



CT-based radiomics and clinical characteristics for predicting bone metastasis in lung adenocarcinoma patients

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Background: The occurrence of bone metastasis (BM) will seriously shorten the survival time of lung adenocarcinoma patients and aggravate the suffering of patients. Computed tomography (CT)-based clinical radiomics nomogram may help clinicians stratify the risk of BM in lung adenocarcinoma patients, thereby enabling personalized individualized clinical decision making.

Methods: A total of 501 patients with lung adenocarcinoma from March 2017 to March 2019 were enrolled in the study. Based on plain chest CT images, 1130 radiomics features were extracted from each lesion. One-way analysis of variance (ANOVA) and least absolute shrinkage selection operator (LASSO) algorithm were used for radiomics features selection. Univariate and multivariate analyses were used to screen for clinical characteristics and identify independent predictors of BM. Three models (radiomics model, clinical model and combined model) were constructed to predict BM in lung adenocarcinoma patients. Receiver operating characteristic (ROC) curve and decision curve analysis (DCA) were used to evaluate the performance of the three models. The DeLong test was used to compare the performance of the models.

Results: Finally, the clinical model for predicting BM in lung adenocarcinoma patients was constructed based on 5 independent predictors: cytokeratin 19-fragments (CYFRA21-1), stage, Ki-67, edge, and lobulation. The radiomics model was constructed based on 5 radiomics features. The combined model incorporating clinical independent predictors and radiomics was constructed. In the validation cohort, the area under the curve (AUC) of the clinical model, radiomics model and combined model was 0.824, 0.842 and 0.866, respectively. Delong test showed that in the training cohort, the AUC values of the radiomics model and the combined model were statistically different ($P=0.03$), and the AUC values of the other models were not statistically different. DCA showed that the nomogram had a highest net clinical benefit.

Conclusions: The CT-based clinical radiomics nomogram can be used as a non-invasive and quantitative method to help clinicians stratify the risk of BM in patients with lung adenocarcinoma, thereby enabling personalized clinical decision making.

Keywords: Lung adenocarcinoma; computed tomography (CT); bone metastasis (BM); radiomics; nomogram

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Introduction

Lung cancer stands as a leading cause of cancer-related mortality in the present day, with approximately 2.2 million individuals worldwide receiving a diagnosis of this malignancy annually (1,2). Adenocarcinoma emerges as the predominant histological subtype within the spectrum of lung cancer, comprising over 40% of all primary lung cancer cases (3,4). Compared to other subtypes, adenocarcinoma is noted for its heightened propensity for bone metastasis (BM), with an estimated 20–50% of lung adenocarcinoma patients experiencing this occurrence (5,6). Unfortunately, the survival outlook for patients enduring BM is notably bleak compared to those with metastases in the respiratory and nervous systems (7). The median survival duration post-BM diagnosis is a mere 6–10 months (8,9). Additionally, a significant portion of BM patients (approximately 46%) experienced skeletal-related events, such as bone pain, pathologic fractures, spinal cord compression, and hypercalcemia (10,11). Furthermore, there is a lack of effective treatment methods after the occurrence of BM, traditional anti-tumor therapies may have limited efficacy in treating BM (12). Hence, developing a reliable risk stratification tool for BM in lung adenocarcinoma patients is crucial for identifying individuals at high-risk of developing BM at an early stage. By accurately identifying high-risk patients, healthcare providers can implement proactive monitoring strategies and offer timely interventions to improve patient outcomes and quality of life.

Computerized tomography (CT) has been widely used in the diagnosis, staging and efficacy evaluation of lung

adenocarcinoma because of its advantages of being non-invasiveness, economy and convenience (13–15).

Traditional CT signs can indicate the aggressiveness of lung adenocarcinoma to some extent. Song and colleagues confirmed that the vascular tumor thrombus of lung adenocarcinoma was associated with solid components and lobulated and calcified features in CT images, while nerve invasion was related to features with bronchial inflation sign in CT images (16). However, these studies frequently rely on conventional subjective assessment signs or rudimentary measurements, such as tumor diameter, to assess disease, while ignoring the differences in biological behavior caused by tumor heterogeneity (17,18).

Radiomics involves extracting extensive and intricate information from medical imaging data in a high-throughput fashion, revealing details beyond human visual perception (19). These quantitative or semi-quantitative data from the images can offer insights into the heterogeneity and genetic traits of the lesions (20–22). In recent years, radiomics has been widely used in the diagnosis, clinical staging, histopathological classification, genetic diagnosis, therapeutic effect evaluation, prognosis prediction of lung adenocarcinoma (23–27). However, there are few studies on radiomics for predicting BM in lung adenocarcinoma patients. Therefore, this study aims to investigate the value of clinical characteristics and CT radiomics in predicting BM in lung adenocarcinoma patients. We present this article in accordance with the TRIPOD reporting checklist (available at <https://tcr.amegroups.com/article/view/10.21037/tcr-24-38/rc>).

Methods

Patients and clinical characteristics

The retrospective study was approved by ethics committee of the Affiliated Hospital of Qingdao University (No. QYFYWZLL28400) and individual consent for this retrospective analysis was waived. The study was conducted in accordance with the Declaration of Helsinki (as revised in 2013).

This study included 1,369 patients with confirmed pathologic lung adenocarcinoma diagnosed at the Affiliated Hospital of Qingdao University from March 2017 to March 2019. Following rigorous selection criteria, a subset of patients was excluded: (I) synchronous BM at baseline examination; (II) with other primary malignant tumors; (III) incomplete clinical and follow-up data or poor CT image

Highlight box

Key findings

- Computed tomography-based clinical radiomics nomogram can be used to predict bone metastasis (BM) in lung adenocarcinoma patients.

What is known and what is new?

- Radiomics features have been confirmed to characterize the heterogeneity of tumors and have been widely used to predict the biological behavior of tumors.
- We developed and validated three models to predict the risk of BM in lung adenocarcinoma patients.

What is the implication, and what should change now?

- Our clinical radiomics nomogram can help clinicians stratify the risk of BM in lung adeno-carcinoma patients, thereby enabling personalized clinical decision making.

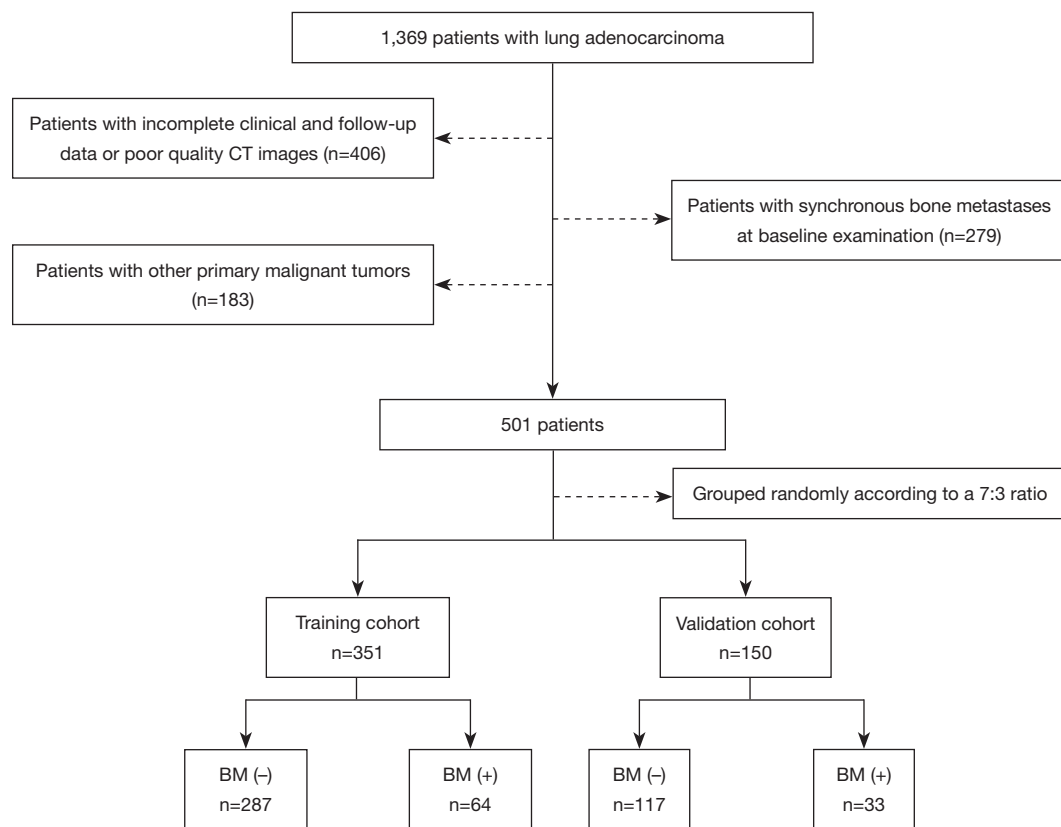


Figure 1 Patient recruitment flow chart. BM, bone metastasis; CT, computed tomography.

quality. Finally, 501 patients were enrolled in the study. *Figure 1* illustrates the recruitment process of patients. It is pertinent to highlight that, for the precise quantification of the correlation between BM and potential risk factors, individuals presenting with pre-existing BM at the initial diagnosis of lung adenocarcinoma were intentionally omitted from the study cohort (n=279). Patients were randomly assigned to the training cohort (n=351) and the validation cohort (n=150) in a 7:3 ratio.

Previous studies have identified gender, age, tumor diameter, serum carbohydrate antigen 125 (CA125), alkaline phosphatase (ALP), and degree of differentiation as independent risk factors for BM in lung cancer (28-30). Based on this, we selected clinical factors including general clinical information, histopathological information, and traditional CT features. General clinical information include age, gender, smoking history, stage, serum carcinoembryonic antigen (CEA), CA125, cytochrome-19-fragment (CYFRA21-1) and ALP within 2 weeks before

surgery or puncture. Stage was evaluated by the 8th edition of the International Association for the Study of Lung Cancer (IASLC) staging system (31). The histopathologic information was interpreted by a pathologist with 5 years of experience in pulmonary diseases, included the Ki-67 expression level, and epidermal growth factor receptor (EGFR) gene status. Traditional CT features included primary tumor maximum diameter, location (peripheral/central), shape (regular/irregular), morphology (solid/mixed/ground-glass), edge (clear/vague), lobulation (yes/no), spiculation (yes/no), cavity (yes/no), vacuole (yes/no), air bronchogram (yes/no), pleural traction (yes/no), pleural thickening (yes/no), pleural effusion (yes/no) and vessel convergence (yes/no). Two experienced radiologists, with 5 and 8 years of professional experience, respectively, independently observed the conventional CT features without prior knowledge of BM status. Consensus was reached when both radiologists shared the same opinion, while any discrepancies were resolved through discussion

and final agreement with a senior radiologist boasting over 15 years of diagnostic expertise.

CT image acquisition and preprocessing

All patients underwent chest CT scans prior to diagnosis, with scanning parameters outlined in [Table S1](#). To mitigate variances resulting from varied parameters, image standardization was implemented using the PyRadiomics python software plugin. Voxel sizes were resampled to a consistent $3 \times 3 \times 3$ mm³ dimension to ensure uniformity (the bin width of the gray value discretization was set to 25) (32).

Follow up

The date of last follow-up was June 30, 2023. The end point of this study was BM identified by bone scanning, positron emission tomography/computed tomography (PET/CT), or biopsy. Patients were followed at least every 6 months for 2 years after diagnosis and at least annually thereafter, with data collected through health-system inquiries and telephone calls.

Clinical model development

Clinical characteristics were screened using univariate and multivariate analyses to identify independent predictors associated with BM, and clinical models were developed based on these independent predictors. Odds ratio (OR) for each factor was used as an estimate of the relative risk with 95% confidence intervals (CIs).

Segmentation and feature extraction

Segmentation of 3D regions of interest (ROI) was performed with the use of ITK-SNAP software (version 3.8.0, www.itksnap.org) (33).

The images were initially segmented by Radiologist 1, following which 60 patients' CT images were randomly chosen from the entire dataset and re-segmented by Radiologist 2. Inter-class correlation coefficient (ICC) was employed to assess the reproducibility of radiomics features. Features extracted from both segmentations were compared, and only those exhibiting an ICC >0.75 were kept for further analysis (34).

The radiomics features were extracted using the python software plug-in PyRadiomics. A total of 1,130 radiomics features were extracted, including 14 shape features, 18

first-order features, 24 Gray Level Co-occurrence Matrix (GLCM) features, 14 Gray Level Dependence Matrix (GLDM) features, 16 Gray Level Run Length Matrix (GLRLM) features, 16 Gray Level Size Zone Matrix (GLSZM) features, 5 Neighboring Gray Tone Difference Matrix (NGTDM) features, and 1,023 filter and wavelet features. [Figure 2](#) illustrates the flow of the study.

Radiomics feature selection and model development

During model development, the training cohort data underwent dimensionality reduction screening to identify optimal radiomics features for model construction. Subsequently, the validation cohort data was inputted into the developed model for verification, assessing its predictive performance.

To prevent overfitting, a two-step process was employed for dimension reduction of radiomics features in the training cohort. Initially, distinguishing features between the BM and non-BM groups were identified through analysis of variance (ANOVA). Subsequently, the optimal features were chosen using the least absolute shrinkage selection operator (LASSO) algorithm (35). Combining the selected features, the radiomics model was developed, and the radiomics score (Rad-score) was calculated for each patient. The nomogram was then constructed, incorporating radiomics features and independent clinical predictors, assigned individual scores on a 0–100 scale, and summed to determine the overall risk of BM in lung adenocarcinoma patients. Calibration curves were utilized to evaluate the alignment between predicted outcomes and actual observations.

Efficacy evaluation of models

Receiver operating characteristic (ROC) curves were generated, area under the curve (AUC), accuracy, sensitivity and specificity were used to evaluate the efficacy of the three models (clinical model, radiomics model and combined model). The DeLong test was used to compare the performance of the models.

Decision curve analysis (DCA) was used to evaluate the clinical utility of the prediction model by calculating the net gain at different probability thresholds (36).

Statistical analysis

SPSS software (Version 25.0, IBM) was used for univariate analysis (including Chi-squared or Mann-Whitney U test).

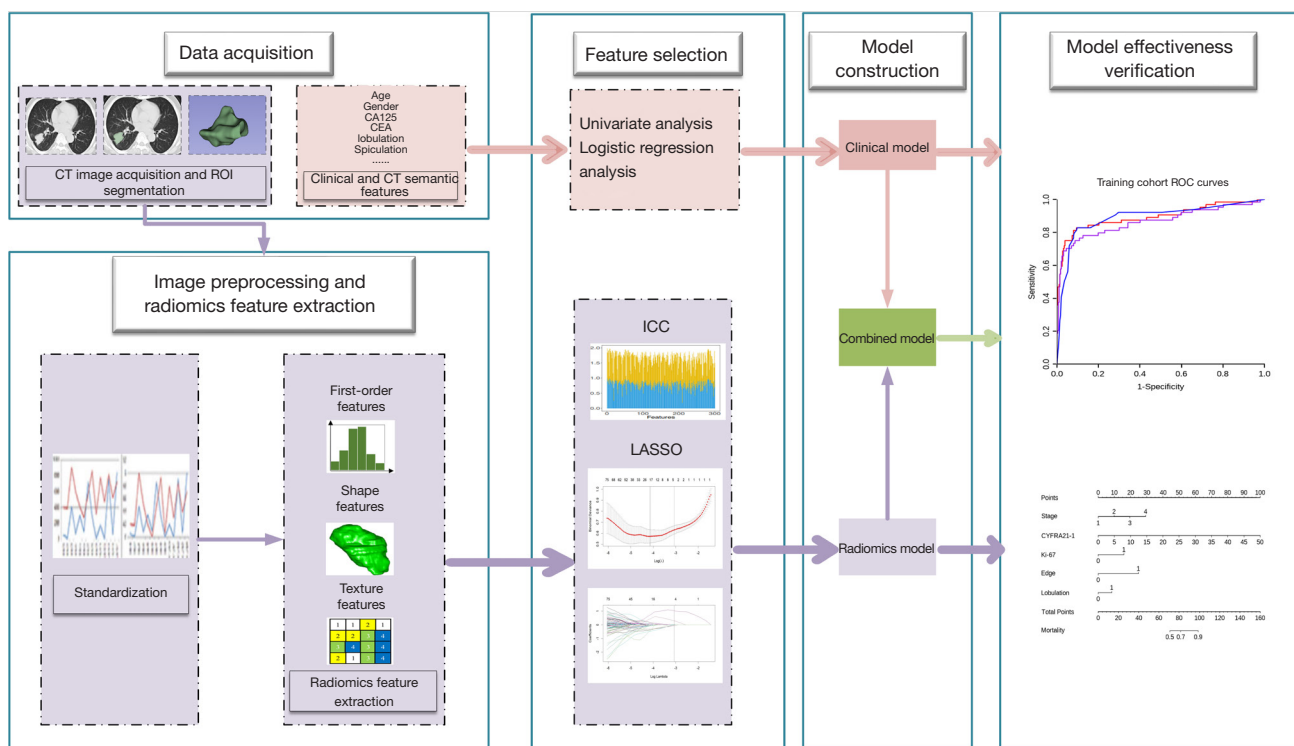


Figure 2 Workflow diagram illustrates the development of three models for predicting BM in patients with lung adenocarcinoma. CT, computed tomography; ROI, region of interest; CEA, carcinoembryonic antigen; CA125, carbohydrate antigen 125; ICC, inter-class correlation coefficient; LASSO, least absolute shrinkage selection operator; BM, bone metastasis; ROC, receiver operating characteristic; CYFRA21-1, cytokeratin 19-fragments.

ANOVA, ICC, LASSO regression analysis, ROC analysis, calibration curve, DCA were performed in R statistical software (Version 4.1.0, <https://www.r-project.org>). Two-sided $P < 0.05$ were considered to indicate statistical significance.

Results

Clinical characteristics

Among 501 lung adenocarcinoma patients, the median follow-up time was 58 months (range, 2–76 months) and 97 patients (19.36%) experienced BM. The baseline data of the patients are shown in *Table 1*. There was no significant difference in the distribution of clinical characteristics between the training cohort and validation cohort (*Table S2*). After univariate and multivariate analysis, 5 independent risk predictors for BM in lung adenocarcinoma patients were determined: CYFRA21-1 (OR =1.211, $P=0.002$), stage (OR =2.637, $P<0.001$), Ki-67 (OR =26.444, $P=0.006$), edge (OR =9.752, $P<0.001$), and lobulation (OR =4.308, $P=0.02$). The results of the multivariate analysis of

clinical characteristics are shown in *Table S3*.

Radiomics feature selection and model construction

There were 1,094 stable features retained, and 735 features were selected by ANOVA, finally, after LASSO analysis, five radiomics features were used to construct the radiomics model. *Figure 3* shows the process of radiomics features selection and its corresponding coefficients. In addition, the Rad-score of each patient were calculated, calculation formula is in *Appendix 1*.

Efficacy and clinical application of the model

The predictive efficacy of the models is shown in *Table 2* and the ROC curve (*Figure 4*) showed that the three prediction models had good performance and could finely predict BM in lung adenocarcinoma patients. In the validation cohort, the AUC of the clinical model, radiomics model and combined model was 0.824 (95% CI: 0.734–0.913), 0.842

Table 1 Baseline characteristics of the patients

Characteristics	Training cohort (n=351)			Validation cohort (n=150)		
	BM (+)	BM (-)	P value	BM (+)	BM (-)	P value
Age, year, median (range)	59.00 (52.00–65.00)	61.00 (53.00–66.00)	0.296	60.00 (53.50–63.50)	61.00 (52.00–65.00)	0.656
Maximum diameter, mm, median (range)	35.50 (21.00–45.00)	20.00 (13.00–30.00)	<0.001	34.00 (23.50–43.50)	21.00 (13.50–28.00)	<0.001
CEA, ng/mL, median (range)	13.60 (2.98–47.50)	1.65 (0.93–3.16)	<0.001	4.92 (2.19–26.00)	1.63 (1.02–3.87)	<0.001
CA125, U/mL, median (range)	21.53 (10.25–75.00)	10.00 (7.51–15.65)	<0.001	14.00 (8.00–67.00)	11.00 (8.00–14.13)	0.079
CYFRA21-1, ng/mL, median (range)	3.99 (2.42–7.96)	2.27 (1.77–3.17)	<0.001	3.53 (2.19–5.09)	2.32 (1.78–3.16)	0.002
ALP, U/L, median (range)	72.50 (62.00–88.00)	67.00 (56.00–82.00)	0.039	72.50 (62.00–85.00)	68.00 (55.00–84.00)	0.317
Gender (male/female)	39/25	117/170	0.003	10/23	49/68	0.229
Smoking history (yes/no)	27/37	73/214	0.007	8/25	36/81	0.467
Ki-67 ($\leq 5\%$ / $> 5\%$)	1/63	149/138	<0.001	5/28	62/55	<0.001
EGFR (mutant/wild)	41/23	163/124	0.287	22/11	61/56	0.138
Location (peripheral/central)	54/10	278/9	<0.001	29/4	115/2	0.028
Shape (regular/irregular)	12/52	77/210	0.179	8/25	23/94	0.566
Edge (clear/vague)	15/49	183/104	<0.001	9/24	65/52	0.004
Lobulation (yes/no)	55/9	156/131	<0.001	25/8	70/47	0.094
Spiculation (yes/no)	29/35	87/200	0.021	18/15	37/80	0.016
Cavity (yes/no)	1/63	6/281	0.785	5/28	3/114	0.016
Vacuole (yes/no)	9/55	38/249	0.861	4/29	17/100	0.946
Air bronchogram (yes/no)	25/39	52/235	<0.001	15/18	27/90	0.011
Pleural traction (yes/no)	49/15	138/149	<0.001	28/5	65/52	0.002
Pleural thickening (yes/no)	14/50	20/267	<0.001	5/28	10/107	0.430
Pleural effusion (yes/no)	19/45	14//273	<0.001	6/27	3/114	0.003
Vessel convergence (yes/no)	18/46	39/248	0.004	7/26	28/89	0.744
Morphology (solid/mixed/ground-glass)	60/3/1	159/62/66	<0.001	27/3/3	66/20/31	0.027
Stage (I/II/III/IV)	7/15/16/26	229/22/22/14	<0.001	8/1/12/12	89/8/13/7	<0.001

BM, bone metastasis; CEA, carcinoembryonic antigen; CA125, carbohydrate antigen 125; CYFRA21-1, cytokeratin-19-fragments; ALP, alkaline phosphatase; EGFR, epidermal growth factor receptor.

(95% CI: 0.754–0.930) and 0.866 (95% CI: 0.786–0.947), respectively. Delong test showed that in the training cohort, the AUC values of the radiomics model and the combined model were statistically different ($P=0.03$), and the AUC values of the other models were not statistically different, detailed results are provided in [Table S4](#). The integrated

nomogram ([Figure 5A](#)) incorporating both radiomic and clinical characteristics was developed. The calibration curves ([Figure 5B, 5C](#)) confirmed close alignment between predicted outcomes and real situation. DCA ([Figure 6](#)) showed that the nomogram had a highest net clinical benefit.

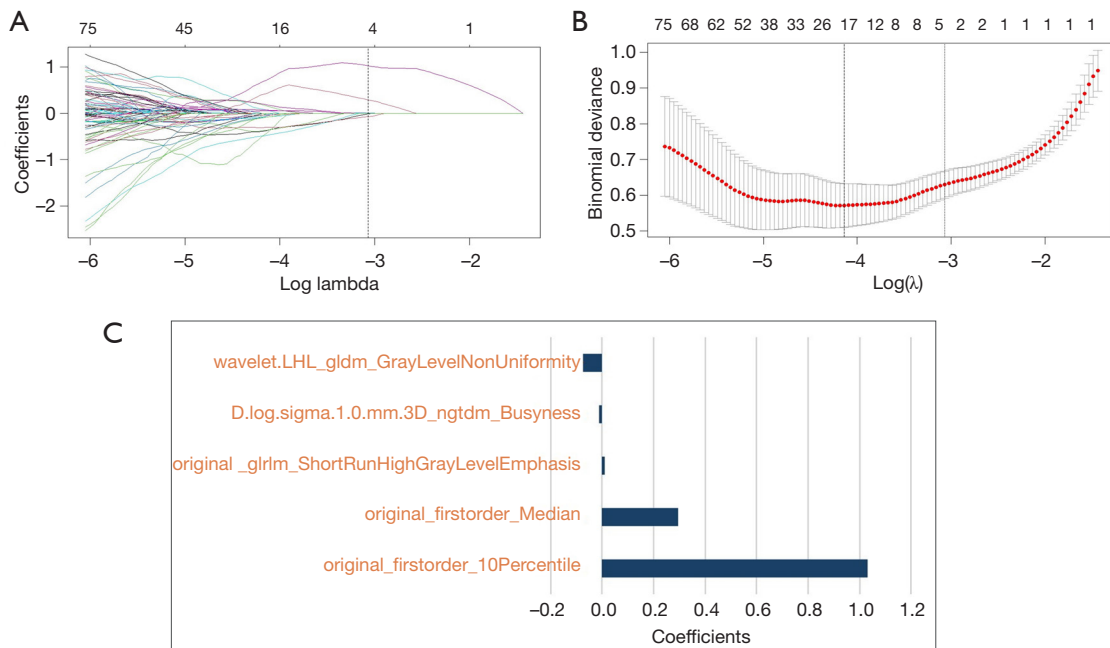


Figure 3 Radiomics features selection using LASSO binary logistic regression model. (A) Features were selected by LASSO regression and 10-fold cross-validation; (B) coefficient curves based on radiomic features with non-zero coefficients are determined by λ; (C) 5 radiomic features and their corresponding coefficients were selected. LASSO, least absolute shrinkage selection operator.

Table 2 Predictive efficacy of the three models

Model	Training cohort				Validation cohort			
	AUC (95% CI)	Accuracy	Sensitivity	Specificity	AUC (95% CI)	Accuracy	Sensitivity	Specificity
Radiomics model	0.865 (0.802–0.928)	0.883	0.750	0.913	0.842 (0.754–0.930)	0.827	0.758	0.846
Clinical model	0.890 (0.837–0.944)	0.889	0.828	0.902	0.824 (0.734–0.913)	0.853	0.697	0.897
Combined model	0.894 (0.838–0.950)	0.892	0.828	0.906	0.866 (0.786–0.947)	0.860	0.727	0.897

AUC, area under the curve; CI, confidence interval.

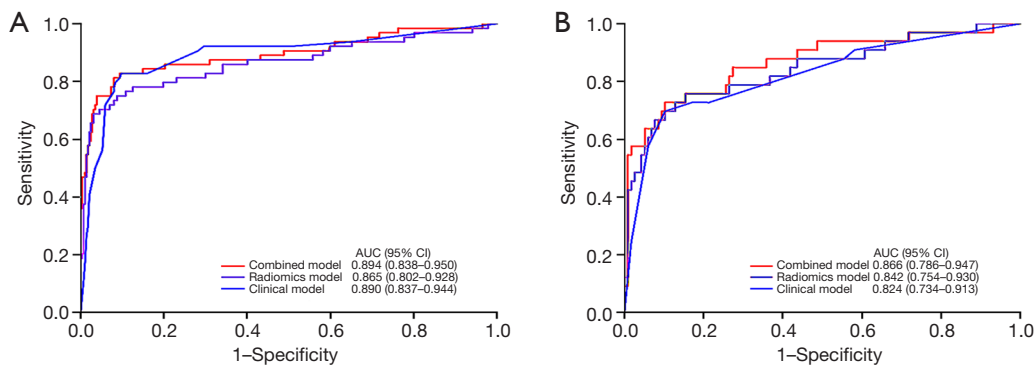


Figure 4 ROC curve for the three models in the training (A) and validation cohorts (B). ROC, receiver operating characteristic; CI, confidence interval.

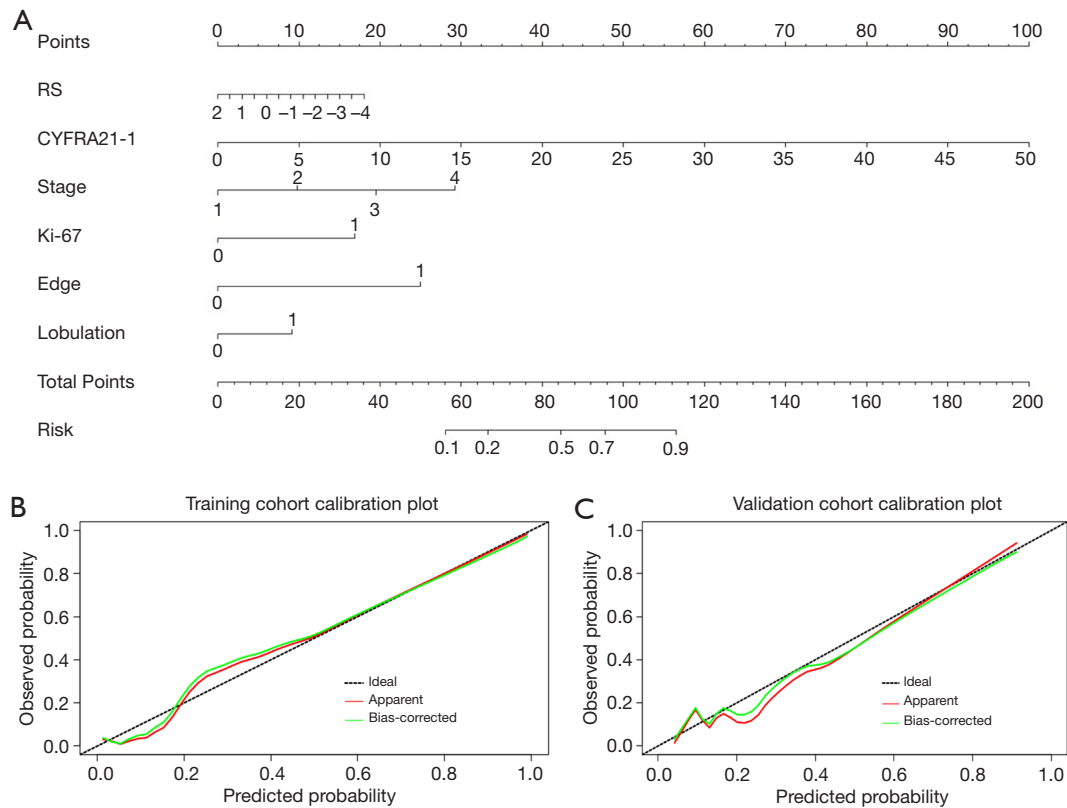


Figure 5 The clinical-radiomics nomogram based on the combined model was developed for clinical application. (A) The clinical-radiomics nomogram; (B) calibration curves of the nomogram in the training cohort; (C) calibration curves of the nomogram in the validation cohort. RS, radiomics score; CYFRA21-1, cytokeratin 19-fragments.

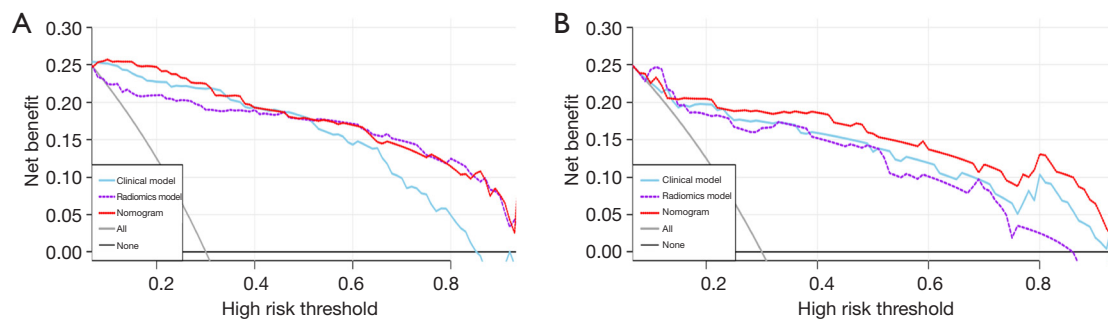


Figure 6 DCA of the three models in the training (A) and validation (B) cohorts. The vertical axis represents the net benefit and the horizontal axis represents the threshold probability. DCA, decision curve analysis.

Discussion

In this study, 19.36% of the cohort of patients with lung adenocarcinoma developed BM during the course of their disease. In other studies, the BM rate varied between 20% and 50% (5,6), which may be due to methodological

differences between studies. Notably patients who developed BM at the time of diagnosis were excluded from our study population. The endpoint event (i.e., BM) occurs in only about 1/5 of all patients, and how to cope with this data imbalance caused by the epidemiology of the disease or the characteristics of the disease itself is currently

controversial. It has been argued that in machine learning research, oversampling for small-sample classification (represented by the SMOTE classical algorithm) can improve model efficacy in some cases, but it has also been pointed out that these algorithms for extended samples tend to lead to overfitting and do not really improve model performance (37-39), in our study, we did not perform sample balancing on the raw data in order to avoid model overfitting problems. Our findings underscore the strong predictive capabilities of three models for forecasting BM in lung adenocarcinoma, with the integrated radiomics and clinical characteristics model exhibiting superior predictive efficacy compared to singular clinical or radiomics models. This model achieved an impressive AUC of 0.894 and 0.866 in the training and validation cohorts, respectively.

Many studies had focused on the risk predictors of BM in NSCLC, Li *et al.* analyzed the clinical characteristics of 50,581 NSCLC patients based on machine learning, and the results showed that the sex, grade, laterality, histology, T stage, N stage, and chemotherapy were independent risk predictors of BM (40). In a study of risk predictors for distant metastasis (DM) in patients with completely resected lung adenocarcinoma patients, larger tumor size, lymph node metastasis, and vascular lymphatic invasion were considered to be significantly associated with the occurrence of BM (41). In our study, stage, Ki-67, edge and lobulation were thought to be associated with the occurrence of BM, which are basically consistent with the results of previous studies. It is worth to mention that we found that abnormal elevation of CYFRA21-1 was associated with the occurrence of BM, which is consistent with Zhang *et al.*'s opinion that CYFRA21-1 levels have a stronger correlation with the occurrence of metastasis in patients with lung cancer, especially lung adenocarcinoma (42).

By translating images into quantitative data, radiomics is poised to emerge as a novel tool for depicting tumor heterogeneity and guiding personalized treatment strategies. Previous studies have confirmed the potential value of radiomics in predicting DM of lung adenocarcinoma patients. Coroller *et al.* delineated that 35 CT-based radiomics attributes exhibited correlations with DM occurrences (43). Furthermore, Peng *et al.* developed and validated 5 models leveraging clinical and CT radiomics features in a cohort of 253 patients with solid lung adenocarcinoma for predicting DM. Ultimately, their findings highlighted that an integrated model encompassing three-dimensional (3D), two-dimensional (2D) radiomics features alongside clinical characteristics

yielded superior predictive efficacy (AUC =0.892) (44). However, the application of radiomics in predicting BM of lung adenocarcinoma has not been reported.

In our study, 5 CT-based radiomics features were found to be associated with BM in lung adenocarcinoma, most (3/5) of which were texture features. Texture features use the distribution characteristics of gray levels in medical images to evaluate the heterogeneity within lesions (45), previous studies have found that texture features of CT images are related to tumor metabolism and staging in NSCLC (46), and have the potential to act as imaging biomarkers for reflecting tumor hypoxia and angiogenesis (47). In a recent study, CT images of 428 patients with clinical stage IA lung adenocarcinoma were analyzed, and the results showed that the texture-based nomogram could predict the pathological aggressiveness of early lung adenocarcinoma with an AUC of 0.849 (48). The study by Sacconi *et al.* also demonstrated a potential association between CT texture features and EGFR and survival in patients with lung adenocarcinoma (49). Based on the above research, we suggest that these radiomics features representing tumor microenvironment and heterogeneity information may be related to BM in patients with lung adenocarcinoma, and the constructed radiomics prediction model achieved good prediction performance (AUC =0.842 in the validation cohort). In addition, the performance of the combined model by including radiomics and independent clinical risk predictors has been improved in predicting BM in lung adenocarcinoma patients, with an AUC of 0.866 in the validation cohort. This tool helps identify patients at high risk for BM prior to surgery, triggering closer monitoring and necessary interventions by clinicians.

Inevitably, there are some limitations to the study. First, it is a retrospective study, which may lead to selection bias. Second, although radiomics has been shown to be a potential tool for characterizing tumor heterogeneity, there is still a lack of standard radiomics processing procedures for image acquisition and segmentation, feature selection, and model evaluation, and well-designed prospective clinical trials with good quality control are needed. Furthermore, the optimal approach for model development involves the creation of three distinct cohorts for training, testing, and external validation. Regrettably, due to limitations in sample size, our study only implemented training and validation cohorts. Moving forward, efforts will be directed towards expanding the sample size to facilitate the creation of a more robust and scientifically sound model.

Conclusions

In conclusion, the CT-based clinical radiomics nomogram can be used as a non-invasive and quantitative method to help clinicians stratify the risk of BM in patients with lung adenocarcinoma, thereby enabling personalized clinical decision making.

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Footnote

Reporting Checklist: The authors have completed the TRIPOD reporting checklist. Available at <https://tclr.amegroups.com/article/view/10.21037/tlcr-24-38/rc>

Data Sharing Statement: Available at <https://tclr.amegroups.com/article/view/10.21037/tlcr-24-38/dss>

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Conflicts of Interest: All authors have completed the ICMJE uniform disclosure form (available at <https://tclr.amegroups.com/article/view/10.21037/tlcr-24-38/coif>). The authors have no conflicts of interest to declare.

Ethical Statement: The authors are accountable for all aspects of the work in ensuring that questions related to the accuracy or integrity of any part of the work are appropriately investigated and resolved. The study was conducted in accordance with the Declaration of Helsinki (as revised in 2013). The study was approved by the ethics committee of Affiliated Hospital of Qingdao University (No. QYFYWZLL28400) and individual consent for this retrospective analysis was waived.

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Appendix 1 The Rad-score formula

$$\begin{aligned} \text{Rad-score} = & 1.031 \times \text{original_firstorder10Percentile} + \\ & 0.294 \times \text{original_firstorder_Median} + \\ & 0.010 \times \text{original_glrlm_ShortRunHighGrayLevelEmphasis} + \\ & -0.011 \times \text{log.sigma.1.0.mm.3D_ngtdm_Busyness} + \\ & -0.074 \times \text{wavelet.LHL_gldm_GrayLevelNonUniformity} \end{aligned}$$

Table S1 CT scanning parameters

CT scanner	CT 256	CT 128	CT 64	CT 64	CT 64	CT 16
Scanner model	Brilliance iCT 256	Somatom Definition Flash	Somatom Sensation 64	Discovery 750	LightSpeed VCT	Brilliance 16
Manufacturer	Philips	Siemens	Siemens	General Electric	General Electric	Philips
Gantry rotation time (s)	0.5	0.28	0.5	0.5	0.5	0.5
Tube voltage (kV)	120	120	120	120	120	120
Tube current	250 mAs	Ref. 200 mAs	200 mAs	200–400 mAs (automatic tube current modulation)	200 mAs	200 mAs
Detector collimation (mm)	0.625	0.6	0.6	0.625	0.625	0.75
Matrix	512×512	512×512	512×512	512×512	512×512	512×512
Pitch	0.915	1.0	1.0	1.375	0.984	1
Slice thickness (mm)	5	5	5	5	5	5

Table S2 Baseline data of patients in the training cohort and validation cohort

Characteristics	Training cohort (n=351)	Validation cohort (n=150)	P value
Age, year, median (range)	61.00 (53.00–63.00)	61.00 (51.00–64.25)	0.253
Maximum diameter, mm, median (range)	21.00 (14.00–32.00)	24.00 (14.75–31.25)	0.643
CEA, ng/mL, median (range)	2.04 (1.02–4.58)	1.81 (1.09–4.86)	0.879
CA125, U/mL, median (range)	10.74 (7.79–18.32)	11.06 (8.00–17.69)	0.733
CYFRA21-1, ng/mL, median (range)	2.41 (1.84–3.47)	2.44 (1.82–3.64)	0.758
ALP, U/L, median (range)	68.00 (56.00–82.00)	69.00 (55.00–84.25)	0.730
Gender (male/female)	156/195	59/91	0.290
Smoking history (yes/no)	100/251	44/106	0.914
Ki-67 ($\leq 5\%$ / $> 5\%$)	150/201	67/83	0.689
EGFR (mutant/wild)	147/204	67/83	0.564
Location (peripheral/central)	332/19	144/6	0.506
Shape (regular/irregular)	89/262	31/119	0.260
Edge (clear/vague)	198/153	74/76	0.145
Lobulation (yes/no)	211/140	95/55	0.496
Spiculation (yes/no)	116/235	55/95	0.434
Cavity (yes/no)	7/344	8/142	0.085
Vacuole (yes/no)	47/304	21/129	0.855
Air bronchogram (yes/no)	77/274	42/108	0.144
Pleural traction (yes/no)	187/164	93/57	0.072
Pleural thickening (yes/no)	34/317	15/135	0.914
Pleural effusion (yes/no)	33/318	9/141	0.208
Vessel convergence (yes/no)	57/294	35/115	0.060
Morphology (solid/mixed/ground-glass)	219/65/67	93/23/34	0.528
Stage (I/II/III/IV)	236/37/38/40	97/9/25/19	0.421

CEA, carcinoembryonic antigen; CA125, carbohydrate antigen 125; CYFRA21-1, cytokeratin-19-fragment; ALP, alkaline phosphatase; EGFR, epidermal growth factor receptor.

Table S3 The results of multivariate analysis

Characteristics	OR (95% CI)	P value
Maximum diameter	0.990 (0.956–1.024)	0.544
CEA	0.999 (0.994–1.005)	0.760
CA125	1.002 (0.997–1.008)	0.389
CYFRA21-1	1.211 (1.073–1.367)	0.002
ALP	0.995 (0.980–1.011)	0.545
Gender	0.601 (0.250–1.443)	0.254
Smoking history	0.307 (0.091–1.033)	0.057
Ki-67	26.444 (2.554–273.831)	0.006
Location	1.809 (0.390–8.383)	0.449
Edge	9.752 (3.407–27.913)	<0.001
Lobulation	4.308 (1.225–15.143)	0.023
Spiculation	1.597 (0.646–3.944)	0.310
Air bronchogram	1.679 (0.619–4.553)	0.309
Pleural traction	2.219 (0.843–5.840)	0.107
Pleural thickening	1.145 (0.326–4.014)	0.833
Pleural effusion	1.874 (0.433–8.116)	0.401
Vessel convergence	1.536 (0.556–4.249)	0.408
Morphology	1.268 (0.427–3.761)	0.669
Stage	2.637 (1.687–4.124)	<0.001

CEA, carcinoembryonic antigen; CA125, carbohydrate antigen 125; CYFRA21-1, cytokeratin-19-fragment; ALP, alkaline phosphatase; OR, odds ratio; CI, confidence interval.

Table S4 Results of the DeLong test of the model

Models	Training cohort		Validation cohort	
	Z value	P value	Z value	P value
Clinical model vs. radiomics model	0.943	0.346	0.387	0.699
Clinical model vs. combined model	0.246	0.806	0.954	0.340
Radiomics model vs. combined model	2.138	0.033*	1.479	0.139

*, statistically significant differences.