs used in this study were outlined manually, and the results largely depended on the experience of radiologists. Semi-automatic or automatic segmentation of ROI should be developed and adopted in the future. Third, this study only focused on the existence of ECE in PCa, and the value of ECE in the prediction of biochemical recurrence or prognosis of PCa was not explored. It is expected that further research will be carried out in a later study.

## Conclusions

The proposed combined model based on MRI radiomics and clinical variables has prospected the predictive value for ECE in PCa patients. It can obtain the maximum net clinical benefits compared to the clinical model, Mehrlivand grade of radiologists, and radiomics model, which could be conducive to the preoperative individualized and accurate diagnosis and treatment of patients.

## Acknowledgments

*Funding:* This work was supported by the Special Program for Diagnosis and Treatment Technology of Clinical Key Diseases in Suzhou (grant No. LCZX202001), Medical and Health Science and Technology Innovation Program in Suzhou (grant No. SKY2022003), and Jiangsu Provincial Key Medical Discipline (grant No. JSDW202242).

## Footnote

*Reporting Checklist:* The authors have completed the TRIPOD reporting checklist. Available at <https://tcr.amegroups.com/article/view/10.21037/tcr-22-2750/rc>

*Data Sharing Statement:* Available at <https://tcr.amegroups.com/article/view/10.21037/tcr-22-2750/dss>

*Peer Review File:* Available at <https://tcr.amegroups.com/article/view/10.21037/tcr-22-2750/prf>

*Conflicts of Interest:* All authors have completed the ICMJE uniform disclosure form (available at <https://tcr.amegroups.com/article/view/10.21037/tcr-22-2750/coif>). The authors have no conflicts of interest to declare.

*Ethical Statement:* The authors are accountable for all aspects of the work in ensuring that questions related to the accuracy or integrity of any part of the work are appropriately investigated and resolved. The study was conducted in accordance with the Declaration of Helsinki (as revised in 2013). The study was approved by the Ethics Committee of The First Affiliated Hospital of Soochow University (No. 262; 2021) and individual consent for this retrospective analysis was waived.

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**Cite this article as:** Yang L, Jin P, Qian J, Qiao X, Bao J, Wang X. Value of a combined magnetic resonance imaging-based radiomics-clinical model for predicting extracapsular extension in prostate cancer: a preliminary study. *Transl Cancer Res* 2023;12(7):1787-1801. doi: 10.21037/tcr-22-2750